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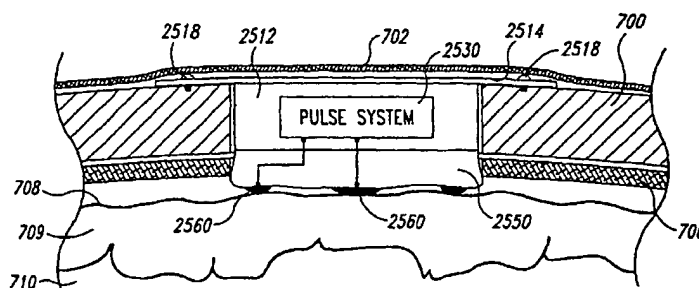
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(54) Title: METHODS AND APPARATUS FOR EFFECTUATING A LASTING CHANGE IN A NEURAL-FUNCTION OF A PATIENT



(57) Abstract: The following disclosure describes several methods and apparatus for intracranial electrical stimulation to treat or otherwise effectuate a change in neural-functions of a patient. Several embodiments of methods in accordance with the invention are directed toward enhancing or otherwise inducing a lasting change in neural activity to effectuate a particular neural-function. Such lasting change in neural activity is defined as "neuroplasticity". The methods in accordance with the invention can be used to treat brain damage (e.g., stroke, trauma, etc.), brain disease (e.g., Alzheimer's, Pick's, Parkinson's, etc.), and/or brain disorders (e.g., epilepsy, depression, etc.). The methods in accordance with the invention can also be used to enhance neural-function of normal, healthy brains (e.g., learning, memory, etc.), or to control sensory functions (e.g., pain). Certain embodiments of methods in accordance with the invention electrically stimulate the brain at a stimulation site where neuroplasticity is occurring. The stimulation site may be different than the region in the brain where neural activity is typically present to perform the particular neural function according to the functional organization of the brain. In one embodiment in which neuroplasticity related to the neural-function occurs in the brain, the method can include identifying the location where such neuroplasticity is present. In an alternative embodiment in which neuroplasticity is not occurring in the brain, an alternative aspect is to induce neuroplasticity at a stimulation site where it is expected to occur. Several embodiments of these methods that are expected to produce a lasting effect on the intended neural activity at the stimulation site use electrical pulses that increase the resting membrane potential of neurons at the stimulation site to a subthreshold level.

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## METHODS AND APPARATUS FOR EFFECTUATING A LASTING CHANGE IN A NEURAL-FUNCTION OF A PATIENT

### CROSS-REFERENCE TO RELATED APPLICATION

This application claims the benefit of U.S. Provisional Application No. 60/217,981, filed July 31, 2000, which is incorporated herein in its entirety.

### TECHNICAL FIELD

Several embodiments of methods and apparatus in accordance with the invention are related to electrically stimulating a region in the cortex or other area of the brain to bring about a lasting change in a physiological function and/or a mental process of a patient.

### BACKGROUND

A wide variety of mental and physical processes are known to be controlled or are influenced by neural activity in particular regions of the brain. In some areas of the brain, such as in the sensory or motor cortices, the organization of the brain resembles a map of the human body; this is referred to as the "somatotopic organization of the brain." There are several other areas of the brain that appear to have distinct functions that are located in specific regions of the brain in most individuals. For example, areas of the occipital lobes relate to vision, regions of the left inferior frontal lobes relate to language in the majority of people, and regions of the cerebral cortex appear to be consistently involved with conscious awareness, memory, and intellect. This type of location-specific functional organization of the brain, in which discrete locations of the brain are statistically likely to control particular mental or physical functions in normal individuals, is herein referred to as the "functional organization of the brain."

Many problems or abnormalities with body functions can be caused by damage, disease and/or disorders of the brain. A stroke, for example, is one very common condition that damages the brain. Strokes are generally caused by emboli

(*e.g.*, obstruction of a vessel), hemorrhages (*e.g.*, rupture of a vessel), or thrombi (*e.g.*, clotting) in the vascular system of a specific region of the cortex, which in turn generally causes a loss or impairment of a neural function (*e.g.*, neural functions related to face muscles, limbs, speech, etc.). Stroke patients are typically treated using physical therapy to rehabilitate the loss of function of a limb or another affected body part. For most patients, little can be done to improve the function of the affected limb beyond the recovery that occurs naturally without intervention. One existing physical therapy technique for treating stroke patients constrains or restrains the use of a working body part of the patient to force the patient to use the affected body part. For example, the loss of use of a limb is treated by restraining the other limb. Although this type of physical therapy has shown some experimental efficacy, it is expensive, time-consuming and little-used. Stroke patients can also be treated using physical therapy plus adjunctive therapies. For example, some types of drugs, such as amphetamines, that increase the activation of neurons in general, appear to enhance neural networks; these drugs, however, have limited efficacy because they are very non-selective in their mechanisms of action and cannot be delivered in high concentrations directly at the site where they are needed. Therefore, there is a need to develop effective treatments for rehabilitating stroke patients and patients that have other types of brain damage.

Other brain disorders and diseases are also difficult to treat. Alzheimer's disease, for example, is known to affect portions of the cortex, but the cause of Alzheimer's disease and how it alters the neural activity in the cortex is not fully understood. Similarly, the neural activity of brain disorders (*e.g.*, depression and obsessive-compulsive behavior) is also not fully understood. Therefore, there is also a need to develop more effective treatments for other brain disorders and diseases.

The neural activity in the brain can be influenced by electrical energy that is supplied from an external source outside of the body. Various neural functions can thus be promoted or disrupted by applying an electrical current to the cortex or other region of the brain. As a result, the quest for treating damage, disease and disorders in the brain have led to research directed toward using electricity or magnetism to control brain functions.

One type of treatment is transcranial electrical stimulation (TES), which involves placing an electrode on the exterior of the scalp and delivering an electrical

current to the brain through the scalp and skull. Patents directed to TES include: U.S. Patent No. 5,540,736 issued to Haimovich et al. (for providing analgesia); U.S. Patent No. 4,140,133 issued to Katrubin et al. (for providing anesthesia); U.S. Patent No. 4,646,744 issued to Capel (for treating drug addiction, appetite disorders, stress, insomnia and pain); and U.S. Patent No. 4,844,075 issued to Liss et al. (for treating pain and motor dysfunction associated with cerebral palsy). TES, however, is not widely used because the patients experience a great amount of pain and the electrical field is difficult to direct or focus accurately.

Another type of treatment is transcranial magnetic stimulation (TMS), which involves producing a high-powered magnetic field adjacent to the exterior of the scalp over an area of the cortex. TMS does not cause the painful side effects of TES. Since 1985, TMS has been used primarily for research purposes in brain-mapping endeavors. Recently, however, potential therapeutic applications have been proposed primarily for the treatment of depression. A small number of clinical trials have found TMS to be effective in treating depression when used to stimulate the left prefrontal cortex.

The TMS treatment of a few other patient groups have been studied with promising results, such as patients with Parkinson's disease and hereditary spinocerebellar degeneration. Patents and published patent applications directed to TMS include: published international patent application WO 98/06342 (describing a transcranial magnetic stimulator and its use in brain mapping studies and in treating depression); U.S. Patent No. 5,885,976 issued to Sandyk (describing the use of transcranial magnetic stimulation to treat a variety of disorders allegedly related to deficient serotonin neurotransmission and impaired pineal melatonin functions); and U.S. Patent No. 5,092,835 issued to Schurig et al. (describing the treatment of neurological disorders (such as autism), treatment of learning disabilities, and augmentation of mental and physical abilities of "normal" people by a combination of transcranial magnetic stimulation and peripheral electrical stimulation).

Independent studies have also demonstrated that TMS is able to produce a lasting change in neural activity within the cortex that occurs for a period of time after terminating the TMS treatment ("neuroplasticity"). For example, Ziemann et al., *Modulation of Plasticity in Human Motor Cortex after Forearm Ischemic Nerve Block*, 18 J Neuroscience 1115 (February 1998), disclose that TMS at subthreshold

levels (e.g., levels at which movement was not induced) in neuro-block models that mimic amputation was able to modify the lasting changes in neural activity that normally accompany amputation. Similarly, Pascual-Leone et al. (submitted for publication) disclose that applying TMS over the contralateral motor cortex in normal subjects who underwent immobilization of a hand in a cast for 5 days can prevent the decreased motor cortex excitability normally associated with immobilization. Other researchers have proposed that the ability of TMS to produce desired changes in the cortex may someday be harnessed to enhance neuro-rehabilitation after a brain injury, such as stroke, but there are no published studies to date.

Other publications related to TMS include Cohen et al., *Studies of Neuroplasticity With Transcranial Magnetic Stimulation*, 15 J. Clin. Neurophysiol. 305 (1998); Pascual-Leone et al., *Transcranial Magnetic Stimulation and Neuroplasticity*, 37 Neuropsychologia 207 (1999); Stefan et al., *Induction of Plasticity in the Human Motor Cortex by Paired Associative Stimulation*, 123 Brain 572 (2000); Sievner et al., *Lasting Cortical Activation after repetitive TMS of the Motor Cortex*, 54 Neurology 956 (Feb. 2000); Pascual-Leone et al., *Study and Modulation of Human Cortical Excitability With Transcranial Magnetic Stimulation*, 15 J. Clin. Neurophysiol. 333 (1998); and Boylan et al., *Magnetolectric Brain Stimulation in the Assessment Of Brain Physiology And Pathophysiology*, 111 Clin. Neurophysiology 504 (2000).

Although TMS appears to be able to produce a change in the underlying cortex beyond the time of actual stimulation, TMS is not presently effective for treating many patients because the existing delivery systems are not practical for applying stimulation over an adequate period of time. TMS systems, for example, are relatively complex and require stimulation treatments to be performed by a healthcare professional in a hospital or physician's office. TMS systems also may not be reliable for longer-term therapies because it is difficult to (a) accurately localize the region of stimulation in a reproducible manner, and (b) hold the device in the correct position over the cranium for a long period, especially when a patient moves or during rehabilitation. Furthermore, current TMS systems generally do not sufficiently focus the electromagnetic energy on the desired region of the cortex for many applications. As such, the potential therapeutic benefit of TMS using existing equipment is relatively limited.

Direct and indirect electrical stimulation of the central nervous system has also been proposed to treat a variety of disorders and conditions. For example, U.S. Patent No. 5,938,688 issued to Schiff notes that the phenomenon of neuroplasticity may be harnessed and enhanced to treat cognitive disorders related to brain injuries caused by trauma or stroke. Schiff's implant is designed to increase the level of arousal of a comatose patient by stimulating deep brain centers involved in consciousness. To do this, Schiff's invention involves electrically stimulating at least a portion of the patient's intralaminar nuclei (*i.e.*, the deep brain) using, *e.g.*, an implantable multipolar electrode and either an implantable pulse generator or an external radiofrequency controlled pulse generator. Schiff's deep brain implant is highly invasive, however, and could involve serious complications for the patient.

Likewise, U.S. Patent No. 6,066,163 issued to John acknowledges the ability of the brain to overcome some of the results of an injury through neuroplasticity. John also cites a series of articles as evidence that direct electrical stimulation of the brain can reverse the effects of a traumatic injury or stroke on the level of consciousness. The system disclosed in John stimulates the patient and modifies the parameters of stimulation based upon the outcome of comparing the patient's present state with a reference state in an effort to optimize the results. Like Schiff, however, the invention disclosed in John is directed to a highly invasive deep brain stimulation system.

Another device for stimulating a region of the brain is disclosed by King in U.S. Patent No. 5,713,922. King discloses a device for cortical surface stimulation having electrodes mounted on a paddle implanted under the skull of the patient. The electrodes are implanted on the surface of the brain in a fixed position. The electrodes in King accordingly cannot move to accommodate changes in the shape of the brain. King also discloses that the electrical pulses are generated by a pulse generator that is implanted in the patient remotely from the cranium (*e.g.*, subclavicular implantation). The pulse generator is not directly connected to the electrodes, but rather it is electrically coupled to the electrodes by a cable that extends from the remotely implanted pulse generator to the electrodes implanted in the cranium. The cable disclosed in King extends from the paddle, around the skull, and down the neck to the subclavicular location of the pulse generator.

King discloses implanting the electrodes in contact with the surface of the cortex to create paresthesia, which is a sensation of vibration or “buzzing” in a patient. More specifically, King discloses inducing paresthesia in large areas by applying electrical stimulation to a higher element of the central nervous system (e.g., the cortex). As such, King discloses placing the electrodes against particular regions of the brain to induce the desired paresthesia. The purpose of creating paresthesia over a body region is to create a distracting stimulus that effectively reduces perception of pain in the body region. Thus, King appears to require stimulation above activation levels.

Although King discloses a device that stimulates a region on the cortical surface, this device is expected to have several drawbacks. First, it is expensive and time-consuming to implant the pulse generator and the cable in the patient. Second, it appears that the electrodes are held at a fixed elevation that does not compensate for anatomical changes in the shape of the brain relative to the skull, which makes it difficult to accurately apply an electrical stimulation to a desired target site of the cortex in a focused, specific manner. Third, King discloses directly activating the neurons to cause paresthesia, which is not expected to cause entrainment of the activity in the stimulated population of neurons with other forms of therapy or adaptive behavior, such as physical or occupational therapy. Thus, King is expected to have several drawbacks.

King and the other foregoing references are also expected to have drawbacks in producing the desired neural activity because these references generally apply the therapy to the region of the brain that is responsible for the physiological function or mental process according to the functional organization of the brain. In the case of a brain injury or disease, however, the region of the brain associated with the affected physiological function or cognitive process may not respond to stimulation therapies. Thus, existing techniques may not produce adequate results that last beyond the stimulation period.

## SUMMARY

The present invention is directed toward several apparatus and methods for effectuating a neural-function of a patient. One aspect of the invention is directed



toward an apparatus for effectuating a neural-function of a patient associated with a first location of the brain of the patient. The apparatus comprises a diagnostic system capable of identifying a stimulation site by determining a region of the brain where an intended neural activity is present in response to generating the intended neural activity remotely from the first location of the brain. This apparatus can also include a stimulation system including an electrode configured to be implanted at the stimulation site and a pulse generator to provide an electrical potential to the electrode.

Another aspect of the invention is directed toward an apparatus for treating a loss of a neural-function at a first cortical location in a brain of a patient. Several embodiments of this aspect of the invention include a diagnostic system capable of selecting a stimulation site at a cortical region of the brain where neural activity is expected to occur to compensate for the loss of neural-function at the first cortical location of the brain. These embodiments can also include a stimulation system having a first electrode and a second electrode. The stimulation system is generally configured to be implanted in the patient proximate to the pia matter in the cortical region, such that the first electrode is at a first area of the stimulation site, and the second electrode is at a second area of the stimulation site.

Another aspect of the invention is directed toward an apparatus for treating a neural-function in a brain of a patient. In this aspect, one embodiment includes a diagnostic system that determines an electrical stimulation threshold for inducing a response in cells at a stimulation site in the cortical region of the brain of the patient. This apparatus can also include a stimulation system having a first electrode, a second electrode, and a controller coupled to the first and second electrodes. The first and second electrodes are configured to be implanted proximate to the pia matter of the brain of the patient. The controller is configured to apply an electrical stimulation between the first and second electrodes at an intensity lower than the stimulation threshold. The controller, therefore, can apply stimulation at a sub-threshold intensity below the activation threshold for a population of neurons at the stimulation site.

Other aspects of apparatus in accordance with the invention are directed toward different features of stimulation systems. One aspect is directed toward an apparatus for applying electrical stimulation to a region of a brain of a patient. In one

embodiment, the apparatus includes an implantable support member configured to be implanted into the patient at least partially within the skull of the patient. This apparatus can also include a pulse system carried by the support member, a first electrode carried by the support member, and a second electrode that is also carried by the support member. The first and second electrodes are coupled to the pulse system.

Another embodiment is directed toward an apparatus that includes an implantable support member configured to be implanted into the patient proximate to the skull of the patient. The support member can include an attachment element to fix the support member to the skull. The apparatus can also include a pulse system carried by the support member, and first and second electrodes that are located in first and second regions of the support member, respectively. The first and second electrodes are coupled to the pulse system.

Other embodiments of apparatus in accordance with the invention have first and second electrodes that are coupled directly to the pulse system within the support member such that the stimulation system is an integrated unit that can be implanted completely within or on the skull of the patient. Other aspects include apparatus in which the support member has a biasing element, and the electrodes are carried by the biasing element.

Several aspects of methods in accordance with the invention are directed toward effectuating a neural-function of a patient. One embodiment of a method for effectuating a neural-function of a patient associated with a first location of the brain includes identifying a stimulation site by generating remotely from the first location an intended neural activity, and then determining a region of the brain where the generated neural activity is present. This method can continue by positioning at least a first electrode at the stimulation site, and then applying an electrical potential to pass a current through the first electrode.

Another embodiment of a method for effectuating a neural-function in a patient includes identifying a stimulation site in and/or on the brain where neural activity has changed in response to a change in the neural-function in the first location of the brain. This method can include positioning first and second electrodes at the stimulation site, and then applying an electrical potential between the first and second electrodes.

Other aspects of methods are directed toward methods for treating a loss of a neural-function at a first cortical location in the brain of a patient. One embodiment, for example, includes selecting a stimulation site at a cortical region of the brain where neural activity is expected to occur to compensate for the loss of neural-function at the first cortical location of the brain. These embodiments can further include positioning a first electrode at a first area of the stimulation site proximate to the pia matter in the cortical region, and also positioning a second electrode at a second area of the stimulation site proximate to the pia matter in the cortical region. The method can further include applying an electrical potential between the first and second electrodes.

Still additional aspects of methods in accordance with the invention are directed toward treating a neural-function in a brain of a patient using sub-threshold stimulation. In one embodiment, the method includes selecting a stimulation site in a first cortical region of the brain, and then determining an electrical stimulation threshold for inducing a response in cells at the stimulation site. This method further includes applying an electrical stimulation between the first and second electrodes at a location proximate to the pia matter of the first cortical region of the brain and at an intensity lower than the stimulation threshold.

## BRIEF DESCRIPTION OF THE DRAWINGS

Figure 1A is a schematic view of neurons.

Figure 1B is a graph illustrating firing an “action potential” associated with normal neural activity.

Figure 1C is a flowchart of a method for effectuating a neural-function of a patient associated with a location in the brain in accordance with one embodiment of the invention.

Figure 2 is a top plan view of a portion of a brain illustrating neural activity in a first region of the brain associated with the neural-function of the patient according to the somatotopic organization of the brain.

Figure 3 is a top plan image of a portion of the brain illustrating a loss of neural activity associated with the neural-function of the patient used in one stage of a method in accordance with an embodiment of the invention.

Figure 4 is a top plan image of the brain of Figure 3 showing a change in location of the neural activity associated with the neural-function of the patient at another stage of a method in accordance with an embodiment of the invention.

Figures 5A and 5B are schematic illustrations of an implanting procedure at a stage of a method in accordance with an embodiment of the invention.

Figure 5C is a graph illustrating firing an "action potential" associated with stimulated neural activity in accordance with one embodiment of the invention.

Figure 6 is an isometric view of an implantable stimulation apparatus in accordance with one embodiment of the invention.

Figure 7 is a cross-sectional view schematically illustrating a part of an implantable stimulation apparatus in accordance with an embodiment of the invention.

Figure 8 is a schematic illustration of a pulse system in accordance with one embodiment of the invention.

Figure 9 is a schematic illustration of an implanted stimulation apparatus and an external controller in accordance with an embodiment of the invention.

Figure 10 is a schematic illustration of an implantable stimulation apparatus having a pulse system and an external controller in accordance with another embodiment of the invention.

Figure 11 is a cross-sectional view schematically illustrating a part of an implantable stimulation apparatus in accordance with an embodiment of the invention.

Figure 12 is a schematic illustration of an implantable stimulation apparatus having a pulse system and an external controller in accordance with another embodiment of the invention.

Figure 13 is a cross-sectional view schematically illustrating a part of an implantable stimulation apparatus having a pulse system and an external controller in accordance with another embodiment of the invention.

Figure 14 is a bottom plan view and Figure 15 is a cross-sectional view illustrating an electrode configuration for an implantable stimulation apparatus in accordance with an embodiment of the invention.

Figure 16 is a bottom plan view and Figure 17 is a cross-sectional view of an electrode configuration for an implantable stimulation apparatus in accordance with another embodiment of the invention.

Figure 18 is a bottom plan view and Figure 19 is a cross-sectional view of an electrode configuration in accordance with yet another embodiment of the invention.

Figure 20 is a bottom plan view of an electrode configuration for an implantable stimulation device in accordance with yet another embodiment of the invention.

Figure 21 is a bottom plan view of an electrode configuration for an implantable stimulation device in accordance with another embodiment of the invention.

Figure 22 is a bottom plan view of yet another embodiment of an electrode configuration for use with an implantable stimulation apparatus in accordance with the invention.

Figure 23 is a bottom plan view and Figure 24 is a cross-sectional view of an electrode configuration for use with a stimulation apparatus in accordance with still another embodiment of the invention.

Figure 25 is an isometric view schematically illustrating a part of an implantable stimulation apparatus with a mechanical biasing element in accordance with an embodiment of the invention.

Figure 26 is a cross-sectional view of a stimulation apparatus having a mechanical biasing element that has been implanted into a skull of a patient in accordance with an embodiment of the invention.

Figure 27 is a cross-sectional view schematically illustrating a part of a stimulation apparatus having a biasing element in accordance with an embodiment of the invention.

Figure 28 is a cross-sectional view of a stimulation apparatus having a biasing element in accordance with still another embodiment of the invention.

Figure 29 is a cross-sectional view of a stimulation apparatus having a biasing element in accordance with yet another embodiment of the invention.

Figure 30 is a cross-sectional view of a stimulation apparatus having a biasing element in accordance with yet another embodiment of the invention.

Figure 31 is a cross-sectional view schematically illustrating a portion of an implantable stimulation apparatus having an external power source and pulse generator in accordance with an embodiment of the invention.

Figure 32 is a cross-sectional view schematically illustrating a portion of an implantable stimulation apparatus having an external power source and pulse generator in accordance with another embodiment of the invention.

Figure 33 is a cross-sectional view illustrating in greater detail a portion of the implantable stimulation apparatus of Figure 32.

Figure 34 is a cross-sectional view schematically illustrating a portion of an implantable stimulation apparatus and an external controller in accordance with another embodiment of the invention.

Figure 35 is a cross-sectional view schematically illustrating a portion of an implantable stimulation apparatus and an external controller in accordance with yet another embodiment of the invention.

Figure 36 is a cross-sectional view schematically illustrating a portion of an implantable stimulation apparatus in accordance with yet another embodiment of the invention.

Figure 37 is an isometric view and Figure 38 is a cross-sectional view illustrating an implantable stimulation apparatus in accordance with an embodiment of the invention.

Figure 39 is a cross-sectional view illustrating an implantable stimulation apparatus in accordance with yet another embodiment of the invention.

Figure 40 is a schematic illustration of an implantable stimulation apparatus in accordance with an embodiment of the invention.

## DETAILED DESCRIPTION

The following disclosure describes several methods and apparatus for intracranial electrical stimulation to treat or otherwise effectuate a change in neural-functions of a patient. Several embodiments of methods in accordance with the invention are directed toward enhancing or otherwise inducing neuroplasticity to effectuate a particular neural-function. Neuroplasticity refers to the ability of the brain to change or adapt over time. It was once thought adult brains became relatively "hard wired" such that functionally significant neural networks could not change significantly over time or in response to injury. It has become increasingly more apparent that these neural networks can change and adapt over time so that meaningful

function can be regained in response to brain injury. An aspect of several embodiments of methods in accordance with the invention is to provide the appropriate triggers for adaptive neuroplasticity. These appropriate triggers appear to cause or enable increased synchrony of functionally significant populations of neurons in a network.

Electrically enhanced or induced neural stimulation in accordance with several embodiments of the invention excites a portion of a neural network involved in a functionally significant task such that a selected population of neurons can become more strongly associated with that network. Because such a network will subserve a functionally meaningful task, such as motor relearning, the changes are more likely to be lasting because they are continually being reinforced by natural use mechanisms. The nature of stimulation in accordance with several embodiments of the invention ensures that the stimulated population of neurons links to other neurons in the functional network. It is expected that this occurs because action potentials are not actually caused by the stimulation, but rather are caused by interactions with other neurons in the network. Several aspects of the electrical stimulation in accordance with selected embodiments of the invention simply allows this to happen with an increased probability when the network is activated by favorable activities, such as rehabilitation or limb use.

The methods in accordance with the invention can be used to treat brain damage (*e.g.*, stroke, trauma, etc.), brain disease (*e.g.*, Alzheimer's, Pick's, Parkinson's, etc.), and/or brain disorders (*e.g.*, epilepsy, depression, etc.). The methods in accordance with the invention can also be used to enhance functions of normal, healthy brains (*e.g.*, learning, memory, etc.), or to control sensory functions (*e.g.*, pain).

Certain embodiments of methods in accordance with the invention electrically stimulate the brain at a stimulation site where neuroplasticity is occurring. The stimulation site may be different than the region in the brain where neural activity is typically present to perform the particular function according to the functional organization of the brain. In one embodiment in which neuroplasticity related to the neural-function occurs in the brain, the method can include identifying the location where such neuroplasticity is present. This particular procedure may accordingly enhance a change in the neural activity to assist the brain in performing the particular

neural function. In an alternative embodiment in which neuroplasticity is not occurring in the brain, an aspect is to induce neuroplasticity at a stimulation site where it is expected to occur. This particular procedure may thus induce a change in the neural activity to instigate performance of the neural function.. Several embodiments of these methods are expected to produce a lasting effect on the intended neural activity at the stimulation site.

The specific details of certain embodiments of the invention are set forth in the following description and in Figures 1A-40 to provide a thorough understanding of these embodiments to a person of ordinary skill in the art. More specifically, several embodiments of methods in accordance with the invention are initially described with reference to Figures 1-5C, and then several embodiments of devices for stimulating the cortical and/or deep-brain regions of the brain are described with reference to Figures 6-40. A person skilled in the art will understand that the present invention may have additional embodiments, or that the invention can be practiced without several of the details described below.

A. Methods for Electrically Stimulating Regions of the Brain

1. Embodiments of Electrically Enhancing Neural Activity

Figure 1A is a schematic representation of several neurons N1-N3 and Figure 1B is a graph illustrating an “action potential” related to neural activity in a normal neuron. Neural activity is governed by electrical impulses generated in neurons. For example, neuron N1 can send excitatory inputs to neuron N2 (*e.g.*, times  $t_1$ ,  $t_3$  and  $t_4$  in Figure 1B), and neuron N3 can send inhibitory inputs to neuron N2 (*e.g.*, time  $t_2$  in Figure 1B). The neurons receive/send excitatory and inhibitory inputs from/to a population of other neurons. The excitatory and inhibitory inputs can produce “action potentials” in the neurons, which are electrical pulses that travel through neurons by changing the flux of sodium (Na) and potassium (K) ions across the cell membrane. An action potential occurs when the resting membrane potential of the neuron surpasses a threshold level. When this threshold level is reached, an “all-or-nothing” action potential is generated. For example, as shown in Figure 1B, the excitatory input at time  $t_3$  causes neuron N2 to “fire” an action potential because the input exceeds the threshold level for generating the action potential. The action



potentials propagate down the length of the axon (the long process of the neuron that makes up nerves or neuronal tracts) to cause the release of neurotransmitters from that neuron that will further influence adjacent neurons.

Figure 1C is a flowchart illustrating a method 100 for effectuating a neural-function in a patient in accordance with an embodiment of the invention. The neural-function, for example, can control a specific mental process or physiological function, such as a particular motor function or sensory function (*e.g.*, movement of a limb) that is normally associated with neural activity at a “normal” location in the brain according to the functional organization of the brain. In several embodiments of the method 100, at least some neural activity related to the neural-function can be occurring at a site in the brain. The site of the neural activity may be at the normal location where neural activity typically occurs to carry out the neural-function according to the functional organization of the brain, or the site of the neural activity may be at a different location where the brain has recruited material to perform the neural activity. In either situation, one aspect of several embodiments of the method 100 is to determine the location in the brain where this neural activity is present.

The method 100 includes a diagnostic procedure 102 involving identifying a stimulation site at a location of the brain where an intended neural activity related to the neural-function is present. In one embodiment, the diagnostic procedure 102 includes generating the intended neural activity in the brain from a “peripheral” location that is remote from the normal location, and then determining where the intended neural activity is actually present in the brain. In an alternative embodiment, the diagnostic procedure 102 can be performed by identifying a stimulation site where neural activity has changed in response to a change in the neural-function. The method 100 continues with an implanting procedure 104 involving positioning first and second electrodes at the identified stimulation site, and a stimulating procedure 106 involving applying an electrical current between the first and second electrodes. Many embodiments of the implanting procedure 104 position two or more electrodes at the stimulation site, but other embodiments of the implanting procedure involve positioning only one electrode at the stimulation site and another electrode remotely from the stimulation site. As such, the implanting procedure 104 of the method 100 can include implanting at least one electrode at the stimulation site. The procedures 102-106 are described in greater detail below.

Figures 2-4 illustrate an embodiment of the diagnostic procedure 102. The diagnostic procedure 102 can be used to determine the region of the brain where stimulation will likely effectuate the desired function, such as rehabilitating a loss of a neural-function caused by a stroke, trauma, disease or other circumstance. Figure 2, more specifically, is an image of a normal, healthy brain 200 having a first region 210 where the intended neural activity occurs to effectuate a specific neural-function in accordance with the functional organization of the brain. For example, the neural activity in the first region 210 shown in Figure 2 is generally associated with the movement of a patient's fingers. The first region 210 can have a high-intensity area 212 and a low-intensity area 214 in which different levels of neural activity occur. It is not necessary to obtain an image of the neural activity in the first region 210 shown in Figure 2 to carry out the diagnostic procedure 102, but rather it is provided to show an example of neural activity that typically occurs at a "normal location" according to the functional organization of the brain 200 for a large percentage of people with normal brain function. It will be appreciated that the actual location of the first region 210 will generally vary between individual patients.

The neural activity in the first region 210, however, can be impaired. In a typical application, the diagnostic procedure 102 begins by taking an image of the brain 200 that is capable of detecting neural activity to determine whether the intended neural activity associated with the particular neural function of interest is occurring at the region of the brain 200 where it normally occurs according to the functional organization of the brain. Figure 3 is an image of the brain 200 after the first region 210 has been affected (*e.g.*, from a stroke, trauma or other cause). As shown in Figure 3, the neural activity that controlled the neural-function for moving the fingers no longer occurs in the first region 210. The first region 210 is thus "inactive," which is expected to result in a corresponding loss of the movement and/or sensation in the fingers. In some instances, the damage to the brain 200 may result in only a partial loss of the neural activity in the damaged region. In either case, the image shown in Figure 3 establishes that the loss of the neural-function is related to the diminished neural activity in the first region 210. The brain 200 may accordingly recruit other neurons to perform neural activity for the affected neural-function (*i.e.*, neuroplasticity), or the neural activity may not be present at any location in the brain.

Figure 4 is an image of the brain 200 illustrating a plurality of potential stimulation sites 220 and 230 for effectuating the neural-function that was originally performed in the first region 210 shown in Figure 2. Figures 3 and 4 show an example of neuroplasticity in which the brain compensates for a loss of neural-function in one region of the brain by recruiting other regions of the brain to perform neural activity for carrying out the affected neural-function. The diagnostic procedure 102 utilizes the neuroplasticity that occurs in the brain to identify the location of a stimulation site that is expected to be more responsive to the results of an electrical, magnetic, sonic, genetic, biologic, and/or pharmaceutical procedure to effectuate the desired neural-function.

One embodiment of the diagnostic procedure 102 involves generating the intended neural activity remotely from the first region 210 of the brain, and then detecting or sensing the location in the brain where the intended neural activity has been generated. The intended neural activity can be generated by applying an input that causes a signal to be sent to the brain. For example, in the case of a patient that has lost the use of limb, the affected limb is moved and/or stimulated while the brain is scanned using a known imaging technique that can detect neural activity (*e.g.*, functional MRI, positron emission tomography, etc.). In one specific embodiment, the affected limb can be moved by a practitioner or the patient, stimulated by sensory tests (*e.g.*, pricking), or subject to peripheral electrical stimulation. The movement/stimulation of the affected limb produces a peripheral neural signal from the limb that is expected to generate a response neural activity in the brain. The location in the brain where this response neural activity is present can be identified using the imaging technique. Figure 4, for example, can be created by moving the affected fingers and then noting where neural activity occurs in response to the peripheral stimulus. By peripherally generating the intended neural activity, this embodiment may accurately identify where the brain has recruited matter (*i.e.*, sites 220 and 230) to perform the intended neural activity associated with the neural-function.

An alternative embodiment of the diagnostic procedure 102 involves identifying a stimulation site at a second location of the brain where the neural activity has changed in response to a change in the neural-function of the patient. This embodiment of the method does not necessarily require that the intended neural

activity be generated by peripherally actuating or stimulating a body part. For example, the brain can be scanned for neural activity associated with the impaired neural-function as a patient regains use of an affected limb or learns a task over a period of time. This embodiment, however, can also include peripherally generating the intended neural activity remotely from the brain explained above.

In still another embodiment, the diagnostic procedure 102 involves identifying a stimulation site at a location of the brain where the intended neural activity is developing to perform the neural-function. This embodiment is similar to the other embodiments of the diagnostic procedure 102, but it can be used to identify a stimulation site at (a) the normal region of the brain where the intended neural activity is expected to occur according to the functional organization of the brain and/or (b) a different region where the neural activity occurs because the brain is recruiting additional matter to perform the neural-function. This particular embodiment of the method involves monitoring neural activity at one or more locations where the neural activity occurs in response to the particular neural-function of interest. For example, to enhance the ability to learn a particular task (*e.g.*, playing a musical instrument, memorizing, etc.), the neural activity can be monitored while a person performs the task or thinks about performing the task. The stimulation sites can be defined by the areas of the brain where the neural activity has the highest intensity, the greatest increases, and/or other parameters that indicate areas of the brain that are being used to perform the particular task.

Figures 5A and 5B are schematic illustrations of the implanting procedure 104 described above with reference to Figure 1C for positioning the first and second electrodes relative to a portion of the brain of a patient 500. Referring to Figure 5A, a stimulation site 502 is identified in accordance with an embodiment of the diagnostic procedure 102. In one embodiment, a skull section 504 is removed from the patient 500 adjacent to the stimulation site 502. The skull section 504 can be removed by boring a hole in the skull in a manner known in the art, or a much smaller hole can be formed in the skull using drilling techniques that are also known in the art. In general, the hole can be 0.2-4.0 cm in diameter. Referring to Figure 5B, an implantable stimulation apparatus 510 having first and second electrodes 520 can be implanted in the patient 500. Suitable techniques associated with the implantation procedure are known to practitioners skilled in the art. After the stimulation apparatus

510 has been implanted in the patient 500, a pulse system generates electrical pulses that are transmitted to the stimulation site 502 by the first and second electrodes 520. Stimulation apparatus suitable for carrying out the foregoing embodiments of methods in accordance with the invention are described in more detail below with reference to the Figures 6-40.

Several embodiments of methods for enhancing neural activity in accordance with the invention are expected to provide lasting results that promote the desired neural-function. Before the present invention, electrical and magnetic stimulation techniques typically stimulated the normal locations of the brain where neural activity related to the neural-functions occurred according to the functional organization of the brain. Such conventional techniques, however, may not be effective because the neurons in the "normal locations" of the brain may not be capable of carrying out the neural activity because of brain damage, disease, disorder, and/or because of variations of the location specific to individual patients. Several embodiments of methods for enhancing neural activity in accordance with the invention overcome this drawback by identifying a stimulation site based on neuroplastic activity that appears to be related to the neural-function. By first identifying a location in the brain that is being recruited to perform the neural activity, it is expected that therapies (e.g., electrical, magnetic, genetic, biologic, and/or pharmaceutical) applied to this location will be more effective than conventional techniques. This is because the location that the brain is recruiting for the neural activity may not be the "normal location" where the neuro activity would normally occur according to the functional organization of the brain. Therefore, several embodiments of methods for enhancing neural activity in accordance with the invention are expected to provide lasting results because the therapies are applied to the portion of the brain where neural activity for carrying out the neural-function actually occurs in the particular patient.

## 2. Electrically Inducing Desired Neural activity

The method 100 for effectuating a neural-function can also be used to induce neural activity in a region of the brain where such neural activity is not present. As opposed to the embodiments of the method 100 described above for enhancing

existing neural activity, the embodiments of the method 100 for inducing neural activity initiate the neural activity at a stimulation site where it is estimated that neuroplasticity will occur. In this particular situation, an image of the brain seeking to locate where neuroplasticity is occurring may be similar to Figure 3. An aspect of inducing neural activity, therefore, is to develop a procedure to determine where neuroplasticity is likely to occur.

A stimulation site may be identified by estimating where the brain will likely recruit neurons for performing the neural-function. In one embodiment, the location of the stimulation site is estimated by defining a region of the brain that is proximate to the normal location where neural activity related to the neural-function is generally present according to the functional organization of the brain. An alternative embodiment for locating the stimulation site includes determining where neuroplasticity has typically occurred in patients with similar symptoms. For example, if the brain typically recruits a second region of the cortex to compensate for a loss of neural activity in the normal region of the cortex, then the second region of the cortex can be selected as the stimulation site either with or without imaging the neural activity in the brain.

Several embodiments of methods for inducing neural activity in accordance with the invention are also expected to provide lasting results that initiate and promote a desired neural-function. By first estimating the location of a stimulation site where desired neuroplasticity is expected to occur, therapies applied to this location may be more effective than conventional therapies for reasons that are similar to those explained above regarding enhancing neural activity. Additionally, methods for inducing neural activity may be easier and less expensive to implement because they do not require generating neural activity and/or imaging the brain to determine where the intended neural activity is occurring before applying the therapy.

### 3. Applications of Methods for Electrically Stimulating Regions of the Brain

The foregoing methods for enhancing existing neural activity or inducing new neural activity are expected to be useful for many applications. As explained above, several embodiments of the method 100 involve determining an efficacious location of the brain to enhance or induce an intended neural activity that

causes the desired neural-functions to occur. Additional therapies can also be implemented in combination with the electrical stimulation methods described above. Several specific applications using embodiments of electrical stimulation methods in accordance with the invention either alone or with adjunctive therapies will now be described, but it will be appreciated that the methods in accordance with the invention can be used in many additional applications.

a. General Applications

The embodiments of the electrical stimulation methods described above are expected to be particularly useful for rehabilitating a loss of mental functions, motor functions and/or sensory functions caused by damage to the brain. In a typical application, the brain has been damaged by a stroke or trauma (*e.g.*, automobile accident). The extent of the particular brain damage can be assessed using functional MRI or another appropriate imaging technique as explained above with respect to Figure 3. A stimulation site can then be identified by: (a) peripherally stimulating a body part that was affected by the brain damage to induce the intended neural activity and determining the location where a response neural activity occurs; (b) determining where the neural activity has changed as a patient gains more use of the affected body part; and/or (c) estimating the location that the brain may recruit neurons to carry out the neural activity that was previously performed by the damaged portion of the brain. An electrical stimulation therapy can then be applied to the selected stimulation site by placing the first and second electrodes relative to the stimulation site to apply an electrical current in that portion of the brain. As explained in more detail below, it is expected that applying an electrical current to the portion of the brain that has been recruited to perform the neural activity related to the affected body part will produce a lasting neurological effect for rehabilitating the affected body part.

Several specific applications are expected to have a stimulation site in the cortex because neural activity in this part of the brain effectuates motor functions and/or sensory functions that are typically affected by a stroke or trauma. In these applications, the electrical stimulation can be applied directly to the pial surface of the brain or at least proximate to the pial surface (*e.g.*, the dura mater, the fluid surrounding the cortex, or neurons within the cortex). Suitable devices for applying

the electrical stimulation to the cortex are described in detail with reference to Figures 6-40.

The electrical stimulation methods can also be used with adjunctive therapies to rehabilitate damaged portions of the brain. In one embodiment, the electrical stimulation methods can be combined with physical therapy and/or drug therapies to rehabilitate an affected neural function. For example, if a stroke patient has lost the use of a limb, the patient can be treated by applying the electrical therapy to a stimulation site where the intended neural activity is present while the affected limb is also subject to physical therapy. An alternative embodiment can involve applying the electrical therapy to the stimulation site and chemically treating the patient using amphetamines or other suitable drugs.

The embodiments of the electrical stimulation methods described above are also expected to be useful for treating brain diseases, such as Alzheimer's, Parkinson's, and other brain diseases. In this application, the stimulation site can be identified by monitoring the neural activity using functional MRI or other suitable imaging techniques over a period of time to determine where the brain is recruiting material to perform the neural activity that is being affected by the disease. It may also be possible to identify the stimulation site by having the patient try to perform an act that the particular disease has affected, and monitoring the brain to determine whether any response neural activity is present in the brain. After identifying where the brain is recruiting additional matter, the electrical stimulation can be applied to this portion of the brain. It is expected that electrically stimulating the regions of the brain that have been recruited to perform the neural activity which was affected by the disease will assist the brain in offsetting the damage caused by the disease.

The embodiments of the electrical stimulation methods described above are also expected to be useful for treating neurological disorders, such as depression, passive-aggressive behavior, weight control, and other disorders. In these applications, the electrical stimulation can be applied to a stimulation site in the cortex or another suitable part of the brain where neural activity related to the particular disorder is present. The embodiments of electrical stimulation methods for carrying out the particular therapy can be adapted to either increase or decrease the particular neural activity in a manner that produces the desired results. For example, an amputee may feel phantom sensations associated with the amputated limb. This phenomenon



can be treated by applying an electrical pulse that reduces the phantom sensations. The electrical therapy can be applied so that it will modulate the ability of the neurons in that portion of the brain to execute sensory functions.

b. Pulse Forms and Potentials

The electrical stimulation methods in accordance with the invention can use several different pulse forms to effectuate the desired neuroplasticity. The pulses can be a bi-phasic or monophasic stimulus that is applied to achieve a desired potential in a sufficient percentage of a population of neurons at the stimulation site. In one embodiment, the pulse form has a frequency of approximately 2-1000 Hz, but the frequency may be particularly useful in the range of approximately 40-200 Hz. For example, initial clinical trials are expected to use a frequency of approximately 50-100 Hz. The pulses can also have pulse widths of approximately 10 $\mu$ s-100ms, or more specifically the pulse width can be approximately 20-200 $\mu$ s. For example, a pulse width of 50-100 $\mu$ s may produce beneficial results.

It is expected that one particularly useful application of the invention involves enhancing or inducing neuroplasticity by raising the resting membrane potential of neurons to bring the neurons closer to the threshold level for firing an action potential. Because the stimulation raises the resting membrane potential of the neurons, it is expected that these neurons are more likely to “fire” an action potential in response to excitatory input at a lower level.

Figure 5C is a graph illustrating applying a subthreshold potential to the neurons N1-N3 of Figure 1A. At times  $t_1$  and  $t_2$ , the excitory/inhibitory inputs from other neurons do not “bridge-the-gap” from the resting potential at -X mV to the threshold potential. At time  $t_3$ , the electrical stimulation is applied to the brain to raise the resting potential of neurons in the stimulated population such that the resting potential is at -Y mV. As such, at time  $t_4$  when the neurons receive another excitatory input, even a small input exceeds the gap between the raised resting potential -Y mV and the threshold potential to induce action potentials in these neurons. For example, if the resting potential is approximately -70 mV and the threshold potential is approximately -50 mV, then the electrical stimulation can be applied to raise the resting potential of a sufficient number of neurons to approximately -52 to -60 mV.

The actual electrical potential applied to electrodes implanted in the brain to achieve a subthreshold potential stimulation will vary according to the individual patient, the type of therapy, the type of electrodes, and other factors. In general, the pulse form of the electrical stimulation (*e.g.*, the frequency, pulse width, wave form, and voltage potential) is selected to raise the resting potential in a sufficient number neurons at the stimulation site to a level that is less than a threshold potential for a statistical portion of the neurons in the population. The pulse form, for example, can be selected so that the applied voltage of the stimulus achieves a change in the resting potential of approximately 10%-95%, and more specifically of 60%-80%, of the difference between the unstimulated resting potential and the threshold potential.

In one specific example of a subthreshold application for treating a patient's hand, electrical stimulation is not initially applied to the stimulation site. Although physical therapy related to the patient's hand may cause some activation of a particular population of neurons that is known to be involved in "hand function," only a low level of activation might occur because physical therapy only produces a low level of action potential generation in that population of neurons. However, when the subthreshold electrical stimulation is applied, the resting membrane potentials of the neurons in the stimulated population are elevated. These neurons now are much closer to the threshold for action potential formation such that when the same type of physical therapy is given, this population of cells will have a higher level of activation because these cells are more likely to fire action potentials.

Subthreshold stimulation may produce better results than simply stimulating the neurons with sufficient energy levels to exceed the threshold for action potential formation. One aspect of subthreshold stimulation is to increase the probability that action potentials will occur in response to the ordinary causes of activation – such as physical therapy. This will allow the neurons in this functional network to become entrained together, or "learn" to become associated with these types of activities. If neurons are given so much electricity that they continually fire action potentials without additional excitatory inputs (suprathreshold stimulation), this will create "noise" and disorganization that will not likely cause improvement in function. In fact, neurons that are "overdriven" soon deplete their neurotransmitters and effectively become silent.

The application of a subthreshold stimulation is very different than suprathreshold stimulation. Subthreshold stimulation in accordance with several embodiments of the invention, for example, does not intend to directly make neurons fire action potentials with the electrical stimulation in a significant population of neurons at the stimulation site. Instead, subthreshold stimulation attempts to decrease the "activation energy" required to activate a large portion of the neurons at the stimulation site. As such, subthreshold stimulation in accordance with certain embodiments of the invention is expected to increase the probability that the neurons will fire in response to the usual intrinsic triggers, such as trying to move a limb, physical therapy, or simply thinking about movement of a limb, etc. Moreover, coincident stimulation associated with physical therapy is expected to increase the probability that the action potentials that are occurring with an increased probability due to the subthreshold stimulation will be related to meaningful triggers, and not just "noise."

The stimulus parameters set forth above, such as a frequency selection of approximately 50-100 Hz and an amplitude sufficient to achieve an increase of 60% to 80% of the difference between the resting potential and the threshold potential are specifically selected so that they will increase the resting membrane potential of the neurons, thereby increasing the likelihood that they will fire action potentials, without directly causing action potentials in most of the neuron population. In addition, and as explained in more detail below with respect to Figures 6-40, several embodiments of stimulation apparatus in accordance with the invention are designed to precisely apply a pulse form that produces subthreshold stimulation by selectively stimulating regions of the cerebral cortex of approximately 1-2 cm (the estimated size of a "functional unit" of cortex), directly contacting the pial surface with the electrodes to consistently create the same alterations in resting membrane potential, and/or biasing the electrodes against the pial surface to provide a positive connection between the electrodes and the cortex.

#### B. Devices for Electrically Stimulating Regions of the Brain

Figures 6-40 illustrate stimulation apparatus in accordance with several embodiments of the invention for electrically stimulating regions of the brain in

accordance with one or more of the methods described above. The devices illustrated in Figures 6-40 are generally used to stimulate a region of the cortex proximate to the pial surface of the brain (*e.g.*, the dura mater, the pia mater, the fluid between the dura mater and the pia mater, and a depth in the cortex outside of the white matter of the brain). The devices can also be adapted for stimulating other portions of the brain in other embodiments.

1. Implantable Stimulation Apparatus with Integrated Pulse Systems

Figure 6 is an isometric view and Figure 7 is a cross-sectional view of a stimulation apparatus 600 in accordance with an embodiment of the invention for stimulating a region of the cortex proximate to the pial surface. In one embodiment, the stimulation apparatus 600 includes a support member 610, an integrated pulse-system 630 (shown schematically) carried by the support member 610, and first and second electrodes 660 (identified individually by reference numbers 660a and 660b). The first and second electrodes 660 are electrically coupled to the pulse system 630. The support member 610 can be configured to be implanted into the skull or another intracranial region of a patient. In one embodiment, for example, the support member 610 includes a housing 612 and an attachment element 614 connected to the housing 612. The housing 612 can be a molded casing formed from a biocompatible material that has an interior cavity for carrying the pulse system 630. The housing can alternatively be a biocompatible metal or another suitable material. The housing 612 can have a diameter of approximately 1-4 cm, and in many applications the housing 612 can be 1.5-2.5 cm in diameter. The housing 612 can also have other shapes (*e.g.*, rectilinear, oval, elliptical) and other surface dimensions. The stimulation apparatus 600 can weigh 35g or less and/or occupy a volume of 20cc or less. The attachment element 614 can be a flexible cover, a rigid plate, a contoured cap, or another suitable element for holding the support member 610 relative to the skull or other body part of the patient. In one embodiment, the attachment element 614 is a mesh, such as a biocompatible polymeric mesh, metal mesh, or other suitable woven material. The attachment element 614 can alternatively be a flexible sheet of Mylar, a polyester, or another suitable material.

Figure 7, more specifically, is a cross-sectional view of the stimulation apparatus 600 after it has been implanted into a patient in accordance with an embodiment of the invention. In this particular embodiment, the stimulation apparatus 600 is implanted into the patient by forming an opening in the scalp 702 and cutting a hole 704 through the skull 700 and through the dura mater 706. The hole 704 should be sized to receive the housing 612 of the support member 610, and in most applications, the hole 704 should be smaller than the attachment element 614. A practitioner inserts the support member 610 into the hole 704 and then secures the attachment element 614 to the skull 700. The attachment element 614 can be secured to the skull using a plurality of fasteners 618 (*e.g.*, screws, spikes, etc.) or an adhesive. In an alternative embodiment, a plurality of downwardly depending spikes can be formed integrally with the attachment element 614 to define anchors that can be driven into the skull 700.

The embodiment of the stimulation apparatus 600 shown in Figure 7 is configured to be implanted into a patient so that the electrodes 660 contact a desired portion of the brain at the stimulation site. The housing 612 and the electrodes 660 can project from the attachment element 614 by a distance "D" such that the electrodes 660 are positioned at least proximate to the pia mater 708 surrounding the cortex 709. The electrodes 660 can project from a housing 612 as shown in Figure 7, or the electrodes 660 can be flush with the interior surface of the housing 612. In the particular embodiment shown in Figure 7, the housing 612 has a thickness "T" and the electrodes 660 project from the housing 612 by a distance "P" so that the electrodes 660 press against the surface of the pia mater 708. The thickness of the housing 612 can be approximately 0.5-4 cm, and is more generally about 1-2 cm. The configuration of the stimulation apparatus 600 is not limited to the embodiment shown in Figures 6 and 7, but rather the housing 612, the attachment element 614, and the electrodes 660 can be configured to position the electrodes in several different regions of the brain. For example, in an alternate embodiment, the housing 612 and the electrodes 660 can be configured to position the electrodes deep within the cortex 709, and/or a deep brain region 710. In general, the electrodes can be flush with the housing or extend 0.1 mm to 5 cm from the housing. More specific embodiments of pulse system and electrode configurations for the stimulation apparatus will be described below.

Several embodiments of the stimulation apparatus 600 are expected to be more effective than existing transcranial electrical stimulation devices and transcranial magnetic stimulation devices. It will be appreciated that much of the power required for transcranial therapies is dissipated in the scalp and skull before it reaches the brain. In contrast to conventional transcranial stimulation devices, the stimulation apparatus 600 is implanted so that the electrodes are at least proximate to the pial surface of the brain 708. Several embodiments of methods in accordance with the invention can use the stimulation apparatus 600 to apply an electrical therapy directly to the pia mater 708, the dura mater 706, and/or another portion of the cortex 709 at significantly lower power levels than existing transcranial therapies. For example, a potential of approximately 1 mV to 10 V can be applied to the electrodes 660; in many instances a potential of 100 mV to 5 V can be applied to the electrodes 660 for selected applications. It will also be appreciated that other potentials can be applied to the electrodes 660 of the stimulation apparatus 600 in accordance with other embodiments of the invention.

Selected embodiments of the stimulation apparatus 600 are also capable of applying stimulation to a precise stimulation site. Again, because the stimulation apparatus 600 positions the electrodes 660 at least proximate to the pial surface 708, precise levels of stimulation with good pulse shape fidelity will be accurately transmitted to the stimulation site in the brain. It will be appreciated that transcranial therapies may not be able to apply stimulation to a precise stimulation site because the magnetic and electrical properties of the scalp and skull may vary from one patient to another such that an identical stimulation by the transcranial device may produce a different level of stimulation at the neurons in each patient. Moreover, the ability to focus the stimulation to a precise area is hindered by delivering the stimulation transcranially because the scalp, skull and dura all diffuse the energy from a transcranial device. Several embodiments of the stimulation apparatus 600 overcome this drawback because the electrodes 660 are positioned under the skull 700 such that the pulses generated by the stimulation apparatus 600 are not diffused by the scalp 702 and skull 700.

## 2. Integrated Pulse Systems for Implantable Stimulation Apparatus

The pulse system 630 shown in Figures 6 and 7 generates and/or transmits electrical pulses to the electrodes 660 to create an electrical field at a stimulation site in a region of the brain. The particular embodiment of the pulse system 630 shown in Figure 7 is an "integrated" unit in that is carried by the support member 610. The pulse system 630, for example, can be housed within the housing 612 so that the electrodes 660 can be connected directly to the pulse system 630 without having leads outside of the stimulation apparatus 600. The distance between the electrodes 660 and the pulse system 630 can be less than 4 cm, and it is generally 0.10 to 2.0 cm. The stimulation apparatus 600 can accordingly provide electrical pulses to the stimulation site without having to surgically create tunnels running through the patient to connect the electrodes 660 to a pulse generator implanted remotely from the stimulation apparatus 600. It will be appreciated, however, that alternative embodiments of stimulation apparatus in accordance with the invention can include a pulse system implanted separately from the stimulation apparatus 600 in the cranium or an external pulse system. Several particular embodiments of pulse systems that are suitable for use with the stimulation apparatus 600 will now be described in more detail.

Figures 8 and 9 schematically illustrate an integrated pulse system 800 in accordance with one embodiment of the invention for being implanted in the cranium within the stimulation apparatus 600. Referring to Figure 8, the pulse system 800 can include a power supply 810, an integrated controller 820, a pulse generator 830, and a pulse transmitter 840. The power supply 810 can be a primary battery, such as a rechargeable battery or another suitable device for storing electrical energy. In alternative embodiments, the power supply 810 can be an RF transducer or a magnetic transducer that receives broadcast energy emitted from an external power source and converts the broadcast energy into power for the electrical components of the pulse system 800. The integrated controller 820 can be a wireless device that responds to command signals sent by an external controller 850. The integrated controller 820, for example, can communicate with the external controller 850 by RF or magnetic links 860. The integrated controller 820 provides control signals to the

pulse generator 830 in response to the command signals sent by the external controller 850. The pulse generator 830 can have a plurality of channels that send appropriate electrical pulses to the pulse transmitter 840, which is coupled to the electrodes 660. Suitable components for the power supply 810, the integrated controller 820, the pulse generator 830, and the pulse transmitter 840 are known to persons skilled in the art of implantable medical devices.

Referring to Figure 9, the pulse system 800 can be carried by the support member 610 of the stimulation apparatus 600 in the manner described above with reference to Figures 6 and 7. The external controller 850 can be located externally to the patient 500 so that the external controller 850 can be used to control the pulse system 800. In one embodiment, several patients that require a common treatment can be simultaneously treated using a single external controller 850 by positioning the patients within the operating proximity of the controller 850. In an alternative embodiment, the external controller 850 can contain a plurality of operating codes and the integrated controller 820 for a particular patient can have an individual operating code. A single controller 850 can thus be used to treat a plurality of different patients by entering the appropriate operating code into the controller 850 corresponding to the particular operating codes of the integrated controllers 820 for the patients.

Figure 10 is a schematic view illustrating a pulse system 1000 and an external controller 1010 for use with the stimulation apparatus 600 in accordance with another embodiment of the invention. In this embodiment, the external controller 1010 includes a power supply 1020, a controller 1022 coupled to the power supply 1020, and a user interface 1024 coupled to the controller 1022. The external controller 1010 can also include a pulse generator 1030 coupled to the power supply 1020, a pulse transmitter 1040 coupled to the pulse generator 1030, and an antenna 1042 coupled to the pulse transmitter 1040. The external controller 1010 generates the power and the pulse signal, and the antenna 1042 transmits a pulse signal 1044 to the pulse system 1000 in the stimulation apparatus 600. The pulse system 1000 receives the pulse signal 1044 and delivers an electrical pulse to the electrodes. The pulse system 1000, therefore, does not necessarily include an integrated power supply, controller and pulse generator within the housing 610 because these components are in the external controller 1010.



Figure 11 is a schematic view illustrating an embodiment of the pulse system 1000 in greater detail. In this embodiment, the pulse system 1000 is carried by the support member 610 of the stimulation apparatus 600. The pulse system 1000 can include an antenna 1060 and a pulse delivery system 1070 coupled to the antenna 1060. The antenna 1060 receives the pulse signal 1044 from the external controller 1010 and sends the pulse signal 1044 to the pulse delivery system 1070, which transforms the pulse signal 1044 into electrical pulses. Accordingly, the electrodes 660 can be coupled to the pulse delivery system 1070. The pulse delivery system 1070 can include a filter to remove noise from the pulse signal 1044 and a pulse former that creates an electrical pulse from the pulse signal 1044. The pulse former can be driven by the energy in the pulse signal 1044, or in an alternative embodiment, the pulse system 1000 can also include an integrated power supply to drive the pulse former.

Figure 12 is a schematic view illustrating an embodiment of pulse system 1200 for use in an embodiment of the stimulation apparatus 600, and an external controller 1210 for controlling the pulse system 1200 remotely from the patient using RF energy. In this embodiment, the external controller 1210 includes a power supply 1220, a controller 1222 coupled to the power supply 1220, and a pulse generator 1230 coupled to the controller 1222. The external controller 1210 can also include a modulator 1232 coupled to the pulse generator 1230 and an RF generator 1234 coupled to the modulator 1232. In operation, the external controller 1210 broadcasts pulses of RF energy via an antenna 1242.

The pulse system 1200 can be housed within the stimulation apparatus 600 (not shown). In one embodiment, the pulse system 1200 includes an antenna 1260 and a pulse delivery system 1270. The antenna 1260 incorporates a diode (not shown) that rectifies the broadcast RF energy from the antenna 1242. The pulse delivery system 1270 can include a filter 1272 and a pulse former 1274 that forms electrical pulses which correspond to the RF energy broadcast from the antenna 1242. The pulse system 1200 is accordingly powered by the RF energy in the pulse signal from the external controller 1210 such that the pulse system 1200 does not need a separate power supply carried by the stimulation apparatus 600.

Figure 13 is a cross-sectional view of a pulse system 1300 for use in another embodiment of the implantable stimulation apparatus 600, together with an

external controller 1310 for remotely controlling the pulse system 1300 externally from the patient using magnetic energy. In this embodiment, the external controller 1310 includes a power supply 1320, a controller 1322 coupled to the power supply 1320, and a user interface 1324 coupled to the controller 1322. The external controller 1310 can also include a pulse generator 1330 coupled to the controller 1322, a pulse transmitter 1340 coupled to the pulse generator 1330, and a magnetic coupler 1350 coupled to the pulse transmitter 1340. The magnetic coupler 1350 can include a ferrite core 1352 and a coil 1354 wrapped around a portion of the ferrite core 1352. The coil 1354 can also be electrically connected to the pulse transmitter 1340 so that electrical pulses applied to the coil 1354 generate changes in a corresponding magnetic field. The magnetic coupler 1350 can also include a flexible cap 1356 to position the magnetic coupler 1350 over the implanted stimulation apparatus 600.

The pulse system 1300 can include a ferrite core 1360 and a coil 1362 wrapped around a portion of the ferrite core 1360. The pulse system 1310 can also include a pulse delivery system 1370 including a rectifier and a pulse former. In operation, the ferrite core 1360 and the coil 1362 convert the changes in the magnetic field generated by the magnetic coupler 1350 into electrical pulses that are sent to the pulse delivery system 1370. The electrodes 660 are coupled to the pulse delivery system 1370 so that electrical pulses corresponding to the electrical pulses generated by the pulse generator 1330 in the external controller 1310 are delivered to the stimulation site on the patient.

### 3. Electrode Configurations

Figures 14-24 illustrate electrodes in accordance with various embodiments of the invention that can be used with the stimulation apparatus disclosed herein. Figures 14-22 illustrate embodiments of electrodes configured to apply an electrical current to a stimulation site at least proximate to the pial surface of the cortex, and Figures 23 and 24 illustrate embodiments of electrodes configured to apply an electrical current within the cortex or below the cortex. It will be appreciated that other configurations of electrodes can also be used with other implantable stimulation apparatus.

Figure 14 is a bottom plan view and Figure 15 is a cross-sectional view of a stimulation apparatus 1400 in accordance with an embodiment of the invention. In this embodiment, the stimulation apparatus 1400 includes a first electrode 1410 and a second electrode 1420 concentrically surrounding the first electrode 1410. The first electrode 1410 can be coupled to the positive terminal of a pulse generator 1430, and the second electrode 1420 can be coupled to the negative terminal of the pulse generator 1430. Referring to Figure 15, the first and second electrodes 1410 and 1420 generate a toroidal electric field 1440.

Figure 16 is a bottom plan view and Figure 17 is a cross-sectional view of a stimulation apparatus 1600 in accordance with another embodiment of the invention. In this embodiment, the stimulation apparatus 1600 includes a first electrode 1610, a second electrode 1620 surrounding the first electrode 1610, and a third electrode 1630 surrounding the second electrode 1620. The first electrode 1610 can be coupled to the negative terminals of a first pulse generator 1640 and a second pulse generator 1642; the second electrode 1620 can be coupled to the positive terminal of the first pulse generator 1640; and the third electrode 1630 can be coupled to the positive terminal of the second pulse generator 1642. In operation, the first electrode 1610 and the third electrode 1630 generate a first toroidal electric field 1650, and the first electrode the 1610 and the second electrode 1620 generate a second toroidal electric field 1660. The second toroidal electric field 1660 can be manipulated to vary the depth that the first toroidal electric field 1650 projects away from the base of the stimulation apparatus 1600.

Figure 18 is a bottom plan view and Figure 19 is a cross-sectional view of a stimulation apparatus 1800 in accordance with yet another embodiment of the invention. In this embodiment, the stimulation apparatus 1800 includes a first electrode 1810 and a second electrode 1820 spaced apart from the first electrode 1810. The first and second electrodes 1810 and 1820 are linear electrodes which are coupled to opposite terminals of a pulse generator 1830. Referring to Figure 19, the first and second electrodes 1810 and 1820 can generate an approximately linear electric field.

Figure 20 is a bottom plan view of a stimulation apparatus 2000 in accordance with still another embodiment of the invention. In this embodiment, the stimulation apparatus 2000 includes a first electrode 2010, a second electrode 2020, a third electrode 2030, and a fourth electrode 2040. The first and second electrodes

2010 and 2020 are coupled to a first pulse generator 2050, and the third and fourth electrodes 2030 and 2040 are coupled to a second pulse generator 2060. More specifically, the first electrode 2010 is coupled to the positive terminal and the second electrode 2020 is coupled to the negative terminal of the first pulse generator 2050, and the third electrode 2030 is coupled to the positive terminal and the fourth electrode 2040 is coupled to the negative terminal of the second pulse generator 2060. The first and second electrodes 2010 and 2020 are expected to generate a first electric field 2070, and the third and fourth electrodes 2030 and 2040 are expected to generate a second electric field 2072. It will be appreciated that the ions will be relatively free to move through the brain such that a number of ions will cross between the first and second electric fields 2070 and 2072 as shown by arrows 2074. This embodiment provides control of electric field gradients at the stimulation sites.

Figure 21 is a bottom plan view of another embodiment of the stimulation apparatus 2000. In this embodiment, the first electrode 2010 is coupled to the positive terminal and the second electrode 2020 is coupled to the negative terminal of the first pulse generator 2050. In contrast to the embodiment shown in Figure 20, the third electrode 2030 is coupled to the negative terminal and the fourth electrode 2040 is coupled to the positive terminal of the second pulse generator 2070. It is expected that this electrode arrangement will result in a plurality of electric fields between the electrodes. This allows control of the direction or orientation of the electric field.

Figure 22 is a bottom plan view that schematically illustrates a stimulation apparatus 2200 in accordance with still another embodiment of the invention. In this embodiment, the stimulation apparatus 2200 includes a first electrode 2210, a second electrode 2220, a third electrode 2230, and a fourth electrode 2240. The electrodes are coupled to a pulse generator 2242 by a switch circuit 2250. The switch circuit 2250 can include a first switch 2252 coupled to the first electrode 2210, a second switch 2254 coupled to the second electrode 2220, a third switch 2256 coupled to the third electrode 2230, and a fourth switch 2258 coupled to the fourth electrode 2240. In operation, the switches 2252-2258 can be opened and closed to establish various electric fields between the electrodes 2210-2240. For example, the first switch 2252 and the fourth switch 2258 can be closed in coordination with a pulse from the pulse generator 2242 to generate a first electric field 2260, and/or the

second switch 2254 and the third switch 2256 can be closed in coordination with another pulse from the pulse generator 2242 to generate a second electric field 2270. The first and second electric fields 2260 and 2270 can be generated at the same pulse to produce concurrent fields or alternating pulses to produce alternating or rotating fields.

Figure 23 is a bottom plan view and Figure 24 is a side elevational view of a stimulation apparatus 2300 in accordance with another embodiment of the invention. In this embodiment, the stimulation apparatus 2300 has a first electrode 2310, a second electrode 2320, a third electrode 2330, and a fourth electrode 2340. The electrodes 2310-2340 can be configured in any of the arrangements set forth above with reference to Figures 14-22. The electrodes 2310-2340 also include electrically conductive pins 2350 and/or 2360. The pins 2350 and 2360 can be configured to extend below the pial surface of the cortex. For example, because the length of the pin 2350 is less than the thickness of the cortex 709, the tip of the pin 2350 will accordingly conduct the electrical pulses to a stimulation site within the cortex 709 below the pial surface. The length of the pin 2360 is greater than the thickness of the cortex 709 to conduct the electrical pulses to a portion of the brain below the cortex 709, such as a deep brain region 710. The lengths of the pins are selected to conduct the electrical pulses to stimulation sites below the pia mater 708. As such, the length of the pins 2350 and 2360 can be the same for each electrode or different for individual electrodes. Additionally, only a selected portion of the electrodes and the pins can have an exposed conductive area. For example, the electrodes 2310-2340 and a portion of the pins 2350 and 2360 can be covered with a dielectric material so that only exposed conductive material is at the tips of the pins. It will also be appreciated that the configurations of electrodes set forth in Figures 14-22 can be adapted to apply an electrical current to stimulation sites below the pia mater by providing pin-like electrodes in a manner similar to the electrodes shown in Figures 23 and 24.

Several embodiments of the stimulation apparatus described above with reference to Figures 6-24 are expected to be more effective than existing transcranial or subcranial stimulation devices. In addition to positioning the electrodes under the skull, many embodiments of the stimulation apparatus described above also accurately focus the electrical energy in desired patterns relative to the pia mater 708, the dura

mater 706, and/or the cortex 709. It will be appreciated that transcranial devices may not accurately focus the energy because the electrodes or other types of energy emitters are positioned relatively far from the stimulation sites and the skull diffuses some of the energy. Also, existing subcranial devices generally merely place the electrodes proximate to a specific nerve, but they do not provide electrode configurations that generate an electrical field in a pattern designed for the stimulation site. Several of the embodiments of the stimulation apparatus described above with reference to Figures 6-24 overcome this drawback because the electrodes can be placed against the neurons at the desired stimulation site. Additionally, the electrode configurations of the stimulation apparatus can be configured to provide a desired electric field that is not diffused by the skull 700. Therefore, several embodiments of the stimulation apparatus in accordance with the invention are expected to be more effective because they can accurately focus the energy at the stimulation site.

#### 4. Implantable Stimulation Apparatus with Biasing Elements

Figures 25-30 illustrate several embodiments of stimulation apparatus having a biasing element in accordance with a different aspect of the invention. The stimulation apparatus shown in Figures 25-30 can be similar to those described above with reference to Figures 6-24. Therefore, the embodiments of the stimulation apparatus shown in Figures 25-30 can have the same pulse systems, support members and electrode configurations described above with reference to Figures 6-24.

Figure 25 is an isometric view and Figure 26 is a cross-sectional view of a stimulation apparatus 2500 in accordance with an embodiment of the invention. In one embodiment, the stimulation apparatus 2500 includes a support member 2510, a pulse-system 2530 carried by the support member 2510, and first and second electrodes 2560 coupled to the pulse system 2530. The support member 2510 can be identical or similar to the support member 610 described above with reference to Figures 6 and 7. The support member 2510 can accordingly include a housing 2512 configured to be implanted in the skull 700 and an attachment element 2514 configured to be connected to the skull 700 by fasteners 2518 (Figure 2), an adhesive, and/or an anchor. The pulse system 2530 can be identical or similar to any of the pulse systems described above with reference to Figures 6-13, and the first and second

electrodes 2560 can have any of the electrode configurations explained above with reference to Figures 14-24. Unlike the stimulation apparatus described above, however, the stimulation apparatus 2500 includes a biasing element 2550 coupled to the electrodes 2560 to mechanically bias the electrodes 2560 away from the support member 2510. In an alternative embodiment, the biasing element 2550 can be positioned between the housing 2512 and the attachment element 2514, and the electrodes 2560 can be attached directly to the housing 2512. As explained in more detail below, the biasing element 2550 can be a compressible member, a fluid filled bladder, a spring, or any other suitable element that resiliently and/or elastically drives the electrodes 2560 away from the support member 2510.

Figure 26 illustrates an embodiment of the stimulation apparatus 2500 after it has been implanted into the skull 700 of a patient. When the fasteners 2518 are attached to the skull 700, the biasing element 2550 should be compressed slightly so that the electrodes 2560 contact the stimulation site. In the embodiment shown in Figure 26, the compressed biasing element 2550 gently presses the electrodes 2560 against the surface of the pia mater 708. It is expected that the biasing element 2550 will provide a uniform, consistent contact between the electrodes 2560 and the pial surface of the cortex 709. The stimulation apparatus 2500 is expected to be particularly useful when the implantable device is attached to the skull and the stimulation site is on the pia mater 708 or the dura mater 706. It can be difficult to position the contacts against the pia mater 708 because the distance between the skull 700, the dura mater 706, and the pia mater 708 varies within the cranium as the brain moves relative to the skull, and also as the depth varies from one patient to another. The stimulation apparatus 2500 with the biasing element 2550 compensates for the different distances between the skull 700 and the pia mater 708 so that a single type of device can inherently fit several different patients. Moreover, the stimulation apparatus 2500 with the biasing element 2550 adapts to changes as the brain moves within the skull. In contrast to the stimulation apparatus 2500 with the biasing element 2550, an implantable device that does not have a biasing element 2550 may not fit a particular patient or may not consistently provide electrical contact to the pia mater.

Figures 27 and 28 are cross-sectional views of stimulation apparatus in which the biasing elements are compressible members. Figure 27, more specifically,

illustrates a stimulation apparatus 2700 having a biasing element 2750 in accordance with an embodiment of the invention. The stimulation apparatus 2700 can have an integrated pulse system 2530 and electrodes 2560 coupled to the pulse system 2530 in a manner similar to the stimulation apparatus 2500. The biasing element 2750 in this embodiment is a compressible foam, such as a biocompatible closed cell foam or open cell foam. As best shown in Figure 27, the biasing element 2750 compresses when the stimulation apparatus 2700 is attached to the skull. Figure 28 illustrates a stimulation apparatus 2800 having a biasing element 2850 in accordance with another embodiment of the invention. The biasing element 2850 can be a compressible solid, such as silicon rubber or other suitable compressible materials. The electrodes 2560 are attached to the biasing element 2850.

Figure 29 is a cross-sectional view of a stimulation apparatus 2900 having a biasing element 2950 in accordance with another embodiment of the invention. The stimulation apparatus 2900 can have a support member 2910 including an internal passageway 2912 and a diaphragm 2914. The biasing element 2950 can include a flexible bladder 2952 attached to the support member 2910, and the electrodes 2560 can be attached to the flexible bladder 2952. In operation, the flexible bladder 2952 is filled with a fluid 2954 until the electrodes 2560 press against the stimulation site. In one embodiment, the flexible bladder 2952 is filled by inserting a needle of a syringe 2956 through the diaphragm 2914 and injecting the fluid 2954 into the internal passageway 2912 and the flexible bladder.

Figure 30 is a cross-sectional view of a stimulation apparatus 3000 having a biasing element 3050 in accordance with another embodiment of the invention. In this embodiment, the biasing element 3050 is a spring and the electrodes 2560 are attached to the spring. The biasing element 3050 can be a wave spring, a leaf spring, or any other suitable spring that can mechanically bias the electrodes 2560 against the stimulation site.

Although several embodiments of the stimulation apparatus shown in Figures 25-30 can have a biasing element and any of the pulse systems set forth above with respect to Figures 6-13, it is not necessary to have a pulse system contained within the support member. Therefore, certain embodiments of implantable stimulation apparatus in accordance with the invention can have a pulse system and/or



a biasing member in any combination of the embodiments set forth above with respect to Figures 6-30.

5. Implantable Stimulation Apparatus with External Pulse Systems

Figures 31-35 are schematic cross-sectional views of various embodiments of implantable stimulation apparatus having external pulse systems. Figure 31, more specifically, illustrates an embodiment of a stimulation apparatus 3100 having a biasing element 3150 to which a plurality of electrodes 3160 are attached in a manner similar to the stimulation apparatus described above with reference to Figures 25-30. It will be appreciated that the stimulation apparatus 3100 may not include the biasing element 3150. The stimulation apparatus 3100 can also include an external receptacle 3120 having an electrical socket 3122 and an implanted lead line 3124 coupling the electrodes 3160 to contacts (not shown) in the socket 3122. The lead line 3124 can be implanted in a subcutaneous tunnel or other passageway in a manner known to a person skilled and art.

The stimulation apparatus 3100, however, does not have an internal pulse system carried by the portion of the device that is implanted in the skull 700 of the patient 500. The stimulation apparatus 3100 receives electrical pulses from an external pulse system 3130. The external pulse system 3130 can have an electrical connector 3132 with a plurality of contacts 3134 configured to engage the contacts within the receptacle 3120. The external pulse system 3130 can also have a power supply, controller, pulse generator, and pulse transmitter to generate the electrical pulses. In operation, the external pulse system 3130 sends electrical pulses to the stimulation apparatus 3100 via the connector 3132, the receptacle 3120, and the lead line 3124.

Figures 32 and 33 illustrate an embodiment of a stimulation apparatus 3200 for use with an external pulse system in accordance with another embodiment of the invention. Referring to Figure 33, the stimulation apparatus 3200 can include a support structure 3210 having a socket 3212, a plurality of contacts 3214 arranged in the socket 3212, and a diaphragm 3216 covering the socket 3212. The stimulation apparatus 3200 can also include a biasing element 3250 and a plurality of electrodes 3260 attached to the biasing element 3250. Each electrode 3260 is directly coupled to

one of the contacts 3214 within the support structure 3210. It will be appreciated that an alternative embodiment of the stimulation apparatus 3200 does not include the biasing element 3250.

Referring to Figures 32 and 33 together, the stimulation apparatus 3200 receives the electrical pulses from an external pulse system 3230 that has a power supply, controller, pulse generator, and pulse transmitter. The external pulse system 3230 can also include a plug 3232 having a needle 3233 (Figure 33) and a plurality of contacts 3234 (Figure 33) arranged on the needle 3233 to contact the internal contacts 3214 in the socket 3212. In operation, the needle 3233 is inserted into the socket 3212 to engage the contacts 3234 with the contacts 3214, and then the pulse system 3230 is activated to transmit electrical pulses to the electrodes 3260.

Figures 34 and 35 illustrate additional embodiments of stimulation apparatus for use with external pulse systems. Figure 34 illustrates an embodiment of a stimulation apparatus 3400 having electrodes 3410 coupled to a lead line 3420 that extends under the scalp 702 of the patient 500. The lead line 3420 is coupled to an external pulse system 3450. Figure 35 illustrates an embodiment of a stimulation apparatus 3500 having a support member 3510, electrodes 3512 coupled to the support member 3510, and an external receptacle 3520 mounted on the scalp 702. The external receptacle 3520 can also be connected to the support member 3510. The external receptacle 3520 can have a socket 3522 with contacts (not shown) electrically coupled to the electrodes 3512. The stimulation apparatus 3500 can be used with the external pulse system 3130 described above with reference to Figure 31 by inserting the plug 3132 into the socket 3522 until the contacts 3134 on the plug 3132 engage the contacts within the socket 3522.

## 6. Alternate Embodiments of Implantable Stimulation Apparatus

Figure 36 is a schematic cross-sectional view of an implantable stimulation apparatus 3600 in accordance with another embodiment of the invention. In one embodiment, the stimulation apparatus 3600 has a support structure 3610 and a plurality of electrodes 3620 coupled to the support structure 3610. The support structure 3610 can be configured to be implanted under the skull 700 between an interior surface 701 of the skull 700 and the pial surface of the brain. The support

structure 3610 can be a flexible or compressible body such that the electrodes 3620 contact the pia mater 708 when the stimulation apparatus 3600 is implanted under the skull 700. In other embodiments, the support structure 3610 can position the electrodes 3620 so that they are proximate to, but not touching, the pia mater 708.

In one embodiment, the stimulation apparatus 3600 can receive electrical pulses from an external controller 3630. For example, the external controller 3630 can be electrically coupled to the stimulation apparatus 3600 by a lead line 3632 that passes through a hole 711 in the skull 700. In an alternative embodiment, the stimulation apparatus 3600 can include an integrated pulse system similar to the pulse systems described above with reference to Figures 6-13. Such an embodiment of the stimulation apparatus 3600 can accordingly use a wireless external control unit. It will be appreciated that the electrodes 3620 of the stimulation apparatus 3600 can have several of the electrode configurations described above with reference to Figures 14-24.

Figures 37 and 38 illustrate one embodiment of the implantable stimulation apparatus 3600. Referring to Figure 37, the support structure 3610 can be a flexible substrate and the electrodes 3620 can be conductive elements that are printed onto the flexible substrate. The stimulation apparatus 3600, for example, can be manufactured in a manner similar to flexible printed circuit assemblies that are used in electrical components. The stimulation apparatus 3600 can be implanted under the skull 700 using an insertion tool 3700. In one embodiment, the insertion tool 3700 has a handle 3702 and a shaft 3704 projecting from the handle 3702. The shaft 3704 can have a slot 3706 configured to receive a flat portion of the support member 3610. Referring to Figure 38, the support member 3610 is wrapped around the shaft 3704, and then the stimulation apparatus 3600 is passed to a tube 3720 positioned in the hole 711 through the scalp 700 and the dura mater 706. After the stimulation apparatus 3600 has been passed through the tube 3720, it is unfurled to place the electrodes 3620 at least proximate to the pia mater 708. The electrodes 3620 can be coupled to an external controller by the lead lines 3632.

Figure 39 illustrates another embodiment of an implantable stimulation apparatus 3900 that is also configured to be positioned between the skull 700 and the pia mater 708. In one embodiment, the stimulation apparatus 3900 can include a support member 3910 and a plurality of electrodes 3920 coupled to the support

member 3910. The electrodes 3920 can be coupled to individual lead lines 3922 to connect the electrodes 3920 to an external pulse system. In an alternative embodiment, an integrated pulse system 3930 can be carried by the support member 3910 so that the electrodes 3920 can be coupled directly to the integrated pulse system 3930 without external lead lines 3922. The support member 3910 can be a resiliently compressible member, an inflatable balloon-like device, or a substantially solid incompressible body. In the particular embodiment shown in Figure 39, the support member 3910 is an inflatable balloon-like device that carries the electrodes 3920. In operation, the stimulation apparatus 3900 is implanted by passing the distal end of the support member 3910 through the hole 711 in the skull 700 until the electrodes 3920 are positioned at a desired stimulation site.

Figure 40 is a schematic illustration of a stimulation apparatus 4000 together with an internal pulse system 4030 in accordance with another embodiment of the invention. The stimulation apparatus 4000 can include a support member 4010, a biasing element 4015 carried by the support member 4010, and a plurality of electrodes 4020 carried by the biasing element 4015. The internal pulse system 4030 can be similar to any of the integrated pulse systems described above with reference to Figures 6-13, but the internal pulse system 4030 is not an integrated pulse system because it is not carried by the housing 4010. The internal pulse system 4030 can be coupled to the electrodes 4020 by a cable 4034. In a typical application, the cable 4034 is implanted subcutaneously in a tunnel from a subclavicular region, along the back of the neck, and around the skull. The stimulation apparatus 4000 can also include any of the electrode configurations described above with reference to Figures 14-24.

From the foregoing, it will be appreciated that specific embodiments of the invention have been described herein for purposes of illustration, but that various modifications may be made without deviating from the spirit and scope of the invention. Accordingly, the invention is not limited except as by the appended claims.

1. An apparatus for applying electrical stimulation to a region of a brain of a patient, comprising:

an implantable support member configured to be implanted into the patient at least partially within the skull of the patient;

a pulse system carried by the support member;

a first electrode carried by the support member, the first electrode being coupled to the pulse system; and

a second electrode carried by the support member, the second electrode being spaced apart from the first electrode, and the second electrode being coupled to the pulse system.

2. The apparatus of claim 1 wherein the support member comprises an attachment element and a housing carried by the attachment element, the attachment element being attachable to the skull, and the housing carrying the first and second electrodes.

3. The apparatus of claim 2 wherein the attachment element comprises a mesh.

4. The apparatus of claim 2 wherein the attachment element comprises a plate.

5. The apparatus of claim 1 wherein the support member comprises an attachment element and a housing, the attachment element being a mesh, and the housing having a proximal side attached to the attachment element, a distal side to which the first and second electrodes are attached, and a cavity in which the pulse system is housed.

6. The apparatus of claim 1 wherein the support member comprises an attachment element for attachment to the skull and a housing configured to be implanted in a hole in the skull, the housing having a proximal side attached to the attachment element, a distal side to which the first and second electrodes are attached, and a cavity in which the pulse system is housed, and wherein the housing has a depth of approximately 1-2 cm.

7. The apparatus of claim 1 wherein the support member comprises a compressible member configured to be positioned between the skull and the dura mater or pial surface of the brain.

8. The apparatus of claim 1 wherein:  
the support member comprises a housing configured to be implanted at least partially within the skull, the housing having a cavity; and  
the pulse system comprises a power supply and a pulse generator within the cavity of the housing.

9. The apparatus of claim 1 wherein:  
the support member comprises a housing configured to be implanted at least partially within the skull, the housing having a cavity; and  
the pulse system comprises a pulse generator within the cavity of the housing.

10. The apparatus of claim 1 wherein:  
the support member comprises a housing configured to be implanted at least partially within the skull, and the housing has a cavity; and  
the pulse system comprises a pulse delivery system within the cavity of the housing, the pulse delivery system having a receiver for receiving a pulse of broadcast energy generated by an external pulse generator and a pulse former for converting the broadcast energy into an electrical pulse within the support member.

11. The apparatus of claim 1 wherein:  
the support member comprises a housing configured to be implanted at least partially within the skull, and the housing has a cavity;  
the pulse system comprises a pulse delivery system within the cavity of the housing, the pulse delivery system having a magnetic pickup coil for receiving a pulse of magnetic energy generated by an external pulse generator; and  
the first and second electrodes are electrically coupled to the pulse system within the housing.

12. The apparatus of claim 1 wherein:  
the support member comprises a housing configured to be implanted at least partially within the skull, and the housing has a cavity;  
the pulse system comprises a pulse delivery system within the cavity of the housing, the pulse delivery system having an antenna capable of receiving RF energy and a pulse former coupled to the antenna; and  
the first and second electrodes are electrically coupled to the pulse system within the housing.

13. The apparatus of claim 1 wherein the first and second electrodes are conductive elements at a distal surface of the support member for being positioned against the pial surface of the brain or at least proximate to the pial surface, and wherein the first electrode has a generally circular shape and the second electrode has a generally circular shape that surrounds the first electrode.

14. The apparatus of claim 1 wherein the first and second electrodes are conductive elements at a distal surface of the support member for being positioned against the pial surface of the brain or at least proximate to the pial surface, and wherein the first electrode is defined by a first conductive pad at a first area of the distal surface and the second electrode is defined by a second conductive pad at a second area of the distal surface.

15. The apparatus of claim 1, further comprising a third electrode and a fourth electrode coupled to the pulse system, and wherein the first, second, third and

fourth electrodes are conductive elements at a distal surface of the support member for being positioned against the pial surface of the brain or at least proximate to the pial surface.

16. The apparatus of claim 1, further comprising a switching circuit having a plurality of switches coupled between the electrodes and the pulse system to selectively generate electrical fields between the first, second, third and fourth electrodes.

17. The apparatus of claim 1 wherein the first and second electrodes comprise implantable pins that project from a distal surface of the support member for penetrating into a cortical region or a deep-brain region of the brain.

18. The apparatus of claim 1, further comprising a mechanical biasing element carried by the support member and coupled to the first and second electrodes.

19. The apparatus of claim 18 wherein the biasing element comprises a compressible foam.

20. The apparatus of claim 18 wherein the biasing element comprises a spring.

21. The apparatus of claim 18 wherein the biasing element comprises an inflatable bladder.

22. The apparatus of claim 1 wherein the housing has an interior surface and the first and second electrodes are carried by the housing to be exposed at the interior surface, and wherein the interior surface has a maximum dimension of not greater than 4 cm.

23. The apparatus of claim 1 wherein the housing has an interior surface and the first and second electrodes are carried by the housing to be exposed at



the interior surface, and wherein the interior surface has a maximum dimension of not greater than approximately 1-2 cm.

24. The apparatus of claim 1 wherein the housing has an outer surface configured to face away from the skull and an interior surface configured to face toward the brain, and wherein the interior surface has a maximum dimension of not greater than approximately 1-2 cm and a depth of the housing between the outer surface and the interior surface is approximately 1-2 cm.

25. An apparatus for applying electrical stimulation to a region of a brain of a patient, comprising:

- an implantable support member configured to be implanted into the patient proximate to a skull of the patient, the support member including an attachment element to fix the support member to the skull;

- a pulse system carried by the support member;

- a first electrode at a first region of the support member, the first electrode being coupled to the pulse system; and

- a second electrode at a second region of the support member spaced apart from the first electrode, the second electrode being coupled to the pulse system.

26. The apparatus of claim 25 wherein:

- the support member comprises a housing configured to be implanted at least partially within the skull, the housing having a cavity; and

- the pulse system comprises a power supply and a pulse generator within the cavity of the housing.

27. The apparatus of claim 25 wherein:

- the support member comprises a housing configured to be implanted at least partially within the skull, the housing having a cavity; and

- the pulse system comprises a pulse generator within the cavity of the housing.

28. The apparatus of claim 25 wherein:

the support member comprises a housing configured to be implanted at least partially within the skull, and the housing has a cavity; and

the pulse system comprises a pulse delivery system within the cavity of the housing, the pulse delivery system having a receiver for receiving a pulse of broadcast energy generated by an external pulse generator and a pulse former for converting the broadcast energy into an electrical pulse within the support member.

29. The apparatus of claim 25 wherein:

the support member comprises a housing configured to be implanted at least partially within the skull, and the housing has a cavity;

the pulse system comprises a pulse delivery system within the cavity of the housing, the pulse delivery system having a magnetic pickup coil for receiving a pulse of magnetic energy generated by an external pulse generator; and

the first and second electrodes are electrically coupled to the pulse system within the housing.

30. The apparatus of claim 25 wherein:

the support member comprises a housing configured to be implanted at least partially within the skull, and the housing has a cavity;

the pulse system comprises a pulse delivery system within the cavity of the housing, the pulse delivery system having an antenna capable of receiving RF energy and a pulse former coupled to the antenna; and

the first and second electrodes are electrically coupled to the pulse system within the housing.

31. The apparatus of claim 25, further comprising a mechanical biasing element carried by the support member and coupled to the first and second electrodes.

32. An apparatus for applying electrical stimulation to a region of a brain of a patient, comprising:

an implantable support member configured to be implanted into the patient proximate to a skull of the patient;

a pulse system carried by the support member;

a first electrode at a first region of the support member, the first electrode being coupled directly to the pulse system within the support member; and

a second electrode at a second region of the support member spaced apart from the first electrode, the second electrode being coupled directly to the pulse system within the support member.

33. The apparatus of claim 32 wherein:

the support member comprises a housing configured to be implanted at least partially within the skull, the housing having a cavity; and

the pulse system comprises a power supply and a pulse generator within the cavity of the housing.

34. The apparatus of claim 32 wherein:

the support member comprises a housing configured to be implanted at least partially within the skull, the housing having a cavity; and

the pulse system comprises a pulse generator within the cavity of the housing.

35. The apparatus of claim 32 wherein:

the support member comprises a housing configured to be implanted at least partially within the skull, and the housing has a cavity; and

the pulse system comprises a pulse delivery system within the cavity of the housing, the pulse delivery system having a receiver for receiving a pulse of broadcast energy generated by an external pulse generator and a pulse former for converting the broadcast energy into an electrical pulse within the support member.

36. The apparatus of claim 32 wherein:  
the support member comprises a housing configured to be implanted at least partially within the skull, and the housing has a cavity;  
the pulse system comprises a pulse delivery system within the cavity of the housing, the pulse delivery system having a magnetic pickup coil for receiving a pulse of magnetic energy generated by an external pulse generator; and  
the first and second electrodes are electrically coupled to the pulse system within the housing.

37. The apparatus of claim 32 wherein:  
the support member comprises a housing configured to be implanted at least partially within the skull, and the housing has a cavity;  
the pulse system comprises a pulse delivery system within the cavity of the housing, the pulse delivery system having an antenna capable of receiving RF energy and a pulse former coupled to the antenna; and  
the first and second electrodes are electrically coupled to the pulse system within the housing.

38. The apparatus of claim 32, further comprising a mechanical biasing element carried by the support member and coupled to the first and second electrodes.

39. An apparatus for applying electrical stimulation to a cortical region of a brain of a patient, comprising:  
an implantable support member configured to be implanted into the patient proximate to a skull of the patient;  
a mechanical biasing element carried by the support member, the mechanical biasing element being elastically deformable; and  
a first electrode and a second electrode, wherein the biasing element is configured to press the first and second electrodes against the brain of the patient.

40. The apparatus of claim 39 wherein the biasing element comprises a compressible foam.

41. The apparatus of claim 39 wherein the biasing element comprises a spring.

42. The apparatus of claim 39 wherein the biasing element comprises an inflatable bladder.

43. The apparatus of claim 39, further comprising a pulse system carried by the support member.

44. The apparatus of claim 43 wherein:  
the support member comprises a housing configured to be implanted at least partially within the skull, the housing having a cavity; and  
the pulse system comprises a power supply and a pulse generator within the cavity of the housing.

45. The apparatus of claim 43 wherein:  
the support member comprises a housing configured to be implanted at least partially within the skull, the housing having a cavity; and  
the pulse system comprises a pulse generator within the cavity of the housing.

46. The apparatus of claim 43 wherein:  
the support member comprises a housing configured to be implanted at least partially within the skull, and the housing has a cavity; and  
the pulse system comprises a pulse delivery system within the cavity of the housing, the pulse delivery system having a receiver for receiving a pulse of broadcast energy generated by an external pulse generator and a pulse former for converting the broadcast energy into an electrical pulse within the support member.

47. The apparatus of claim 43 wherein:  
the support member comprises a housing configured to be implanted at least partially within the skull, and the housing has a cavity;

the pulse system comprises a pulse delivery system within the cavity of the housing, the pulse delivery system having a magnetic pickup coil wrapped around the core for receiving a pulse of magnetic energy generated by an external pulse generator; and

the first and second electrodes are electrically coupled to the pulse system within the housing.

48. The apparatus of claim 43 wherein:

the support member comprises a housing configured to be implanted at least partially within the skull, and the housing has a cavity;

the pulse system comprises a pulse delivery system within the cavity of the housing, the pulse delivery system having an antenna capable of receiving RF energy and a pulse former coupled to the antenna; and

the first and second electrodes are electrically coupled to the pulse system within the housing.

49. The apparatus of claim 39, further comprising an external controller having a power supply, a pulse generator and a pulse transmitter, wherein the external controller is electrically coupled to the electrodes by a cable.

50. The apparatus of claim 39, further comprising:

an external controller having a power supply, a pulse generator and a pulse transmitter, wherein the external controller generates a pulse of broadcast energy; and

a pulse system carried by the support member separate from the external controller, wherein the pulse system is capable of converting the broadcast energy from the external controller into a corresponding electrical pulse; and

wherein the electrodes are coupled to the pulse system.

51. An apparatus for applying electrical stimulation to a cortical region of a brain of a patient, comprising:

an implantable support member configured to be implanted into the patient proximate to a skull of the patient;

a pulse system within the support member;

a biasing element carried by the support member; and

an electrode attached to the biasing element and electrically coupled to the pulse system.

52. The apparatus of claim 51 wherein the support member, the pulse system, the biasing element and the electrode have a total weight of not greater than 35g.

53. The apparatus of claim 51 wherein the support member and the pulse system occupy a volume of not greater than 20 cubic centimeters.

54. An apparatus for effectuating a neural-function of a patient associated with a first location of the brain of the patient, comprising:

a diagnostic system capable of identifying a stimulation site by determining a region of the brain where an intended neural activity is present in response to generating the intended neural activity remotely from the first location of the brain; and

a stimulation system including an electrode configured to be implanted at the stimulation site and a pulse generator to provide an electrical potential to the electrode.

55. The apparatus of claim 54 wherein the diagnostic system comprises an imaging device capable of determining neural activity.

56. The apparatus of claim 54 wherein the diagnostic system comprises a functional MRI device.

57. The apparatus of claim 54 wherein the stimulation system comprises an integrated unit in which the pulse generator is coupled directly to the electrode, and wherein the integrated unit is configured to be implanted adjacent to and/or within the skull of the patient.

58. The apparatus of claim 54 wherein the stimulation system has a flexible substrate, a first electrode on one area of the substrate, and a second electrode on another area of the substrate; and wherein the flexible substrate moves between an insertion configuration to insert the electrode through a small hole in the skull and a deployed configuration larger than the insertion configuration to position the first and second electrodes at least proximate to the cortex of the patient.

59. The apparatus of claim 54 wherein:  
the diagnostic system comprises a sensor capable of sensing a threshold for generating electrophysiologic signals associated with the neural function; and  
the pulse generator is configured to apply an electrical potential to the electrode that is less than the threshold determined by the sensor.

60. An apparatus for treating a loss of a neural-function at a first cortical location of a brain of a patient, comprising:

a diagnostic system capable of selecting a stimulation site at a cortical region of the brain where neural activity is expected to occur to compensate for the loss of neural-function at the first cortical location of the brain; and

a stimulation system having a first electrode and a second electrode, the stimulation system being configured to be implanted in the patient proximate to the pia matter in the cortical region such that the first electrode is at a first area of the stimulation site and the second electrode is at a second area of the stimulation site.

61. The apparatus of claim 60 wherein the diagnostic system comprises an imaging device capable of determining neural activity.

62. The apparatus of claim 60 wherein the diagnostic system comprises a functional MRI device.



63. The apparatus of claim 60 wherein the stimulation system comprises an integrated unit in which the pulse generator is coupled directly to the first and second electrodes, and wherein the integrated unit is configured to be implanted adjacent to and/or within the skull of the patient.

64. The apparatus of claim 60 wherein the stimulation system has a flexible substrate, and the first and second electrodes are carried by the substrate; and wherein the flexible substrate moves between an insertion configuration to insert the electrodes through a small hole in the skull and a deployed configuration larger than the insertion configuration to position the first and second electrodes proximate to the cortex of the patient.

65. The apparatus of claim 60 wherein:  
the diagnostic system comprises a sensor capable of sensing a threshold for generating electrophysiologic signals associated with the neural function; and  
the pulse generator is configured to apply an electrical potential to the first and second electrodes that is less than the threshold determined by the sensor.

66. An apparatus for treating a neural-function in a brain of a patient, comprising:

a diagnostic system that determines an electrical stimulation threshold for inducing a response in cells at a stimulation site in the cortical region of the brain of the patient; and

a stimulation system having a first electrode, a second electrode and a controller coupled to the first and second electrodes, wherein the first and second electrodes are configured to be implanted proximate to the pia matter of the brain of the patient, and wherein the controller is configured to apply an electrical stimulation at an intensity lower than the stimulation threshold between the first and second electrodes.

67. The apparatus of claim 66 wherein the stimulation system comprises an integrated unit in which the pulse generator is coupled directly to the

first and second electrodes, and wherein the integrated unit is configured to be implanted adjacent to and/or within the skull of the patient.

68. The apparatus of claim 66 wherein the stimulation system has a flexible substrate, and the first and second electrodes are carried by the substrate; and wherein the flexible substrate moves between an insertion configuration to insert the first and second electrodes through a small hole in the skull and a deployed configuration larger than the insertion configuration to engage the first and second electrodes with the cortex of the patient.

69. A method of effectuating a neural-function of a patient associated with a first location of the brain of the patient, comprising:

identifying a stimulation site by generating remotely from the first location an intended neural activity and determining a region of the brain where the generated neural activity is present;

positioning at least a first electrode at the stimulation site; and

applying an electrical potential to pass a current through the first electrode.

70. The method of claim 69 wherein the neural-function has been affected by brain damage to the first region of the brain, and wherein:

generating the intended neural activity comprises applying an input for the neural function that causes a signal to be sent to the brain; and

determining a region of the brain wherein the generated neural activity is present comprises detecting the neural activity that occurs in response to the signal sent to the brain.

71. The method of claim 70 wherein the neural function controls use of a body part, and applying an input for the neural function comprises moving the body part.

72. The method of claim 70 wherein the neural function controls use of a body part, and applying an input for the neural function comprises applying a peripheral electrical stimulation to the body part.

73. The method of claim 70 wherein detecting neural activity comprises imaging of the brain.

74. The method of claim 70 wherein detecting neural activity comprises taking a functional MRI image of the brain.

75. The method of claim 70 wherein the neural function controls use of a body part, and wherein:

applying an input to the neural function comprises moving the body part;  
and

imaging the brain for neural activity comprises taking a functional MRI image of the brain.

76. The method of claim 69 wherein identifying a stimulation site comprises applying an input for the neural function that causes a signal to be sent to the brain.

77. The method of claim 76 wherein the neural function controls use of a body part, and applying an input for the neural function comprises moving the body part.

78. The method of claim 76 wherein the neural function controls use of a body part, and applying an input for the neural function comprises applying a peripheral electrical stimulation to the body part.

79. The method of claim 69 wherein the neural-function has been affected by damage, disease and/or a disorder at the first region of the brain, and wherein:

generating the intended neural activity comprises applying a peripheral input to the patient for effectuating the neural function that causes a signal to be sent to the brain; and

determining a region of the brain wherein the generated neural activity is present comprises detecting a change in neural activity in response to the signal sent to the brain.

80. The method of claim 79 wherein determining a region of the brain where the generated neural activity is present comprises determining a location in the brain different than the first location at which the generated neural activity occurs.

81. The method of claim 79 wherein determining a region of the brain where the generated neural activity is present comprises determining a location at which a change in neural activity occurs in correspondence to a change in the neural-function.

82. The method of claim 69 wherein positioning at least a first electrode at the stimulation site comprises positioning first and second electrodes at the stimulation site and resiliently biasing at least one of the first and second electrodes against a surface of the brain.

83. The method of claim 69 wherein positioning at least a first electrode at the stimulation site comprises positioning first and second electrodes at the stimulation site and resiliently biasing at least one of the first and second electrodes against the pia mater.

84. The method of claim 69, further comprising implanting a stimulation apparatus having an integrated pulse system directly coupled to the first electrode so that the stimulation apparatus is adjacent to and/or within the skull of the

patient, and wherein positioning the first electrode comprises placing the first electrode at least proximate to the pia mater.

85. The method of claim 69, further comprising implanting a stimulation apparatus having an integrated pulse system directly coupled to the first electrode so that the stimulation apparatus is adjacent to and/or within the skull of the patient, and wherein positioning the first electrode comprises inserting the first electrode into the cortex of the brain.

86. The method of claim 69 wherein applying an electrical potential comprises placing a voltage of  $\pm 1$  mV to  $\pm 10$  V between the first electrode and a second electrode.

87. The method of claim 69 wherein applying an electrical potential comprises generating electrical pulses at 2 to 1000 Hz.

88. The method of claim 69, further comprising ascertaining a threshold for generating action potentials for cells at the stimulation site, and wherein applying an electrical potential comprises placing a subthreshold voltage less than the threshold for generating action potentials.

89. The method of claim 69, further comprising ascertaining a threshold for generating action potentials for cells at the stimulation site, and wherein applying an electrical potential comprises placing a subthreshold voltage between the first electrode and a second electrode approximately 10-40% less than the threshold for generating action potential.

90. The method of claim 69, further comprising ascertaining a threshold for generating electrophysiologic signals associated with the neural function, and wherein applying an electrical potential comprises placing a subthreshold voltage between the first electrode and a second electrode less than the threshold for generating electrophysiologic signals.

91. The method of claim 69, further comprising ascertaining a threshold for generating electrophysiologic signals for cells at the stimulation site, and wherein applying an electrical potential comprises placing a subthreshold voltage between the first electrode and a second electrode 20-50% less than the threshold for generating electrophysiologic signals.

92. The method of claim 69, further comprising ascertaining a threshold for eliciting the neural function, and wherein applying an electrical potential comprises placing a subthreshold voltage between the first electrode and a second electrode less than the threshold for eliciting the neural function.

93. The method of claim 69, further comprising ascertaining a threshold for eliciting the neural function, and wherein applying an electrical potential comprises placing a subthreshold voltage between the first electrode and a second electrode 30-60% less than the threshold for eliciting the neural function.

94. The method of claim 69 wherein a motor function and/or a sensory function of a body part controlled by the neural-function has been affected by brain damage to the first region of the brain, and wherein the method further comprises performing physical therapy to the affected body part while or immediately after applying the electrical potential between the first electrode and a second electrode.

95. The method of claim 69 wherein a motor function and/or a sensory function of a body part controlled by the neural-function has been affected by brain damage to the first region of the brain, and wherein the method further comprises pharmaceutically stimulating the brain while applying the electrical potential between the first electrode and a second electrode.

96. A method of effectuating a neural-function of a brain of a patient associated with a first location in the brain, comprising:

identifying a stimulation site in and/or on the brain where neural activity has changed in response to a change in the neural-function in the first location of the brain;

positioning a first electrode at the stimulation site;

positioning a second electrode at the stimulation site; and

applying an electrical potential between the first and second electrodes.

97. The method of claim 96 wherein identifying a stimulation site comprises imaging the cortex of the brain.

98. The method of claim 96 wherein identifying a stimulation site comprises:

taking a first image of the brain that shows neural activity related to the neural-function using functional MRI;

taking a second image of the brain that shows neural activity related to the neural-function using functional MRI after taking the first image of the brain; and

comparing a change in the neural activity related to the neural-function.

99. The method of claim 96, further comprising applying a peripheral input to the patient that is expected to generate neural activity in the brain related to performing the neural-function.

100. The method of claim 96, further comprising:

applying a peripheral input to the patient that is expected to generate neural activity in the brain that performs the neural-function; and

identifying a stimulation site comprises taking a first image of the brain that shows neural activity before applying the peripheral input, taking a second image of the brain that shows neural activity while applying the peripheral input, and comparing a change in neural activity in the brain between the first and second images.

101. The method of claim 96 wherein neural activity for the neural-function is expected to occur at the first location in the brain according to a known functional organization of the brain, and wherein identifying the stimulation site comprises detecting neural activity for the neural-function at a second location in the brain different than the first location.

102. The method of claim 101 wherein detecting the neural activity comprises taking functional MRI images of the brain and monitoring neural activity at the second location.

103. The method of claim 96 wherein the neural-function controls learning a task and the neural activity related to the neural function is expected to occur at the first location of the brain according to a known functional organization of the brain, and wherein identifying the stimulation site comprises detecting a change in the neural activity at the first location of the brain while the patient learns the task.

104. The method of claim 103 wherein detecting a change in the neural activity comprises taking functional MRI images of the brain while the patient learns the task.

105. The method of claim 96 wherein the neural-function controls learning a task and the neural activity related to the neural function is expected to occur at the first location of the brain according to a known functional organization of the brain, and wherein identifying the stimulation site comprises detecting a change in the neural activity at a second location different than the first location of the brain while the patient learns the task.

106. The method of claim 105 wherein detecting a change in the neural activity comprises taking functional MRI images of the brain while the patient learns the task.

107. The method of claim 96 wherein the first region of the brain is affected by a disease and neural activity related to the neural-function is expected to



occur at the first location of the brain according to a known functional organization of the brain, and wherein identifying the stimulation site comprises detecting a change in neural activity adjacent to the first region.

108. The method of claim 96 wherein the first region of the brain is affected by a disease and neural activity related to the neural-function is expected to occur at the first location of the brain according to a known functional organization of the brain, and wherein identifying the stimulation site comprises detecting a change in neural activity related to the neural-function at a second location different than the first location.

109. The method of claim 96 wherein the first region of the brain is affected by brain damage and neural activity related to the neural-function is expected to occur at the first location of the brain according to a known functional organization of the brain, and wherein identifying the stimulation site comprises detecting a change in neural activity adjacent to the first region.

110. The method of claim 96 wherein the first region of the brain is affected by brain damage and neural activity related to the neural-function is expected to occur at the first location of the brain according to a known functional organization of the brain, and wherein identifying the stimulation site comprises detecting a change in neural activity related to the neural-function at a second location different than the first location.

111. A method of treating a loss of a neural-function at a first cortical location of a brain of a patient, comprising:

- selecting a stimulation site at a cortical region of the brain where neural activity is expected to occur to compensate for the loss of neural-function at the first cortical location of the brain;

- positioning a first electrode at a first area of the stimulation site proximate to the pia mater in the cortical region;

- positioning a second electrode at a second area of the stimulation site proximate to the pia mater in the cortical region; and

applying an electrical potential between the first and second electrodes.

112. The method of claim 111 wherein the neural-function is generally carried out by neural activity at the first region of the brain according to a known functional organization of the brain, and wherein selecting a stimulation site comprises estimating a location of a second region of the brain where neural activity for performing the neural-function is expected to be present, the location of the second region being spaced apart from the first region.

113. The method of claim 111 wherein:

selecting the stimulation site comprises determining a location at which neuroplasticity for implementing the neural-function is expected to occur; and

applying an electrical potential comprises placing an electrical pulse across the first and second electrodes without imaging the brain for neural activity related to the neural-function.

114. The method of claim 111 wherein selecting the stimulation site comprises determining a location adjacent to the first location of the brain.

115. A method of treating a neural-function in a brain of a patient using an apparatus having a support member, a pulse system carried by the support member, and an electrode assembly including first and second electrodes at an interior surface of the support member, comprising:

implanting the support member in the patient proximate to a skull of the patient to position the pulse system proximate to the skull and to position the first and second electrodes proximate to a stimulation site on and/or in the brain of the patient; and

controlling the pulse system to apply an electrical potential between the first and second electrodes at the stimulation site.

116. A method of treating a neural-function in a brain of a patient using an apparatus having a support member, a pulse system carried by the support

member, and an electrode assembly including first and second electrodes at an interior surface of the support member, comprising:

implanting the support member proximate to a skull of the patient to position the first and second electrodes at least proximate to the pia mater of the brain of the patient at a first cortical location;

mechanically biasing the support member and/or the first and second electrodes to resiliently press the first and second electrodes against one of the dura mater or the pia mater of the brain of the patient at the first cortical region; and

controlling a pulse generator coupled to the first and second electrodes to apply an electrical potential between the first and second electrodes in the first cortical region of the brain.

117. A method of treating a neural-function in a brain of a patient, comprising:

selecting a stimulation site in a first cortical region of the brain;

determining an electrical stimulation threshold for inducing a response in cells at the stimulation site; and

applying an electrical stimulation at an intensity lower than the stimulation threshold between first and second electrodes proximate to the pia mater of the first cortical region of the brain.

118. The method of claim 117, further comprising identifying the stimulation site by determining where neural activity has changed in response to a change in the neural-function.

119. The method of claim 118 wherein identifying a stimulation site comprises:

taking a first image of the brain that shows neural activity related to the neural-function using functional MRI;

taking a second image of the brain that shows neural activity related to the neural-function using functional MRI after taking the first image of the brain; and

comparing a change in the neural activity related to the neural-function.

120. The method of claim 118, further comprising applying a peripheral input to the patient that is expected to generate the neural activity in the brain related to performing the neural-function.

121. The method of claim 118, further comprising:  
applying a peripheral input to the patient designed to generate the neural activity in the brain that performs the neural-function; and  
identifying a stimulation site comprises taking a first image of the brain that shows neural activity before applying the peripheral input, taking a second image of the brain that shows neural activity while applying the peripheral input, and comparing a change in neural activity in the brain between the first and second images.

122. The method of claim 118 wherein neural activity for the neural-function is expected to occur at the first location in the brain according to a known functional organization of the brain, and wherein identifying the stimulation site comprises detecting neural activity for the neural-function at a second location in the brain different than the first location.

123. The method of claim 122 wherein detecting the neural activity comprises taking functional MRI images of the brain and monitoring neural activity at the second location.

124. The method of claim 118 wherein the neural-function controls learning a task and the neural activity related to the neural function is expected to occur at the first location of the brain according to a known functional organization of the brain, and wherein identifying the stimulation site comprises detecting a change in the neural activity at the first location of the brain while the patient learns the task.

125. The method of claim 124 wherein detecting a change in the neural activity comprises taking functional MRI images of the brain while the patient learns the task.

126. The method of claim 118 wherein the neural-function controls learning a task and the neural activity related to the neural function is expected to occur at the first location of the brain according to a known functional organization of the brain, and wherein identifying the stimulation site comprises detecting a change in the neural activity at a second location different than the first location of the brain while the patient learns the task.

127. The method of claim 126 wherein detecting a change in the neural activity comprises taking functional MRI images of the brain while the patient learns the task.

128. The method of claim 118 wherein the first region of the brain is affected by a disease and neural activity related to the neural-function is expected to occur at the first location of the brain according to a known functional organization of the brain, and wherein identifying the stimulation site comprises detecting a change in neural activity adjacent to the first region.

129. The method of claim 118 wherein the first region of the brain is affected by a disease and neural activity related to the neural-function is expected to occur at the first location of the brain according to a known functional organization of the brain, and wherein identifying the stimulation site comprises detecting a change in neural activity related to the neural-function at a second location different than the first location.

130. The method of claim 118 wherein the first region of the brain is affected by brain damage and neural activity related to the neural-function is expected to occur at the first location of the brain according to a known functional organization of the brain, and wherein identifying the stimulation site comprises detecting a change in neural activity adjacent to the first region.

131. The method of claim 118 wherein the first region of the brain is affected by brain damage and neural activity related to the neural-function is expected to occur at the first location of the brain according to a known functional organization

of the brain, and wherein identifying the stimulation site comprises detecting a change in neural activity related to the neural-function at a second location different than the first location.

132. The method of claim 118 wherein applying the electrical potential comprises inducing an increase in a resting membrane potential of neurons subject to the electrical potential.

133. The method of claim 132 wherein applying an electrical stimulation comprises providing an electrical potential between the first and second electrodes that increases the resting membrane potential of a desired population of neurons at the stimulation site by 10%-95% of a voltage gap between the resting membrane potential and an action potential for the desired population of neurons.

134. The method of claim 132 wherein applying an electrical stimulation comprises providing an electrical potential between the first and second electrodes that increases the resting membrane potential of a desired population of neurons at the stimulation site by 10%-95% of a voltage gap between the resting membrane potential and an action potential for the desired population of neurons, and wherein the electrical potential is provided at a frequency of approximately 40-200 Hz.

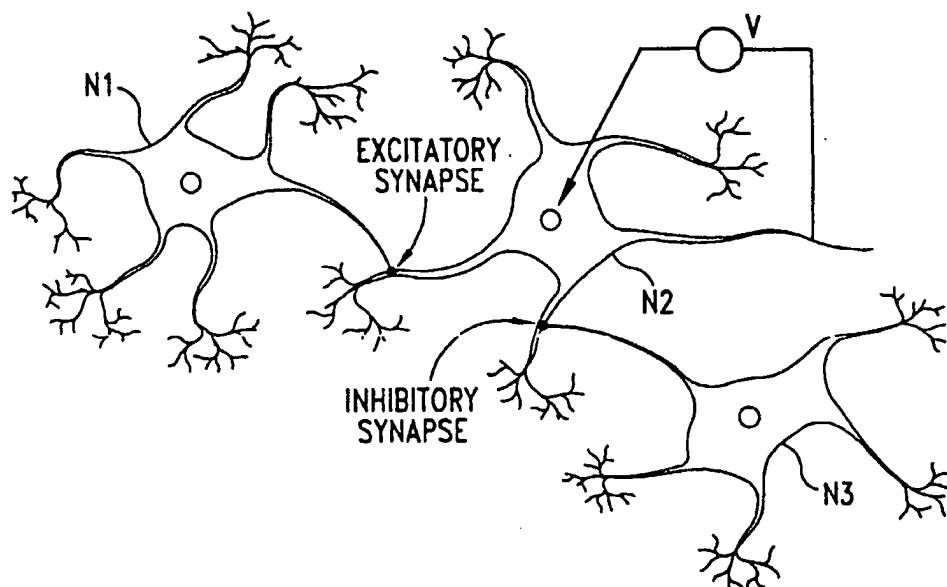
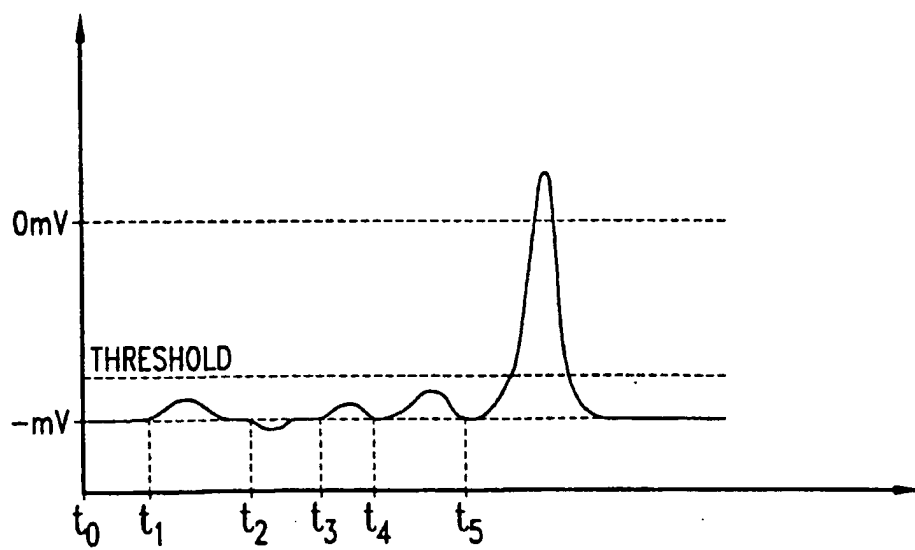
135. The method of claim 132 wherein applying an electrical stimulation comprises providing an electrical potential between the first and second electrodes that increases the resting membrane potential of a desired population of neurons at the stimulation site by 10%-95% of a voltage gap between the resting membrane potential and an action potential for the desired population of neurons, and wherein the electrical potential is provided at a frequency of approximately 40-200 Hz and a pulse width of approximately 20-100 $\mu$ s.

136. The method of claim 132 wherein applying an electrical stimulation comprises providing an electrical potential between the first and second electrodes that increases the resting membrane potential of a desired population of

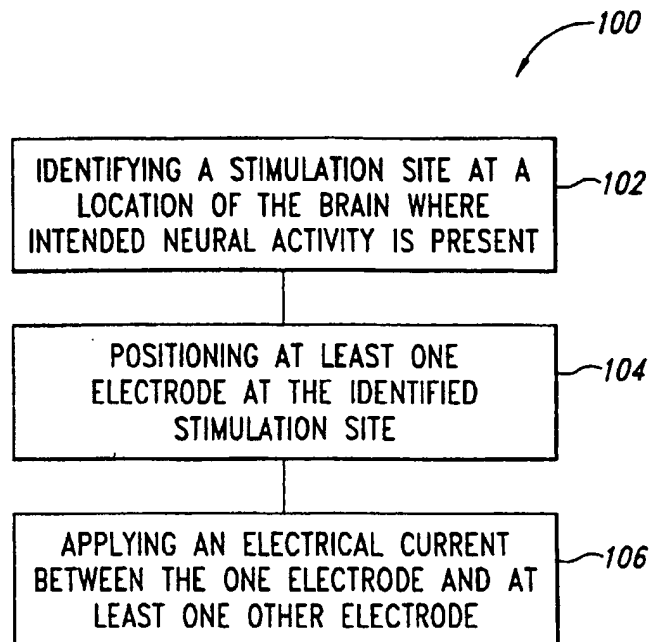
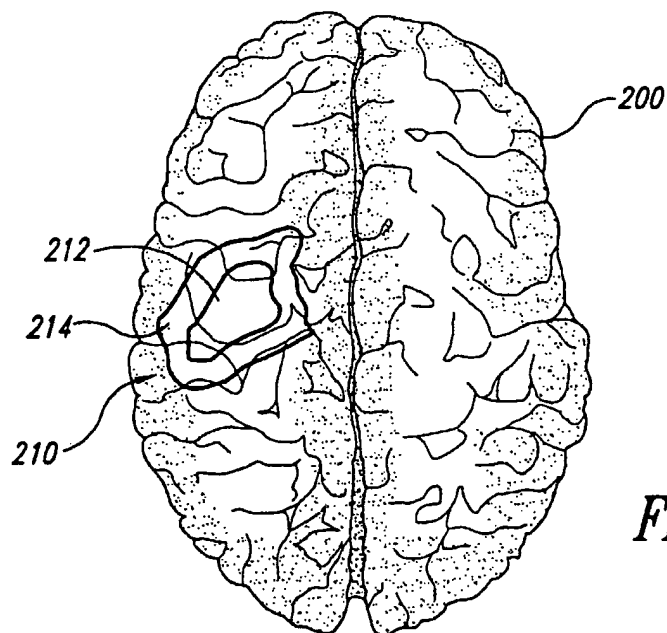
neurons at the stimulation site by 60%-80% of a voltage gap between the resting membrane potential and an action potential for the desired population of neurons.

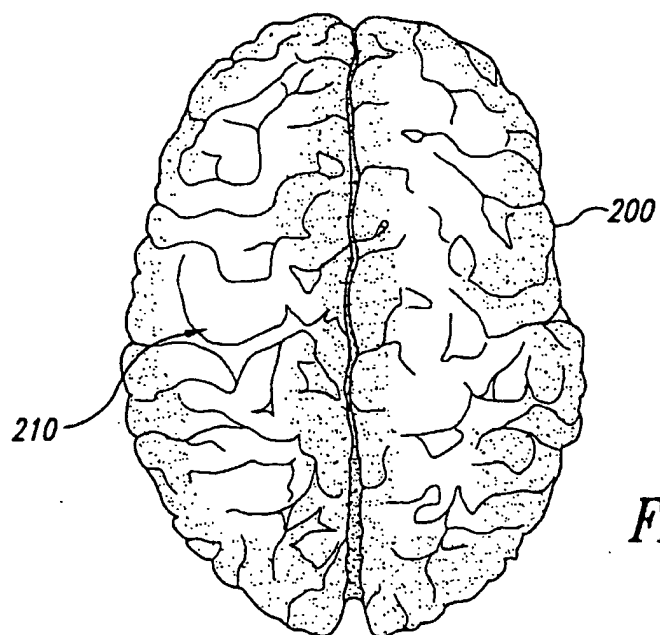
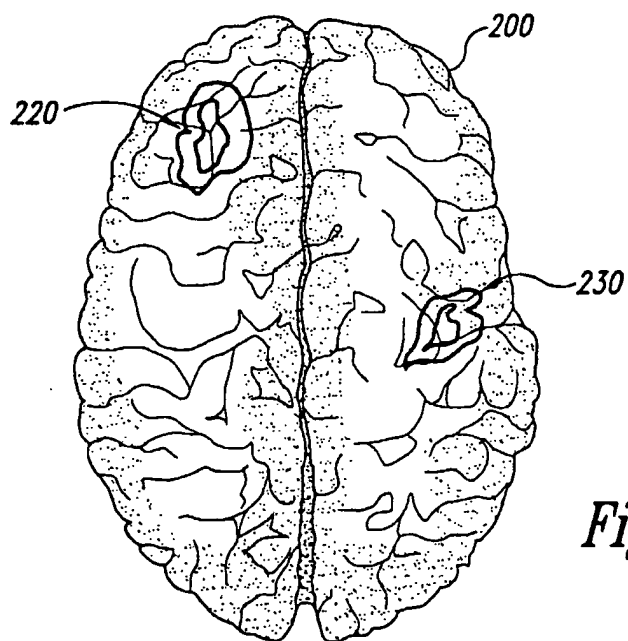
137. The method of claim 132 wherein applying an electrical stimulation comprises providing an electrical potential between the first and second electrodes that increases the resting membrane potential of a desired population of neurons at the stimulation site by 60%-80% of a voltage gap between the resting membrane potential and an action potential for the desired population of neurons, and wherein the electrical potential is provided at a frequency of approximately 40-200 Hz.

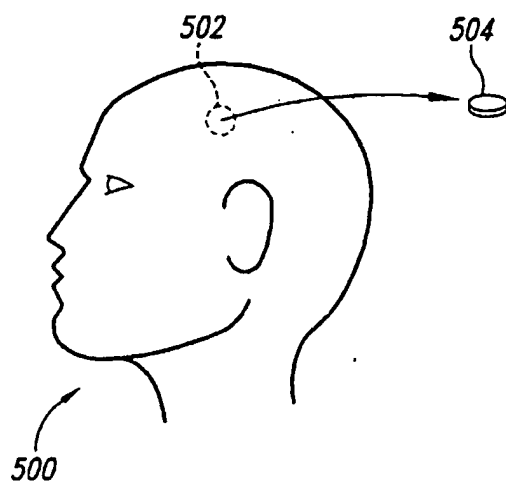
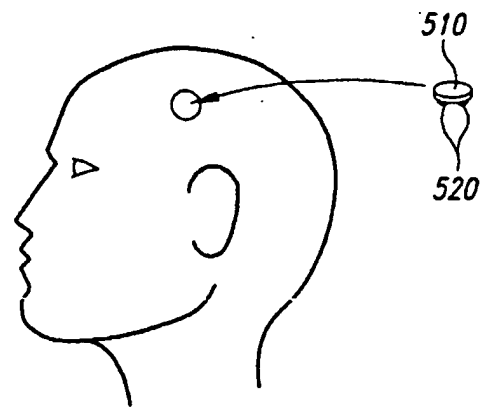
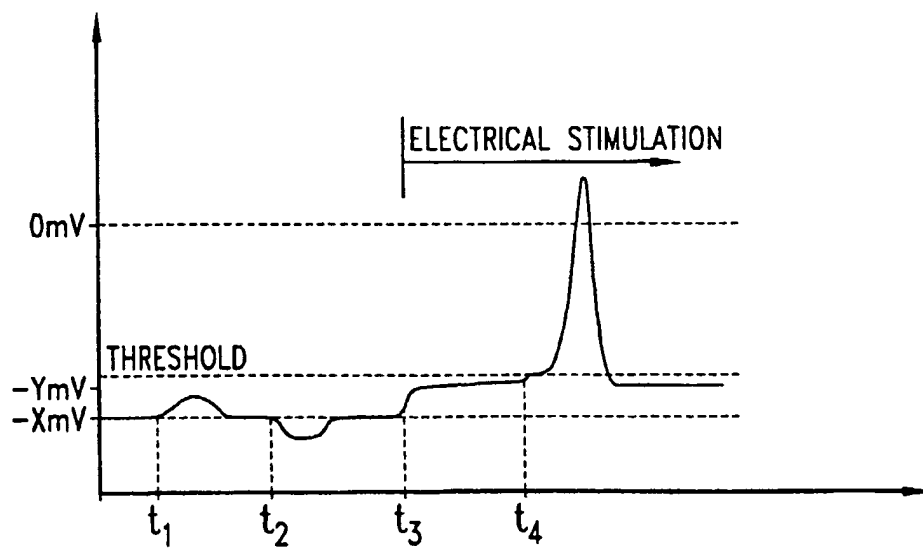
138. The method of claim 132 wherein applying an electrical stimulation comprises providing an electrical potential between the first and second electrodes that increases the resting membrane potential of a desired population of neurons at the stimulation site by 60%-80% of a voltage gap between the resting membrane potential and an action potential for the desired population of neurons, and wherein the electrical potential is provided at a frequency of approximately 40-200 Hz and a pulse width of approximately 20-100 $\mu$ s.

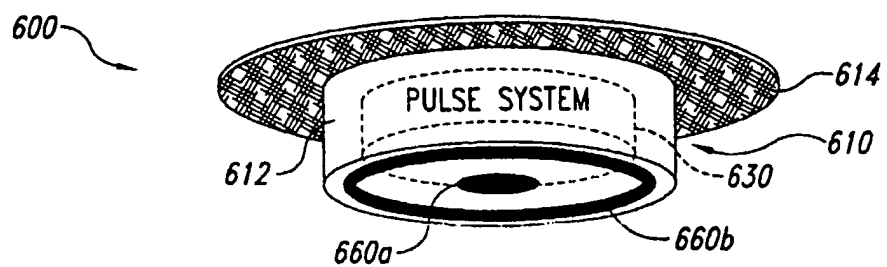
*Fig. 1A**Fig. 1B*



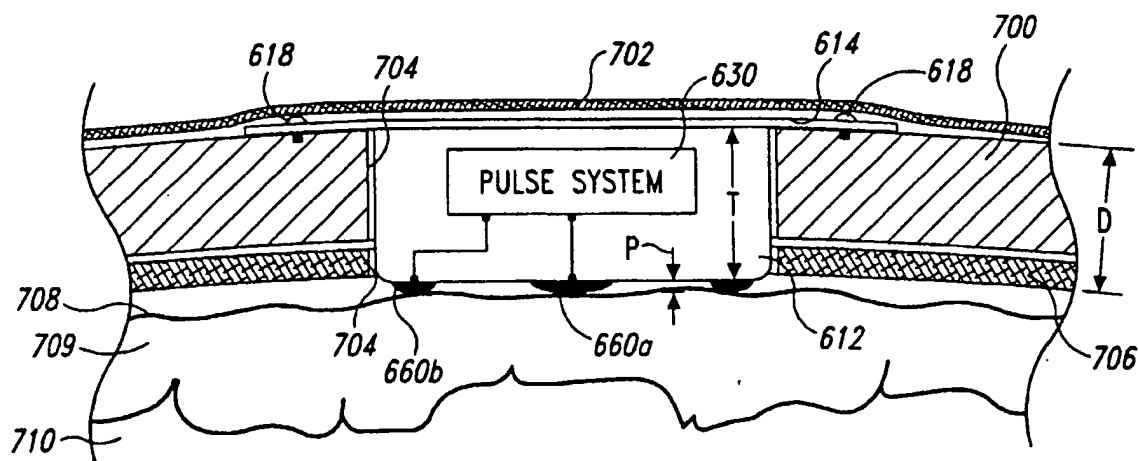
*Fig. 1C**Fig. 2*

*Fig. 3**Fig. 4*

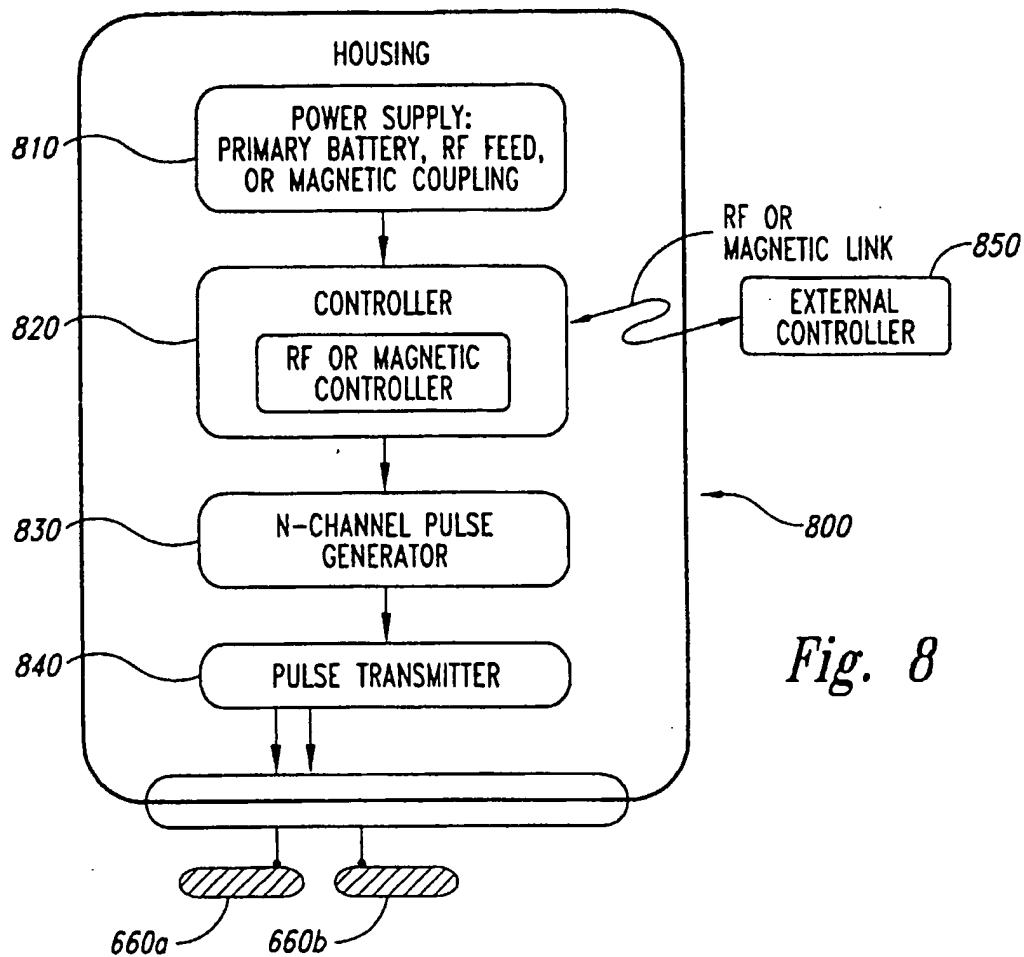
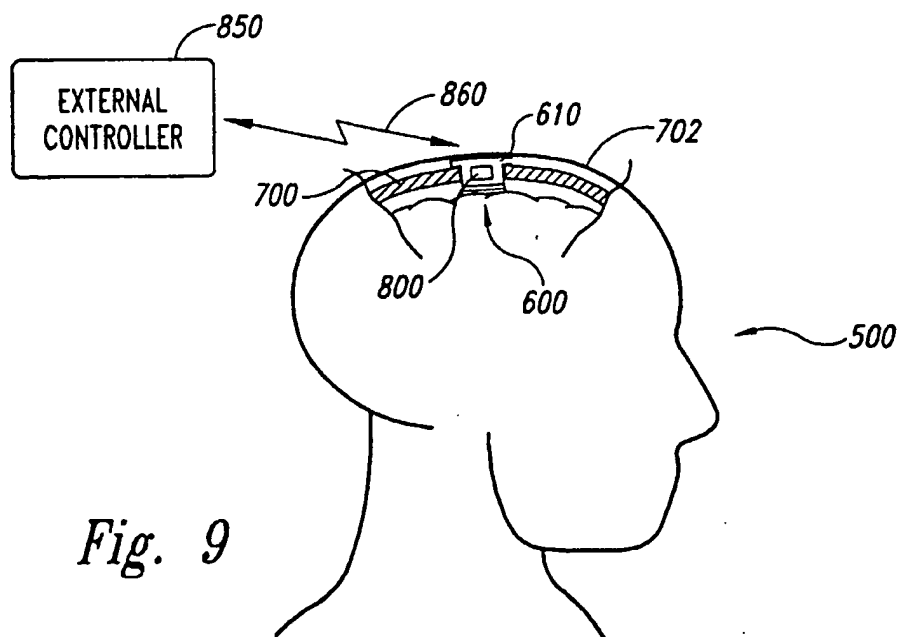
*Fig. 5A**Fig. 5B**Fig. 5C*

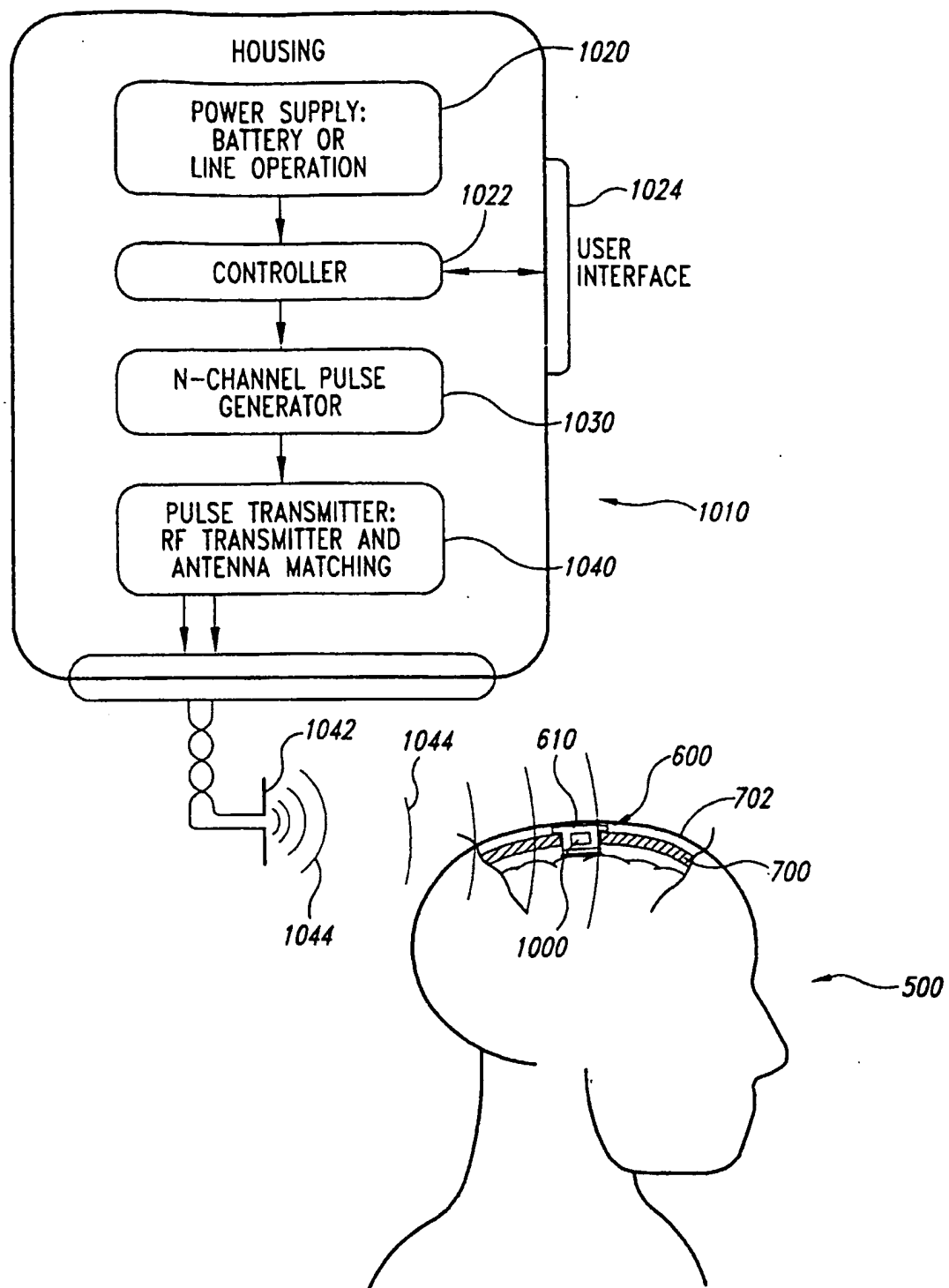


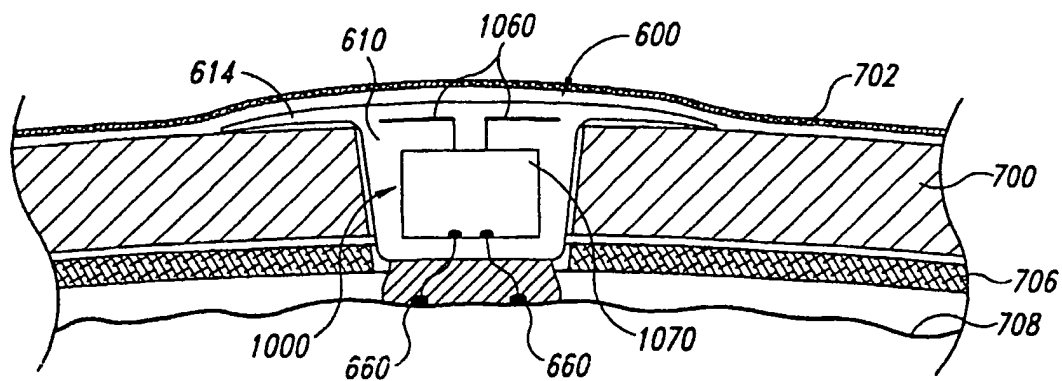
*Fig. 6*



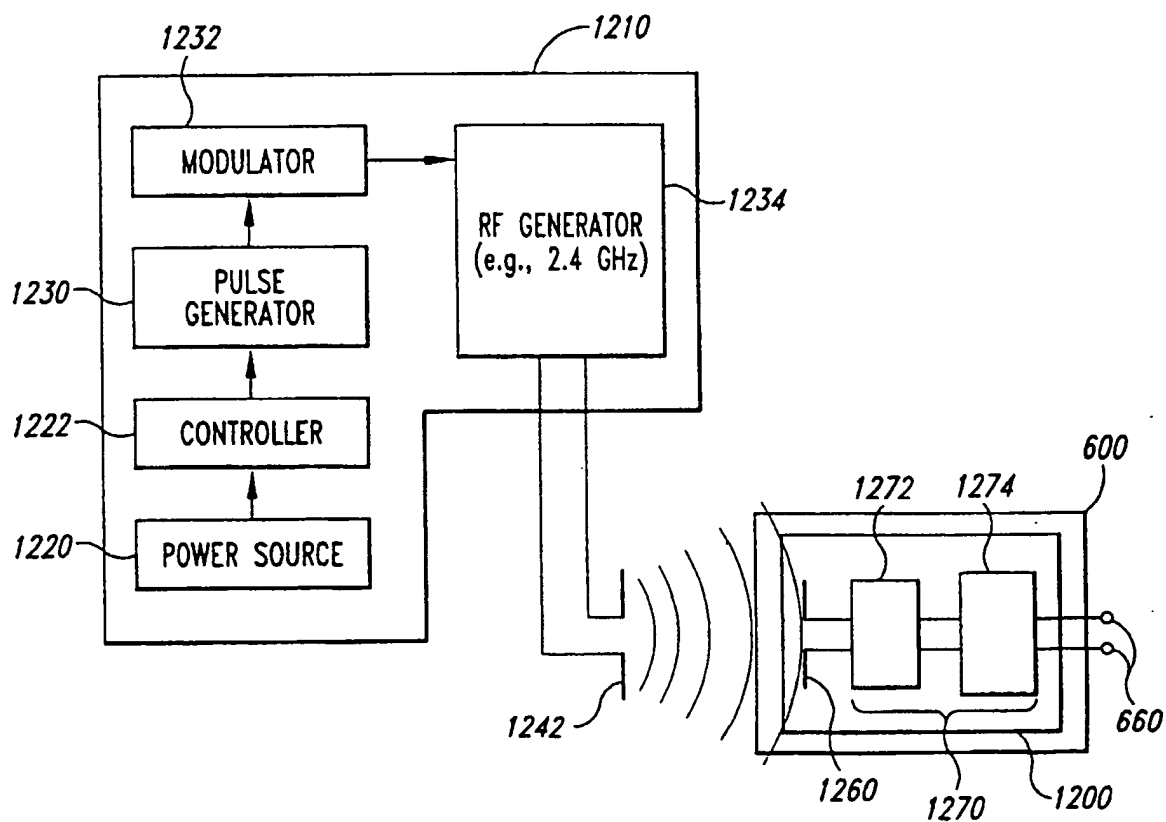
*Fig. 7*

*Fig. 8**Fig. 9*

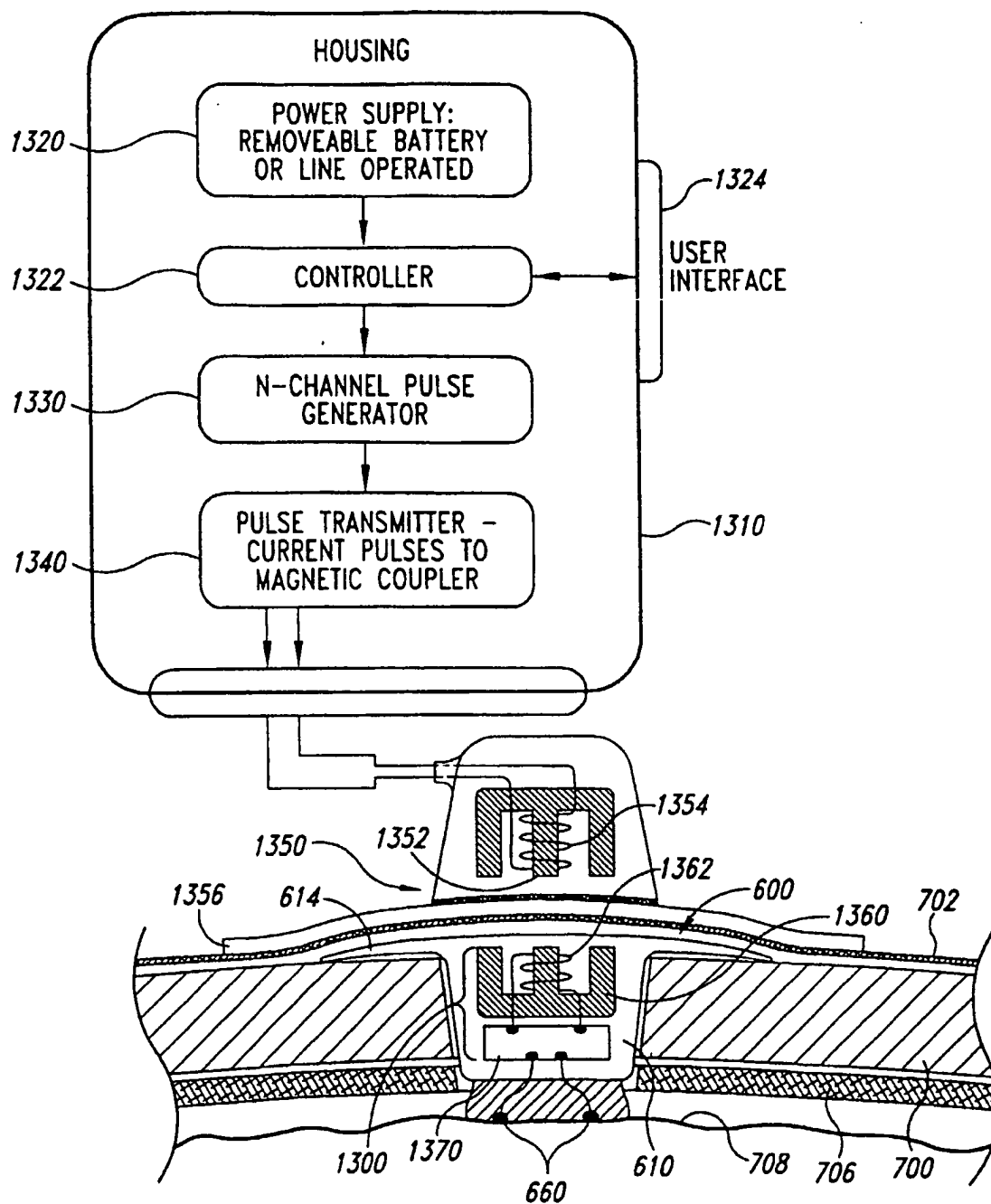
*Fig. 10*



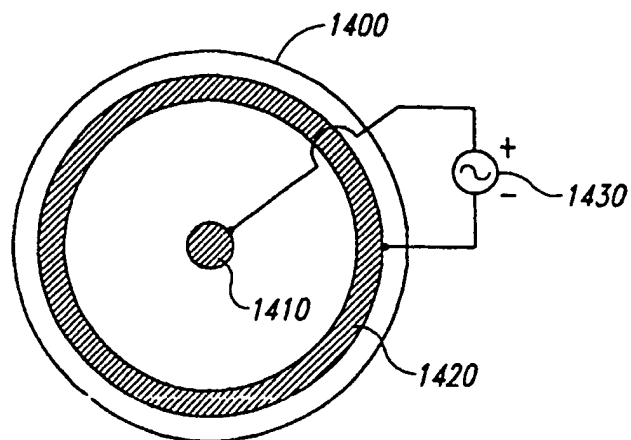
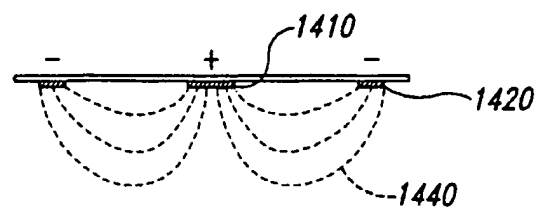
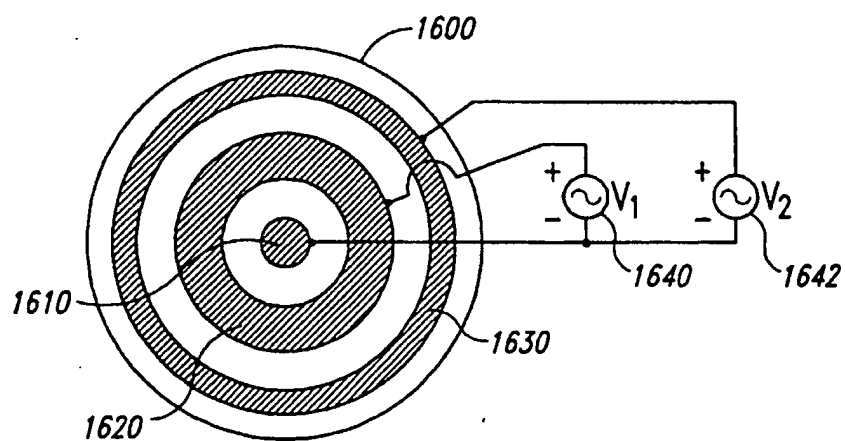
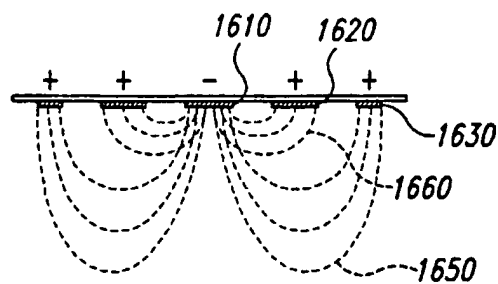
*Fig. 11*



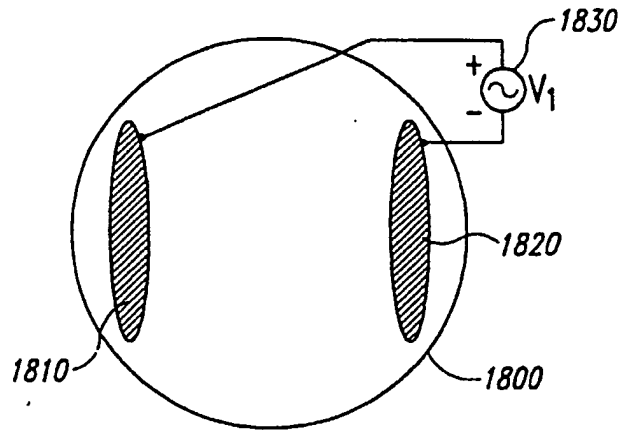
*Fig. 12*

*Fig. 13*

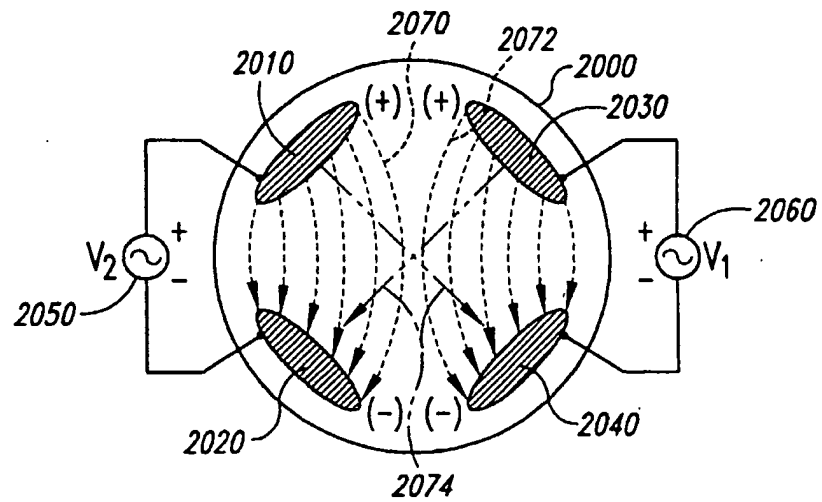
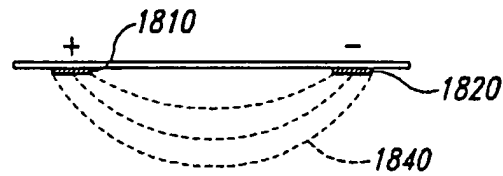


*Fig. 14**Fig. 15**Fig. 16**Fig. 17*

*Fig. 18*



*Fig. 19*



*Fig. 20*

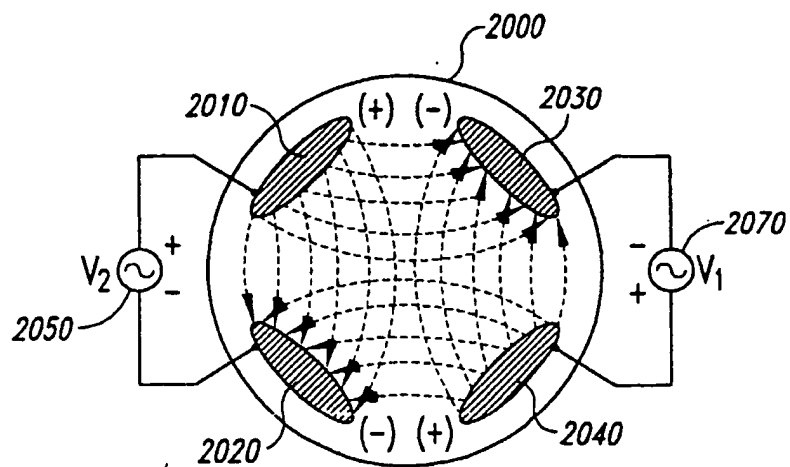
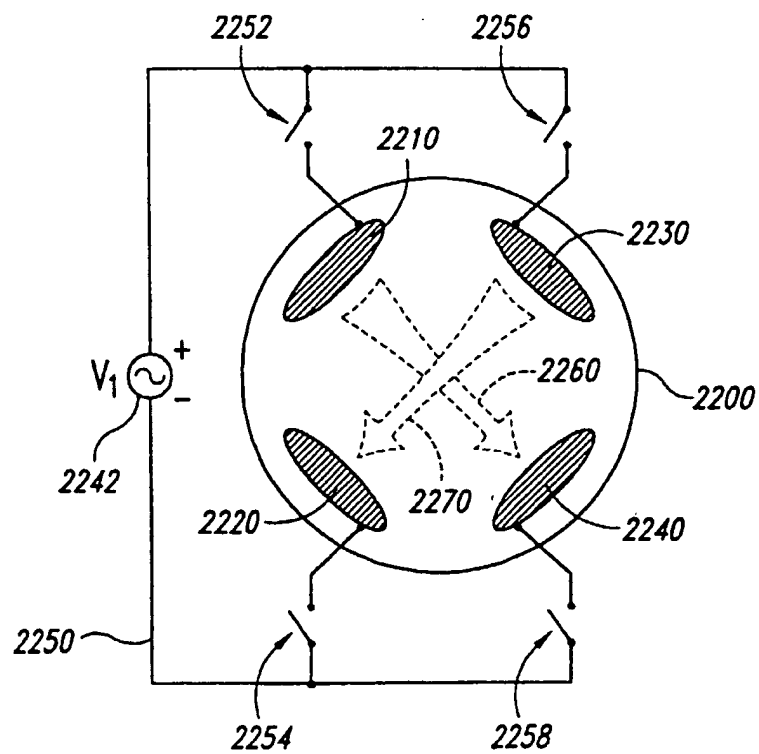
*Fig. 21**Fig. 22*

Fig. 23

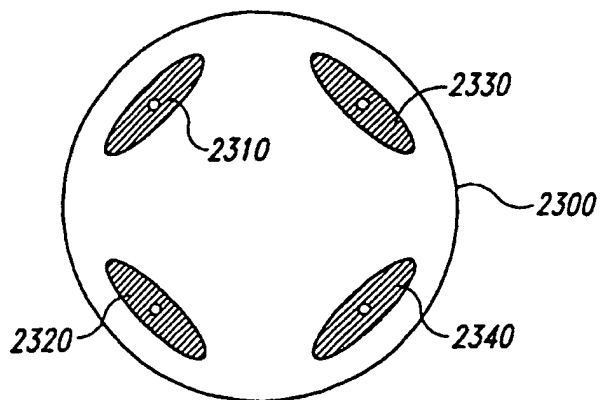
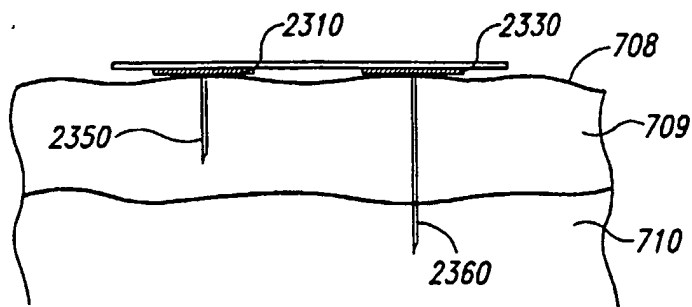


Fig. 24



2500

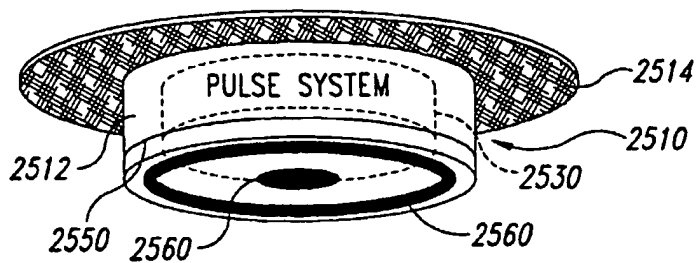


Fig. 25

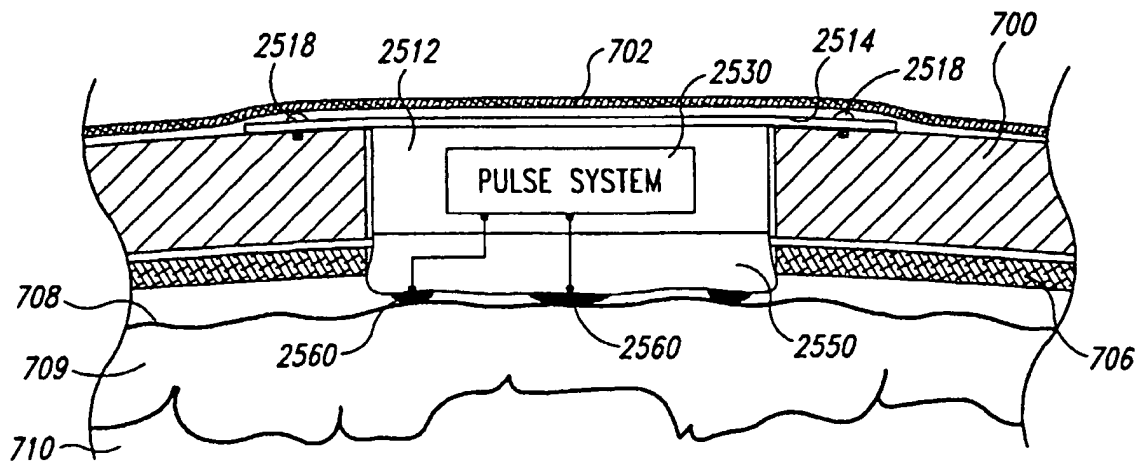
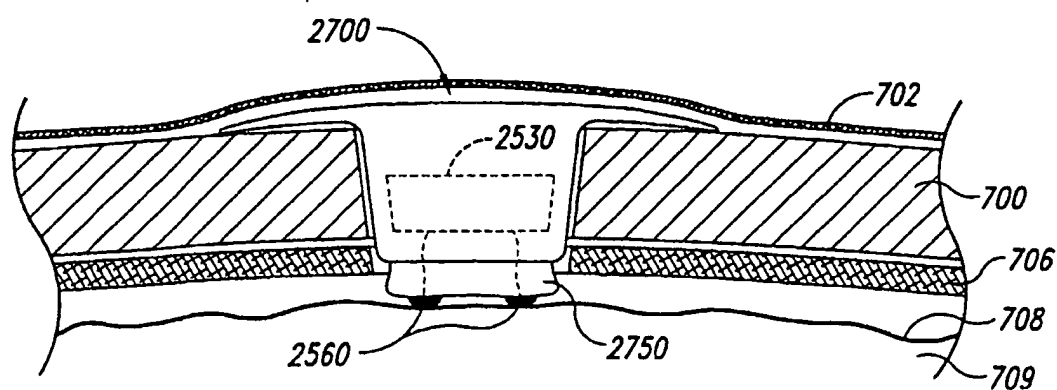
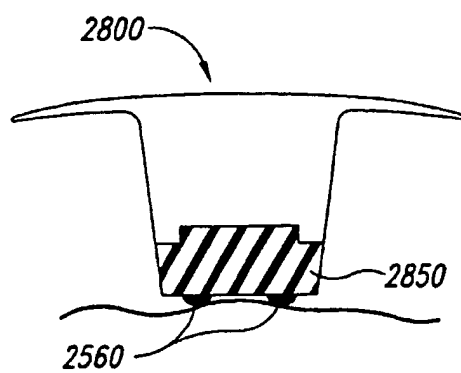
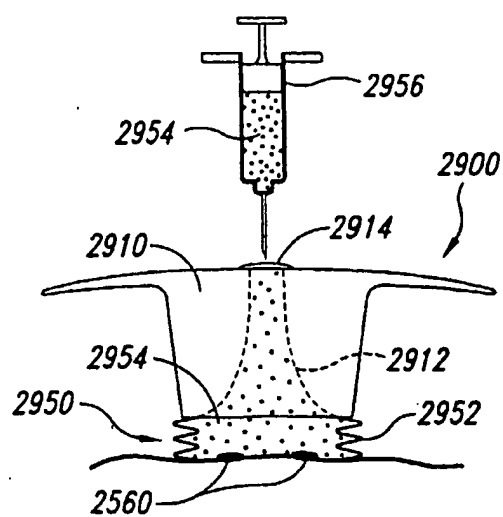
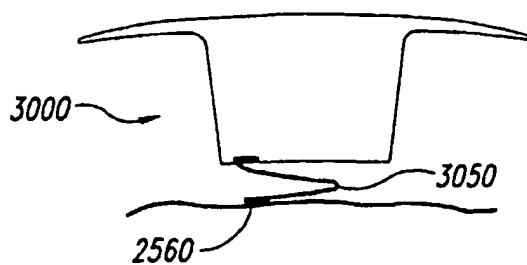
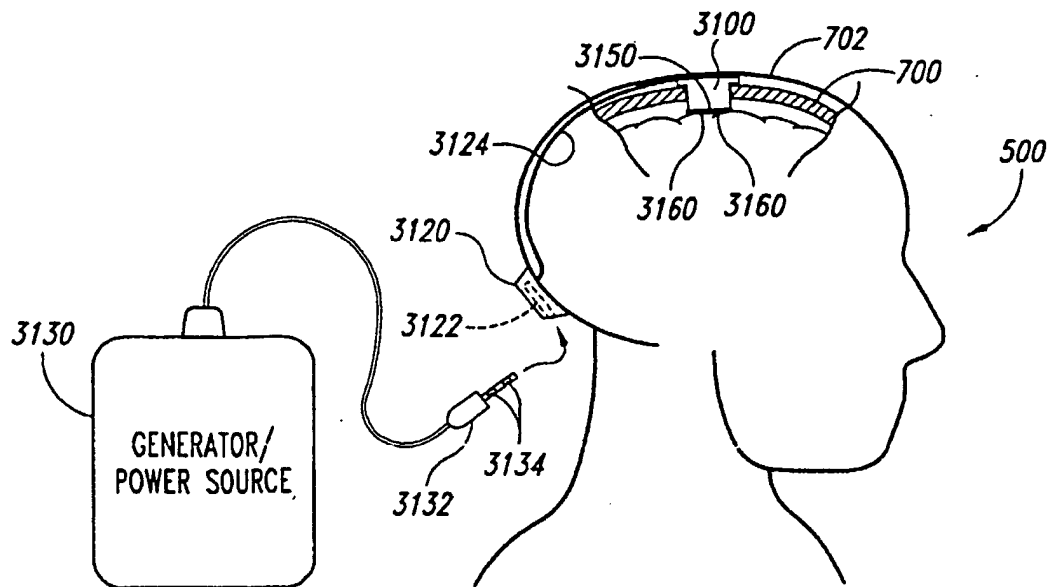
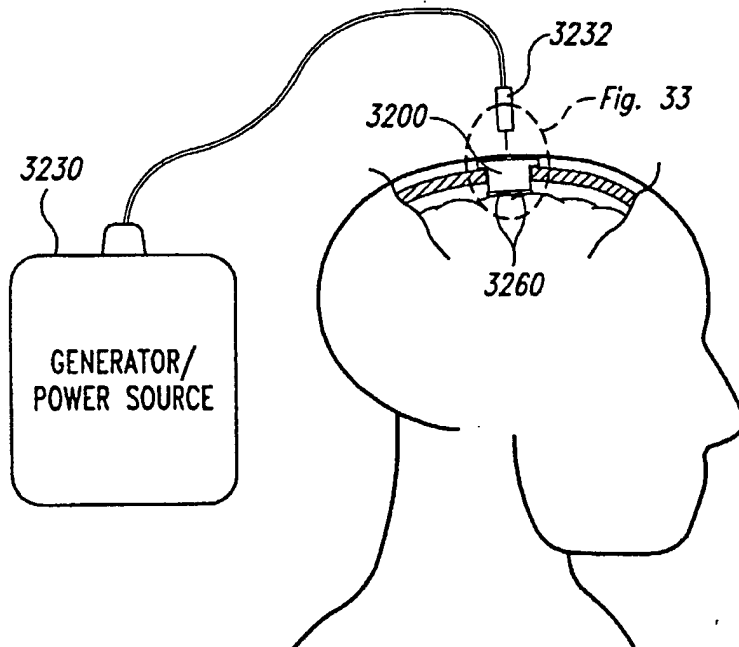


Fig. 26

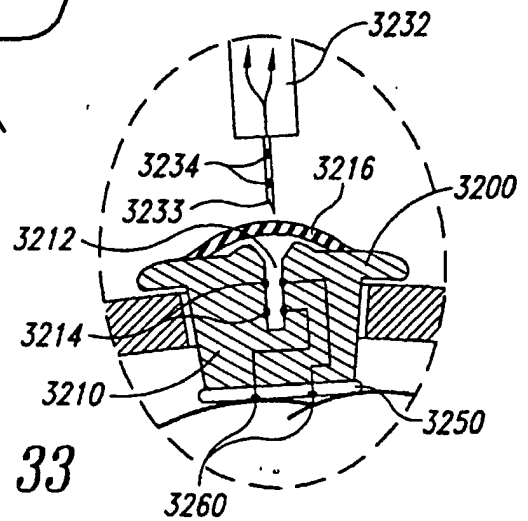
*Fig. 27**Fig. 28**Fig. 29**Fig. 30*



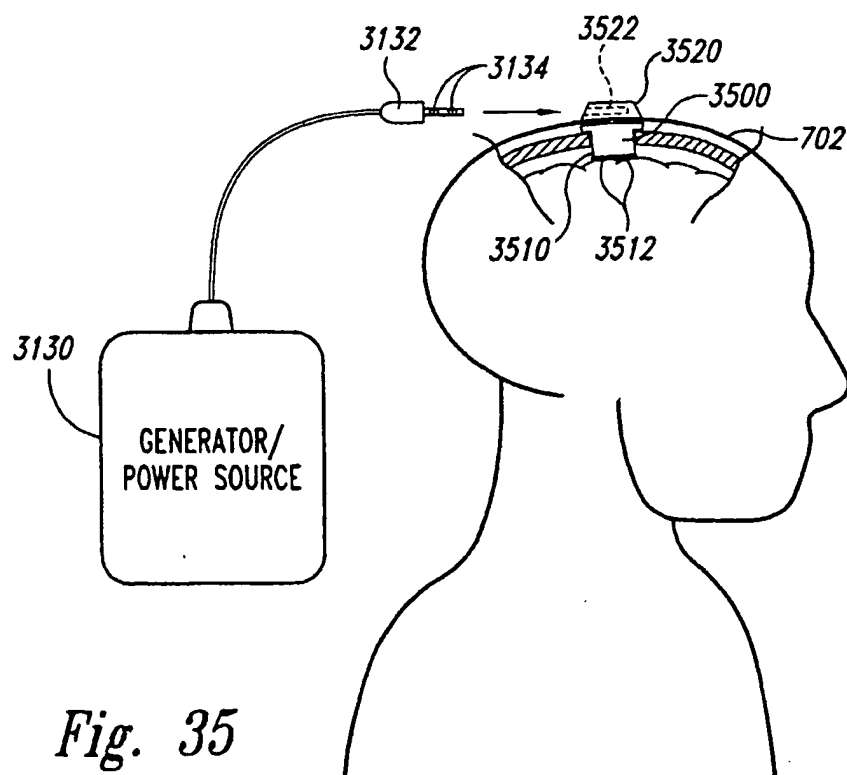
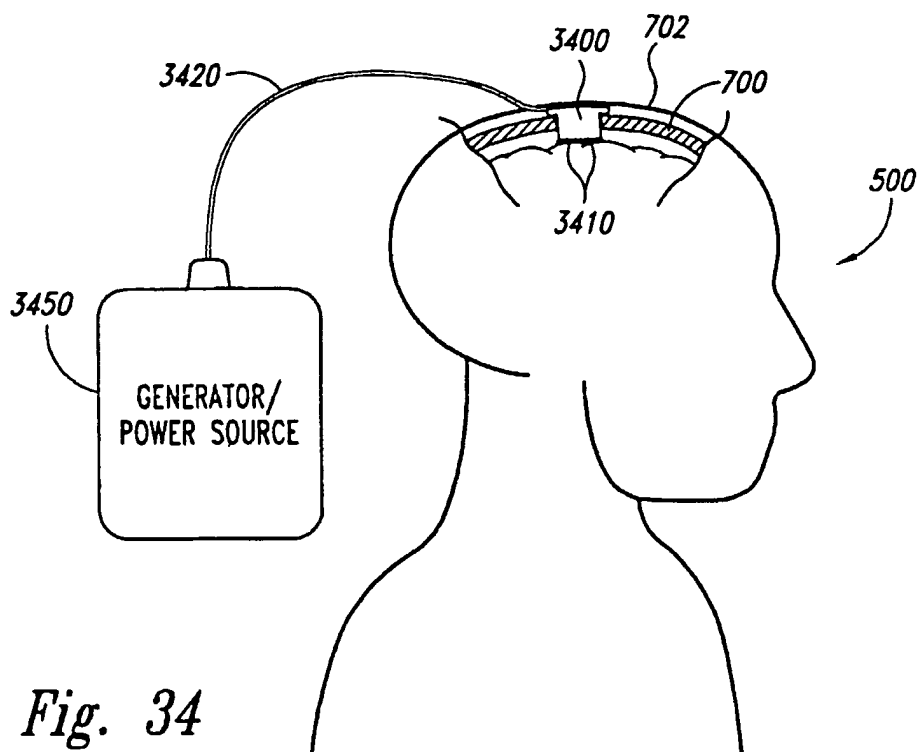
*Fig. 31*

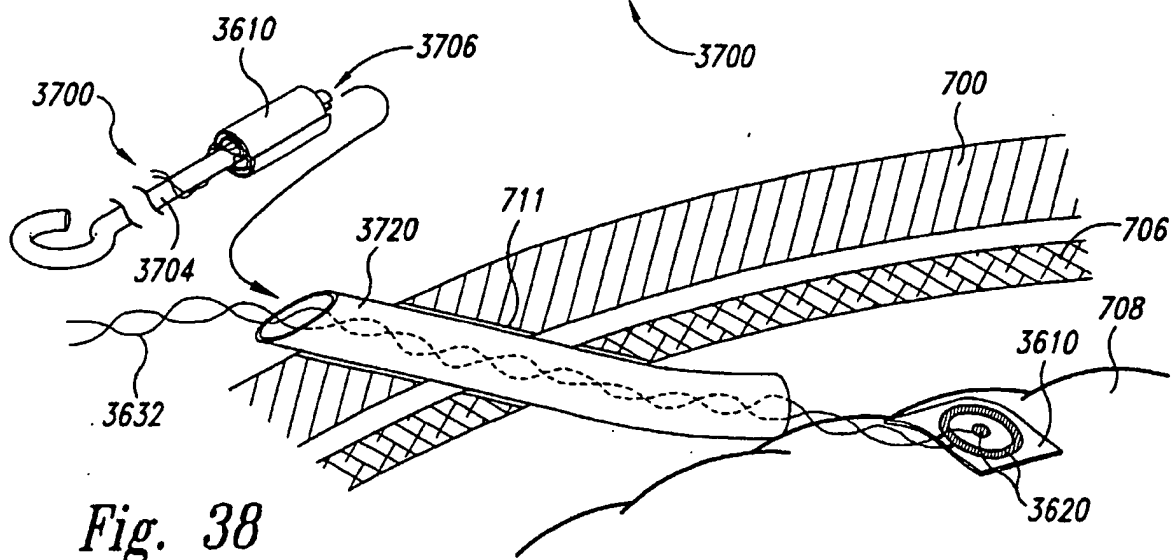
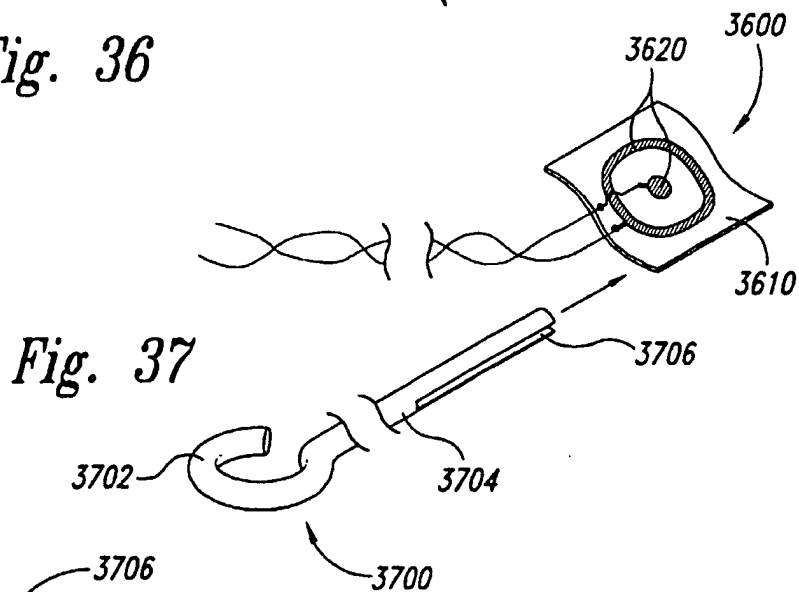
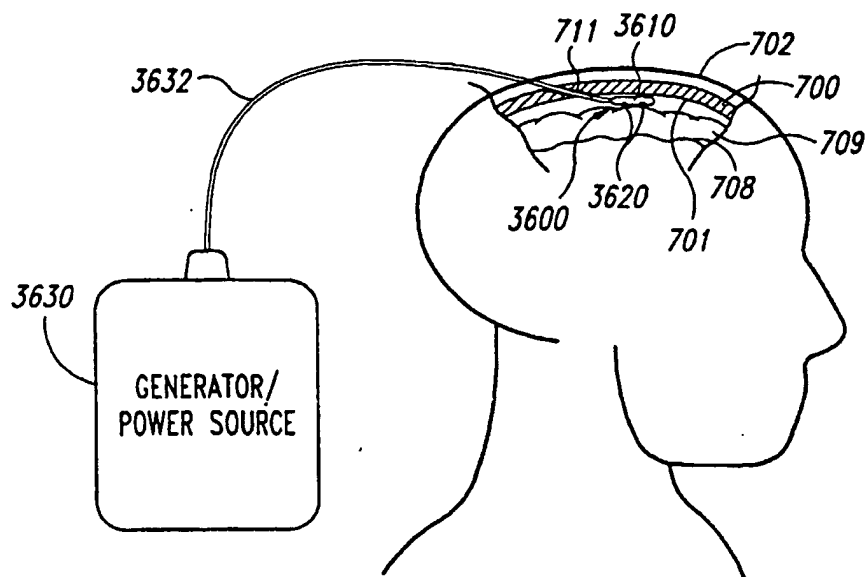


*Fig. 32*

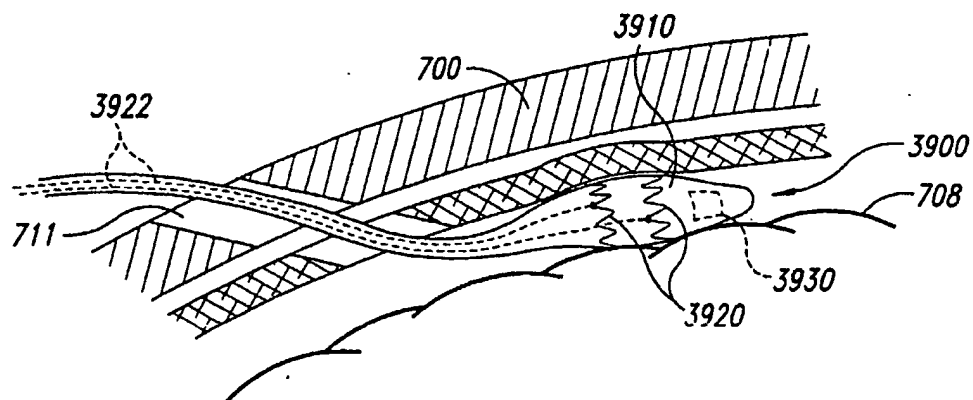
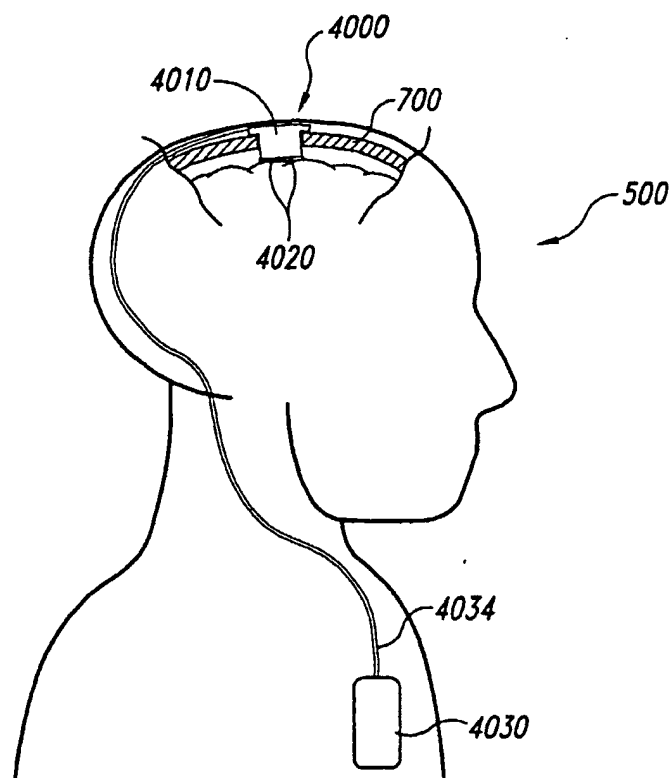


*Fig. 33*







*Fig. 39**Fig. 40*

(19) World Intellectual Property Organization  
International Bureau



(43) International Publication Date  
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PCT

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WA 98006 (US). MORGAN, Carlton, B. [US/US]; 4143 Palomino Drive N.E., Bainbridge Island, WA 98110 (US).

(21) International Application Number: PCT/US02/07077

(74) Agents: PARKER, Paul, T. et al.; Perkins Coie LLP, P.O. Box 1247, Seattle, Washington 98111-1247 (US).

(22) International Filing Date: 7 March 2002 (07.03.2002)

(25) Filing Language: English

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(71) Applicant (*for all designated States except US*): VERTIS NEUROSCIENCE, INC. [US/US]; 2101 Fourth Avenue, Suite 200, Seattle, WA 98121-2329 (US).

(84) Designated States (*regional*): ARIPO patent (GH, GM, KE, LS, MW, MZ, SD, SL, SZ, TZ, UG, ZM, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE, TR), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG).

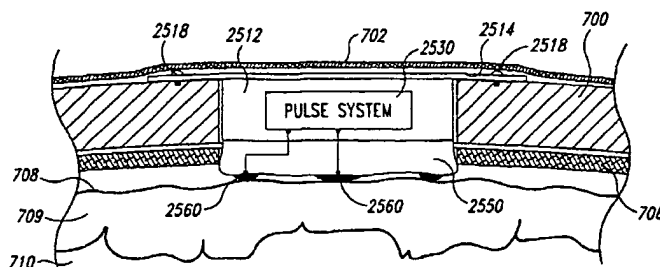
(72) Inventors; and

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[Continued on next page]

(54) Title: METHODS AND APPARATUS FOR EFFECTUATING A LASTING CHANGE IN A NEURAL-FUNCTION OF A PATIENT



(57) Abstract: The following disclosure describes several methods and apparatus for intracranial electrical stimulation to treat or otherwise effectuate a change in neural-functions of a patient. Several embodiments of methods in accordance with the invention are directed toward enhancing or otherwise inducing a lasting change in neural activity to effectuate a particular neural-function. Such lasting change in neural activity is defined as "neuroplasticity". The methods in accordance with the invention can be used to treat brain damage (e.g., stroke, trauma, etc.), brain disease (e.g., Alzheimer's, Pick's, Parkinson's, etc.), and/or brain disorders (e.g., epilepsy, depression, etc.). The methods in accordance with the invention can also be used to enhance neural-function of normal, healthy brains (e.g., learning, memory, etc.), or to control sensory functions (e.g., pain). Certain embodiments of methods in accordance with the invention electrically stimulate the brain at a stimulation site where neuroplasticity is occurring. The stimulation site may be different than the region in the brain where neural activity is typically present to perform the particular neural function according to the functional organization of the brain. In one embodiment in which neuroplasticity related to the neural-function occurs in the brain, the method can include identifying the location where such neuroplasticity is present. In an alternative embodiment in which neuroplasticity is not occurring in the brain, an alternative aspect is to induce neuroplasticity at a stimulation site where it is expected to occur. Several embodiments of these methods that are expected to produce a lasting effect on the intended neural activity at the stimulation site use electrical pulses that increase the resting membrane potential of neurons at the stimulation site to a subthreshold level.

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(88) Date of publication of the international search report:  
6 March 2003

*For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.*

## INTERNATIONAL SEARCH REPORT

International Application No

PCT/US 02/07077

A. CLASSIFICATION OF SUBJECT MATTER  
IPC 7 A61N1/36

According to International Patent Classification (IPC) or to both national classification and IPC

## B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)  
IPC 7 A61N

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal

## C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 6 128 538 A (UPTON ADRIAN R M ET AL) 3 October 2000 (2000-10-03)  the whole document	1,8-12, 25-30, 32-37, 54,60,66
X	WO 95 21591 A (UNIV IOWA RES FOUND) 17 August 1995 (1995-08-17) the whole document	1,25,32, 54,60,66
P,X	WO 01 97906 A (ADVANCED BIONICS CORP) 27 December 2001 (2001-12-27)  the whole document	1,8-12, 25-30, 32-37



Further documents are listed in the continuation of box C.



Patent family members are listed in annex.

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Date of the actual completion of the international search

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Authorized officer

Ferrigno, A

# INTERNATIONAL SEARCH REPORT

International application No.  
PCT/US 02/07077

## Box I Observations where certain claims were found unsearchable (Continuation of item 1 of first sheet)

This International Search Report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. ☒ Claims Nos.: 69-138  
because they relate to subject matter not required to be searched by this Authority, namely:  
Rule 39.1(iv) PCT - Method for treatment of the human or animal body by therapy and surgery
2. ☐ Claims Nos.:  
because they relate to parts of the International Application that do not comply with the prescribed requirements to such an extent that no meaningful International Search can be carried out, specifically:
3. ☐ Claims Nos.:  
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

## Box II Observations where unity of invention is lacking (Continuation of item 2 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

1. ☐ As all required additional search fees were timely paid by the applicant, this International Search Report covers all searchable claims.
2. ☐ As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3. ☐ As only some of the required additional search fees were timely paid by the applicant, this International Search Report covers only those claims for which fees were paid, specifically claims Nos.:
4. ☐ No required additional search fees were timely paid by the applicant. Consequently, this International Search Report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

- ☐ The additional search fees were accompanied by the applicant's protest.
- ☐ No protest accompanied the payment of additional search fees.

# INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/US 02/07077

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(54) **System for optimized brain stimulation**  
System für eine optimierte Gehirnstimulation  
Système pour une stimulation cérébrale optimisée

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(30) Priority: **05.11.1998 US 186490**

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**179 Queen Victoria Street**  
**London EC4V 4EL (GB)**

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**US-A- 5 065 083**                      **US-A- 5 702 429**

**EP 0 998 958 B1**

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## Description

[0001] This invention lies in the field of systems for brain stimulation and recording of brain activity and, more particularly, systems for placement of the lead for stimulating and/or recording at an optimized physiological brain target, for the treatment of conditions such as movement disorders.

[0002] Deep Brain Stimulation (DBS) has been found to be successful in treating a variety of brain-controlled disorders, including movement disorders. Generally, such treatment involves placement of a DBS type lead through a burr hole drilled in the patient's skull, followed by placement of the lead and then applying appropriate stimulation through the lead to the physiological target. The placement portion of the treatment is very critical, and has been the subject of much attention and research. In particular, finding the deep brain target and then placing the permanent lead so that it efficiently stimulates such target is very important. See, for example, U.S. Patent No. 6,011,996, filed January 20, 1998, Gielen et al, which deals with the localization procedure in functional stereotactic brain surgery, i.e., the initial probing to find the optimum site for delivering the stimulation.

[0003] US 5,702,429 discloses a neural stimulation device comprising an implanted lead having a stimulation electrode and a recording electrode.

[0004] WO 97/39796 discloses apparatus for brain stimulation by means of an implantable signal generator and electrode.

[0005] Finding the optimal physiological target in deep brain stimulation implants for the treatment of movement disorders is a particularly complicated task. This is especially true for the treatment of symptoms which cannot be tested at the operating table during lead implant. For instance, it is impossible to test walking and postural stability in Parkinson's Disease (PD) patients during DBS lead implant. Two other major PD symptoms, Rigidity and Akinesia, are also considered difficult to evaluate quantitatively during DBS lead implant. Thus far, no reliable quantitative evaluation procedures exist that can be performed during the surgical DBS implant procedure for these major symptoms.

[0006] A recent procedure has been suggested which allows post-operative quantitative testing of muscle function in PD. See Pascual-Leone, Rapid Rate Transcranial Magnetic Stimulation (rTMS) in Movement Disorders; Movement Disorders, Vol 11, Suppl. #1, pp.:23, 1966. In this procedure, trans-cranial magnetic stimulation of the motor cortex is used to show that the brain is able to control muscle movements in a normal way when and if the DBS electrode is implanted in the optimal physiological position in the Globus Pallidum Internae (GPi) and electrical stimulation with the appropriate parameters is applied through the DBS electrode. Thus, it was shown that those areas of the motor cortex (MC) which are involved in the control of movement in the

muscle of the thumb can only be activated if the appropriate DBS stimulation is concurrently applied to the correct part of the GPi.

[0007] Based on this finding, it is reasonable that an improved procedure could be utilized for optimizing the implant position of the DBS electrode(s) in the GPi or other neuro-modulation target for treating disorders, and particularly movement disorders, by means of deep brain stimulation. Thus, if postural instability of the patient is a major PD symptom, one might be able to find the optimal physiological target for the DBS electrode by seeing when trans-cranial magnetic stimulation of the motor cortex achieves optimal control movement of the leg muscles. However, this magnetic stimulation procedure is not suitable for intra-operative use, i.e., for testing lead position while the lead is stereotactically held. The applied very fast changing and very strong magnetic fields may interact with the DBS electrode in a comparable way as suggested for MRI imaging procedures, which is contra-indicated for DBS patients. Further, the trans-cranial magnetic stimulation coil cannot be accessed to the relevant sites of the brain when the DBS lead is being held by the stereotactic equipment. This means that the Leone procedure is not directly suggested for use in evaluating the excitability of the relevant motor cortex areas during lead implant. Thus, while the prior art procedure is appropriate for certain post-surgical testing because it is non-invasive, it is not suggested for intra-operative use.

[0008] The continued need in the art is a system and procedure that can be utilized during surgery when the DBS lead is being implanted, to determine when it has been placed in the optimal position for stimulation therapy of the patient's particular disorder, or for recording of brain activity. In general terms, the aim is a system for stimulation of the GPi or other neuro-stimulation target, and a feedback target such as the MC. A key to this invention is the recognition that during surgery, there is no need for a non-invasive way of stimulating the feedback target. The invention, rather, provides apparatus for testing for the optimal DBS electrode position during the invasive surgery, and as part of the localization test procedure that is required in any event, enabling a reliable determination of optimal lead placement before permanent lead implant and close of surgery.

[0009] A primary object of this invention is to provide a system for determining with a test lead or permanent lead when a brain electrode is positioned optimally so during stimulation of the brain target normal patient excitability of a feedback target such as the motor cortex achieves the desired result, e.g., the desired body movement of a patient with a movement disorder. Alternatively, another object is to provide an improved capacity to record brain activity.

[0010] The invention takes advantage of the fact that during DBS lead implant, the patient's brain is already subject to an invasive procedure. This being the case, both the neuro-modulation target and the feedback tar-



get can be readily stimulated during surgery. Thus, in the case of movement disorders involving the motor cortex, the stimulation of the motor cortex concurrently with the GPi need not be limited to a non-invasive technique.

[0011] In order to achieve the above objects, the invention provides a brain stimulation system, comprising a brain stimulator or device and lead means for placement of electrodes at predetermined positions within a patient's brain, said brain stimulator device having first pulse means for generating feedback pulses for stimulating a feedback target in the patient's brain and second pulse means for generating DBS pulses for stimulating a neuro-modulation target in said patient's brain; and said lead means being ' connected to said device for conducting said pulses from said device to said respective targets, said lead means comprising a DBS electrode and a conductor for conducting said DBS pulses from said second pulse means to said DBS electrode, a feedback electrode and a conductor for conducting said feedback pulses from said first pulse means to said feedback electrode, and said DBS and feedback electrodes being positioned on said lead means relative to each other so that when said DBS electrode is positioned at said neuro-stimulation target said feedback electrode is positioned at said feedback target.

[0012] By varying the position of the DBS electrodes, and repeatedly stimulating both the DBS target and the feedback target, and observing the relevant patient body movement or other reaction, the optimal DBS target location can be found. Also, either or both of the electrodes can be used for recording brain activity.

[0013] After the finding of the optimal DBS target location, the test lead is removed and a permanent lead positioned so that the DBS electrode(s) is located at the optimal target position. The permanent lead also preferably is aligned along the linear trajectory which includes both the neuro-modulation and the feedback targets, and carries electrodes for stimulating or recording at both targets, thereby enabling post-operative testing. The system preferably includes a generator device with dual stimulus pulse channels for providing stimuli with appropriate parameters for stimulating the respective targets, and sense channels for amplifying and processing detected brain signals.

[0014] Preferred embodiments will now be described, by way of example only, with reference to the drawings.

Figure 1 is a diagrammatic view of a patient's skull and the target path or paths taken to stimulate target areas of the brain in accordance with use of the system of this invention, and/or to record brain activity at the dual target sites.

Figure 2 is a schematic diagram showing a system in accordance with this invention, including an implantable stimulator/recorder device, and a test or permanent lead designed to enable dual stimulation of different brain sites and/or recording of brain signals from such sites.

Figure 3A is a diagrammatic view showing a brain stimulating lead and a slidable sleeve with a window; Figure 3B is a diagrammatic view showing the sleeve in position over the lead portion which carries electrodes for stimulating the motor cortex, thereby enabling adjustment of the location of an effective electrode on the lead for stimulating the motor cortex at the same time that the physiological brain target is stimulated.

Figure 4 is a flow diagram illustrating the primary steps taken in using the system of this invention to determine whether and when the brain lead has been optimally positioned in a patient's brain in order to treat a movement disorder or the like.

[0015] Referring now to Figure 1, there is shown a diagram of a patient's head, with burr holes BH-A and BH-B shown drilled through the patient's skull to allow entry beneath the dura. While Figure 1 presents an illustration of the specific MC/GPi embodiment, it is to be understood that the principles involved are equally applicable to other targets, as discussed above. A normal trajectory would be that indicated through the hole BH-A, along trajectory A, to the GPi. However, as indicated, the motor cortex MC is not along this line. In order to have a single one-dimensional trajectory which will involve both the GPi and the MC, burr hole BH-B is utilized, to provide a trajectory as indicated along indicated line B. It is to be noted that skull sizes vary from patient to patient, and that accordingly the distance from the GPi target and the MC target will be variable, perhaps in the range of up to 2 cm from patient to patient. For this reason, the lead of this invention preferably includes an adjustable electrode location for stimulating the feedback target, e.g., the MC, when the distal electrodes are in place for stimulating the GPi or other brain target.

[0016] Referring now to Figure 2, there is shown a diagram of a stimulator/recorder device 30 coupled to and used in connection with a lead 40. Stimulator device 30 may be, for example, a Medtronic Model 3628, or a modification thereof; and the lead may be a modification of Medtronic InterStim Model 4300 or Medtronic DBS Lead Model 3387. As indicated, the stimulator device contains two pulse generation channels, channel 1 indicated at 32 and channel 2 at 34. Each of these channels is controlled by control block 35, which may appropriately utilize a microprocessor and/or other control and timing circuitry. The lead proximal end 41 is connected to the outputs of the device 30. Channel 1 connects to one or more lead conductors which provide electrical connection to distal electrodes indicated at 46 near the lead distal end 42. These electrodes are positioned at the neuro-modulation target, e.g., the GPi. The pulses generated by channel 1 and delivered to the deep brain location are, for example, pulses of 60-120  $\mu$ s pulse width, typically delivered at a rate in the range of about 50-250 Hz, and with a pulse amplitude of about 1-10 v. The signals delivered by channel 2 are connected through to

electrode 44, which is shown positioned proximally from electrodes 46, and at a distance in the neighborhood of 3-8 cm from the distal electrodes 46, depending on the application. For example, for the MC/GPi embodiment, the positioning of electrode 44 is designed to place it proximate to the motor cortex when the distal electrodes 46 are positioned at the GPi brain target. The pulses delivered by channel 2 are, e.g., pulses of a width 1-10 ms, delivered at a rate of 1 to 5 Hz and with a voltage in the range of 1-10 v. Signals received from the electrodes are processed at sense channels 37,38 and stored at 39.

[0017] Referring now to Figures 3A and 3B, there is shown one arrangement for adjusting the position of electrode 44, to provide for stimulation of the MC concurrently with stimulation of the GPi. In this embodiment, electrode 44 is suitably comprised of a series of smaller ring electrodes, as indicated at 48, the purpose of this design being to achieve a greater lead flexibility. Alternatively, but at the cost of some flexibility, the electrode 44 may be one integral ring electrode, providing a large surface extending around the tubular body 43 of lead 40. Shown above the lead portion carrying electrode 44 is a sliding tubing, or sleeve 50, being a hollow tubing having an inner diameter adapted to just fit over the outer diameter of lead body 43. Tubing 50 is made of an electrically insulative material coating 51, except at a window portion 52 of predetermined length. The tubing 50 extends proximally a sufficient distance so that it can be manipulated, i.e., slid along the lead 43 so as to position the window portion 52 relative to the lead. In Figure 3B, the tubing is illustrated as having been slid down to register with a portion of the rings 48, providing an electrode which is adjustable along the axis of the lead by positioning of the window.

[0018] Referring now to Figure 4, there is illustrated a flow diagram of the primary steps taken in carrying out the procedure of this invention, illustrated with respect to the MC/GPi embodiment. At block 60, the test is initiated by providing a test lead as discussed in connection with Figures 2 through 3B above. Such a test lead is provided with respective MC and GPi electrodes, where the position of the MC electrode is preferably adjustable to account for required patient variations in inter-electrode distance, as discussed in connection with Figure 1. The location of the GPi and the MC are then preliminarily determined, as indicated at 62. The approximate location of the GPi can be determined non-invasively; a more exact location of the GPi target can be determined as discussed in the above referenced U. S. Patent No. 6,011,996. The location of the MC can be determined, e.g., by trans-cranial magnetic stimulation. With this information having been obtained, the desired one-dimensional trajectory through the two targets is known. Next, at 64, a burr hole is drilled to provide entry through the skull for the desired linear trajectory. Note that if a first burr hole is drilled in order to perform the initial localization, it can be used for placement of a sep-

arate lead to the GPi, as discussed above. Then, as indicated at 65, the test lead is stereotactically introduced along the trajectory, and the distal DBS electrode positioned in the area of the GPi. After that, at 66, the position of the MC electrode 44 is adjusted, e.g., in the manner suggested by the discussion of Figures 3A, B. The positioning of electrode 44 with respect to the MC will, of course, depend upon what body portion is to be tested or treated. After this, at 68, the two targets are stimulated, and the relevant body movement, or lack thereof, is noted. This provides the feedback for determining when the DBS electrode has been optimally located. Also, at 68, brain activity at the two sites can be recorded.

[0019] At 70, it is determined whether the DBS electrode complex 46 is optimally located. If no, which would include a state of uncertainty, the position of the DBS electrode is adjusted, as shown at 72, and then the stimulation is repeated, as indicated by the branch that loops back to 68. When the physician is satisfied that an optimal position has been found, the test is concluded, and the permanent lead is implanted, as indicated at 74. The lead is then attached to the generator device, and the patient is chronically stimulated, as indicated at 76.

As mentioned above, by providing a permanent lead that also has an MC electrode, and is placed along the trajectory that encompasses both targets, subsequent tests can be conducted. Further, brain signal recordings can be obtained from the electrode sites, either concurrently, or at one site during stimulation of the other site.

[0020] There is thus provided a system for stimulating or recording at dual sites in a patient's brain, e.g., a feedback site such as the motor cortex, and a deep brain or neuro-modulation site such as the GPi. While the preferred embodiment has been presented as a single lead, either a test or permanent lead, it is to be understood that the invention can likewise be practiced by insertion of two leads, e.g., one for positioning of an electrode at the motor cortex and one for positioning of an electrode at the GPi. As used herein, the term "electrode" means either a single electrode or a plurality of electrodes, as illustrated in Figures 2 and 3A.

## Claims

1. A brain stimulation system, comprising a brain stimulator device (30) and lead means (40) for placement of electrodes at predetermined positions within a patient's brain,

said brain stimulator device having first pulse means (32) for generating feedback pulses for stimulating a feedback target in the patient's brain and second pulse means (34) for generating deep brain stimulation DBS pulses for stimulating a neuro-modulation target in said patient's brain; and  
said lead means (40) being connected to said

- device for conducting said pulses from said device to said respective targets, **characterised in that** said lead means comprising a DBS electrode (46) and a conductor for conducting said DBS pulses from said second pulse means to said DBS electrode, a feedback electrode (44) and a conductor for conducting said feedback pulses from said first pulse means to said feedback electrode, and said DBS and feedback electrodes being positioned on said lead means relative to each other so that when said DBS electrode is positioned at said neuro-stimulation target said feedback electrode is positioned at said feedback target.
2. The system as described in claim 1, wherein said lead means is a single lead (40), and said DBS electrode (44) is positioned near the lead distal end and said feedback electrode is positioned about 3-8 cm from said DBS electrode, whereby said lead can be inserted into the patient's brain along a predetermined path to position said electrodes at said respective feedback and neuro-modulation targets.
  3. The system as described in claim 2, wherein said lead comprises adjusting means for adjusting the position of said feedback electrode to be positioned at the patient's motor cortex when said DBS electrode is positioned at said patient's GPI.
  4. The system as described in claim 3, wherein said lead has a lead body, and said adjusting means comprises a slidable tubing (50) having a window (52), said tubing being slidable over said lead body to expose said feedback electrode at a desired position relative to the motor cortex.
  5. The system as described in claim 4, wherein said feedback electrode has an effective surface area larger than the area of said window.
  6. The system as described in any preceding claim, wherein said first pulse means comprises MC generator means for generating pulses at a rate of about 1-5 Hz for delivery to the patient's motor cortex, and parameter means for controlling said generated pulses to have a duration of about 1-10 ms and a voltage of about 1-10 Volts.
  7. The system as described in any preceding claim, wherein said second pulse means comprises DBS target means for generating pulses at a rate of about 50-250 Hz, and parameter means for controlling generation of said pulses to have a duration in the range of about 60-120  $\mu$ s and a voltage in the range of about 1-10 Volts.
  8. The system as described in any preceding claim,

wherein said brain stimulator device further comprises means (37, 38) for receiving signals from at least one of said electrodes and means (39) for recording such signals.

## Patentansprüche

1. Gehirnstimulationssystem mit einer Gehirnstimulatorvorrichtung (30) und einem Leitungsmittel (40) zum Anordnen von Elektroden an vorgegebenen Positionen innerhalb des Gehirns eines Patienten, wobei die Gehirnstimulatorvorrichtung ein erstes Impulsmittel (32) zum Erzeugen von Rückkopplungsimpulsen zum Stimulieren eines Rückkopplungstargets im Gehirn des Patienten und ein zweites Impulsmittel (34) zum Erzeugen tiefer Gehirnstimulations-DBS-Impulse zum Stimulieren eines Neuro-modulationstargets im Gehirn des Patienten aufweist, und das Leitungsmittel (40) mit der Vorrichtung verbunden ist, um die Impulse von der Vorrichtung zu den jeweiligen Targets zu leiten, **dadurch gekennzeichnet, dass** das Leitungsmittel eine DBS-Elektrode (46) und einen Leiter zum Leiten der DBS-Impulse von dem zweiten Impulsmittel zu der DBS-Elektrode, eine Rückkopplungselektrode (44) und einen Leiter zum Leiten der Rückkopplungsimpulse von dem ersten Impulsmittel zu der Rückkopplungselektrode aufweist und die DBS- und die Rückkopplungselektrode so in Bezug zueinander an dem Leitungsmittel positioniert sind, dass die Rückkopplungselektrode an dem Rückkopplungstarget positioniert ist, wenn die DBS-Elektrode an dem Neurostimulationstarget positioniert ist.
2. System nach Anspruch 1, wobei das Leitungsmittel eine einzige Leitung (40) ist und die DBS-Elektrode (44) in der Nähe des distalen Endes der Leitung positioniert ist und die Rückkopplungselektrode etwa 3 - 8 cm von der DBS-Elektrode positioniert ist, wodurch die Leitung entlang einem vorgegebenen Weg in das Gehirn des Patienten eingeführt werden kann, um die Elektroden an dem jeweiligen Rückkopplungstarget und dem jeweiligen Neuromodulationstarget zu positionieren.
3. System nach Anspruch 2, wobei die Leitung ein Einstellmittel zum Einstellen der Position der Rückkopplungselektrode aufweist, die an der motorischen Hirnrinde des Patienten zu positionieren ist, wenn die DBS-Elektrode am GPI des Patienten positioniert ist.
4. System nach Anspruch 3, wobei die Leitung einen Leitungskörper aufweist und das Einstellmittel ei-

nen verschiebbaren Schlauch (50) mit einem Fenster (52) aufweist, wobei der Schlauch über den Leitungskörper geschoben werden kann, um die Rückkopplungselektrode an einer gewünschten Position in Bezug auf die motorische Hirnrinde freizulegen.

5. System nach Anspruch 4, wobei die Rückkopplungselektrode eine wirksame Oberfläche aufweist, die größer ist als die Fläche des Fensters.

6. System nach einem der vorstehenden Ansprüche, wobei das erste Impulsmittel ein MC-Generatormittel zum Erzeugen von Impulsen mit einer Frequenz von etwa 1 - 5 Hz zur Abgabe an die motorische Hirnrinde des Patienten und ein Parametermittel zum Steuern der erzeugten Impulse, so dass sie eine Dauer von etwa 1 - 10 ms und eine Spannung von etwa 1 - 10 Volt haben, aufweist.

7. System nach einem der vorstehenden Ansprüche, wobei das zweite Impulsmittel ein DBS-Targetmittel zum Erzeugen von Impulsen bei einer Frequenz von etwa 50 - 250 Hz und ein Parametermittel zum Steuern der Erzeugung der Impulse, so dass sie eine Dauer im Bereich von etwa 60 - 120  $\mu$ s und eine Spannung im Bereich von etwa 1 - 10 Volt haben, aufweist.

8. System nach einem der vorstehenden Ansprüche, wobei die Gehirnstimulatorvorrichtung weitere Mittel (37, 38) zum Empfangen von Signalen von mindestens einer der Elektroden und Mittel (39) zum Aufzeichnen solcher Signale aufweist.

## Revendications

1. Système de stimulation cérébrale, comportant un dispositif de stimulation cérébrale (30) et des moyens de branchement (40) pour placer des électrodes à des positions prédéterminées dans le cerveau d'un patient, ledit dispositif de stimulation cérébrale ayant des premiers moyens d'impulsions (32) pour générer des impulsions de rétroaction pour stimuler une cible de rétroaction dans le cerveau du patient et des seconds moyens d'impulsions (34) pour générer des impulsions de stimulation cérébrale profonde (DBS) pour stimuler une cible de neuro-modulation dans ledit cerveau de patient ; et lesdits moyens de branchement (40) étant connectés audit dispositif pour conduire lesdites impulsions à partir dudit dispositif jusqu'auxdites cibles respectives, **caractérisé en ce que** lesdits moyens de branchement comportent une électrode DBS (46) et un conducteur pour conduire lesdites impulsions DBS à partir desdits seconds moyens d'impulsions jusqu'à ladite électrode DBS, une électro-

de de rétroaction (44) et un conducteur pour conduire lesdites impulsions de rétroaction à partir desdits premiers moyens d'impulsions jusqu'à ladite électrode de rétroaction, et lesdites électrodes DBS et de rétroaction étant positionnées sur lesdits moyens de branchement l'une par rapport à l'autre de sorte que lorsque ladite électrode DBS est positionnée au niveau de ladite cible de neuro-stimulation, ladite électrode de rétroaction est positionnée au niveau de ladite cible de rétroaction.

2. Système selon la revendication 1, dans lequel lesdits moyens de branchement sont un branchement unique (40), et ladite électrode DBS (44) est positionnée près de l'extrémité distale de branchement et ladite électrode de rétroaction est positionnée environ à 3 à 8 cm par rapport à ladite électrode DBS, ainsi ledit branchement peut être inséré dans le cerveau du patient le long d'un trajet prédéterminé pour positionner lesdites électrodes au niveau desdites cibles de rétroaction et de neuro-modulation respectives.

3. Système selon la revendication 2, dans lequel ledit branchement comporte des moyens de réglage pour régler la position de ladite électrode de rétroaction de manière à la positionner au niveau du cortex moteur du patient lorsque ladite électrode DBS est positionnée au niveau du Globus Pallidum Internae (GPI) du patient.

4. Système selon la revendication 3, dans lequel ledit branchement a un corps de branchement, et lesdits moyens de réglage comportent un tube coulissant (50) ayant une fenêtre (52), ledit tube pouvant coulisser sur ledit corps de branchement pour exposer ladite électrode de rétroaction à une position voulue par rapport au cortex moteur.

5. Système selon la revendication 4, dans lequel ladite électrode de rétroaction a une surface effective qui est supérieure à la surface de ladite fenêtre.

6. Système selon l'une quelconque des revendications précédentes, dans lequel lesdits premiers moyens d'impulsions comportent des moyens de génération MC pour générer des impulsions à une fréquence d'environ 1 à 5 Hz à appliquer au cortex moteur du patient, et des moyens de paramétrage pour commander lesdites impulsions générées pour qu'elles aient une durée d'environ 1 à 10 ms et une tension d'environ 1 à 10 volts.

7. Système selon l'une quelconque des revendications précédentes, dans lequel lesdits seconds moyens d'impulsions comportent des moyens de cible DBS pour générer des impulsions à une fréquence d'environ 50 à 250 Hz, et des moyens de

paramétrage pour commander la génération desdites impulsions pour qu'elles aient une durée dans la plage d'environ 60 à 120  $\mu$ s et une tension dans la plage d'environ 1 à 10 volts.

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8. Système selon l'une quelconque des revendications précédentes, dans lequel ledit dispositif de stimulation cérébrale comporte de plus des moyens (37, 38) pour recevoir des signaux provenant d'au moins l'un parmi lesdites électrodes et lesdits 10 moyens (39) pour enregistrer ces signaux.

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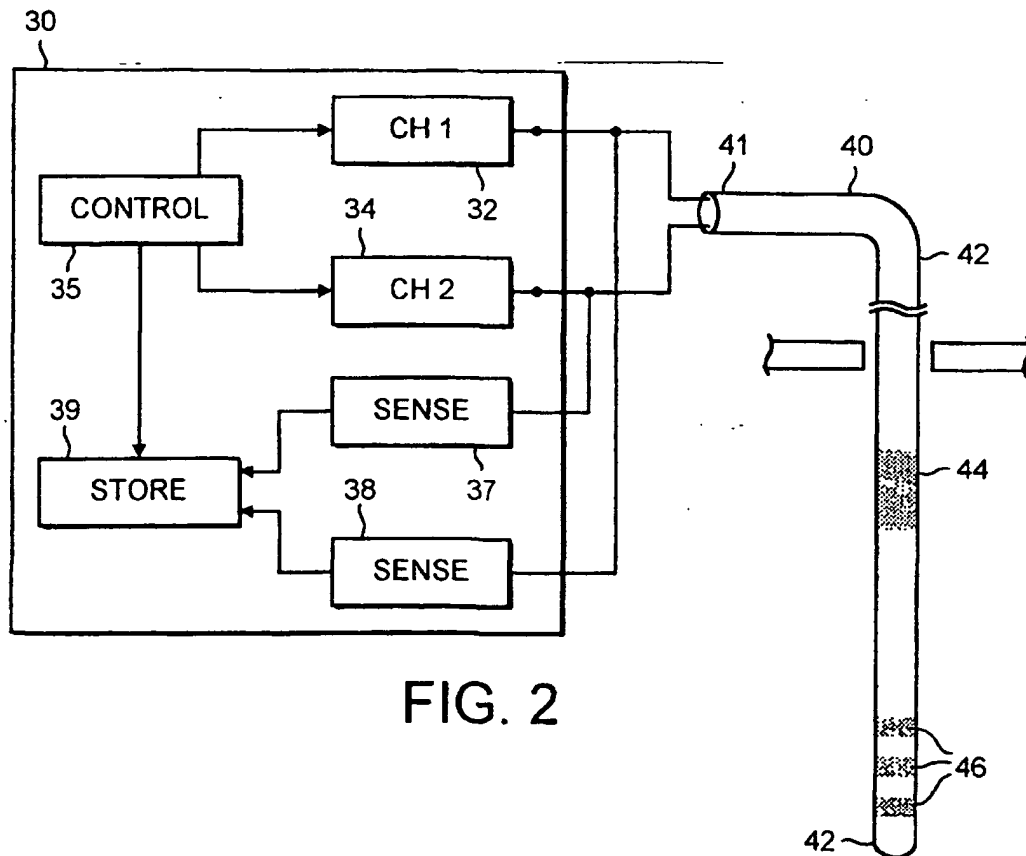
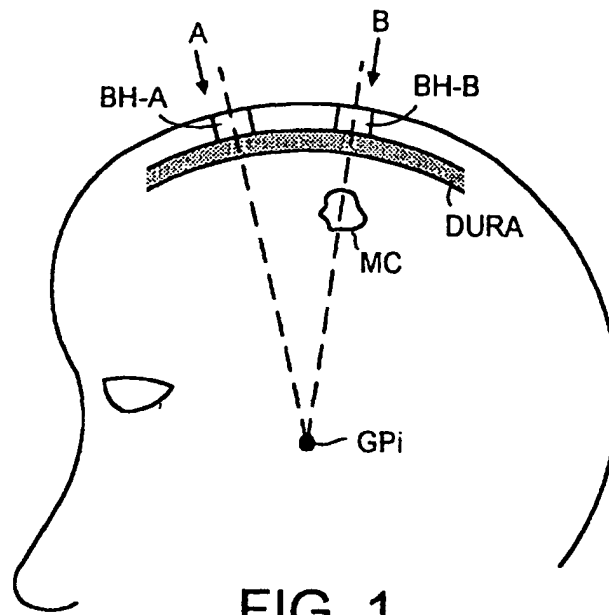
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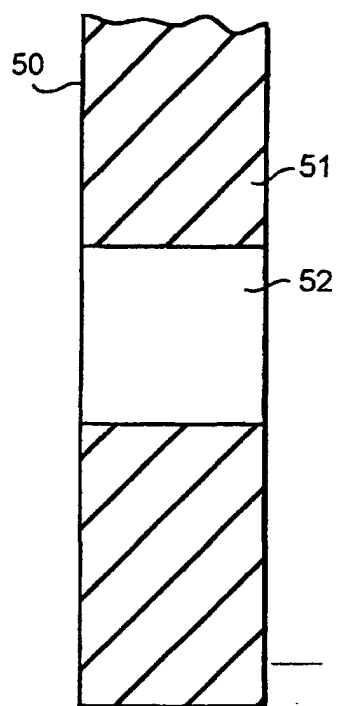


FIG. 3A

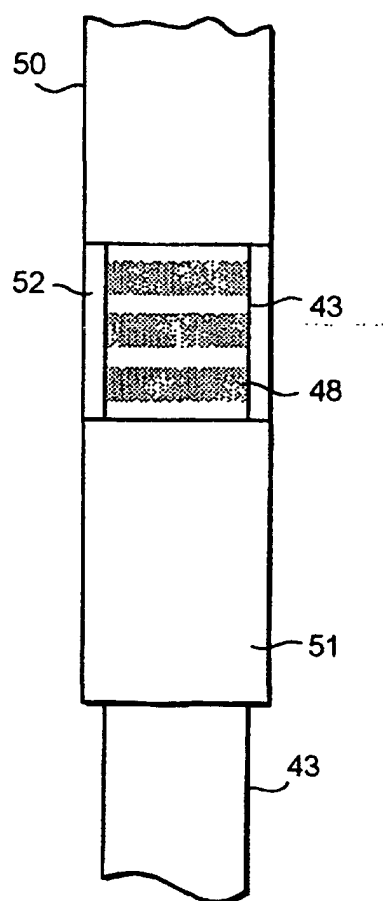


FIG. 3b

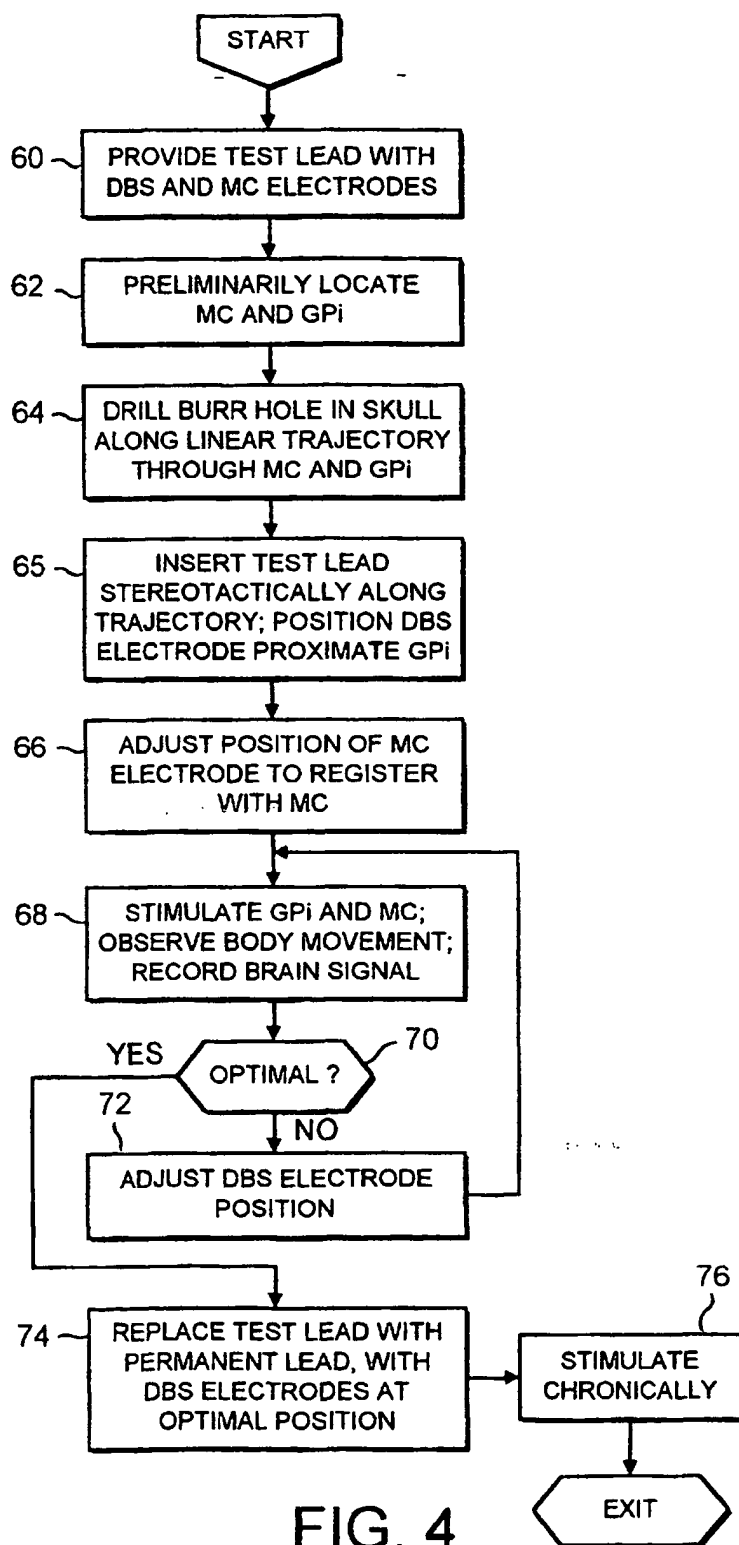


FIG. 4